



# Imaging with PET and SPECT

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# Basics of Radionuclide Production

**Knowledge of production process**

**Purification**

**Recovery of target material**

**Analytical methods (quality control)**

# Radionuclide Production

- (A) **Cyclotron** (ca. 250 world-wide)  
**(Ion accelerator)**
- (B) **Reactor** (ca. 250 Research reactors world-wide)
- 
- (C) **Generators**

# General Aspect

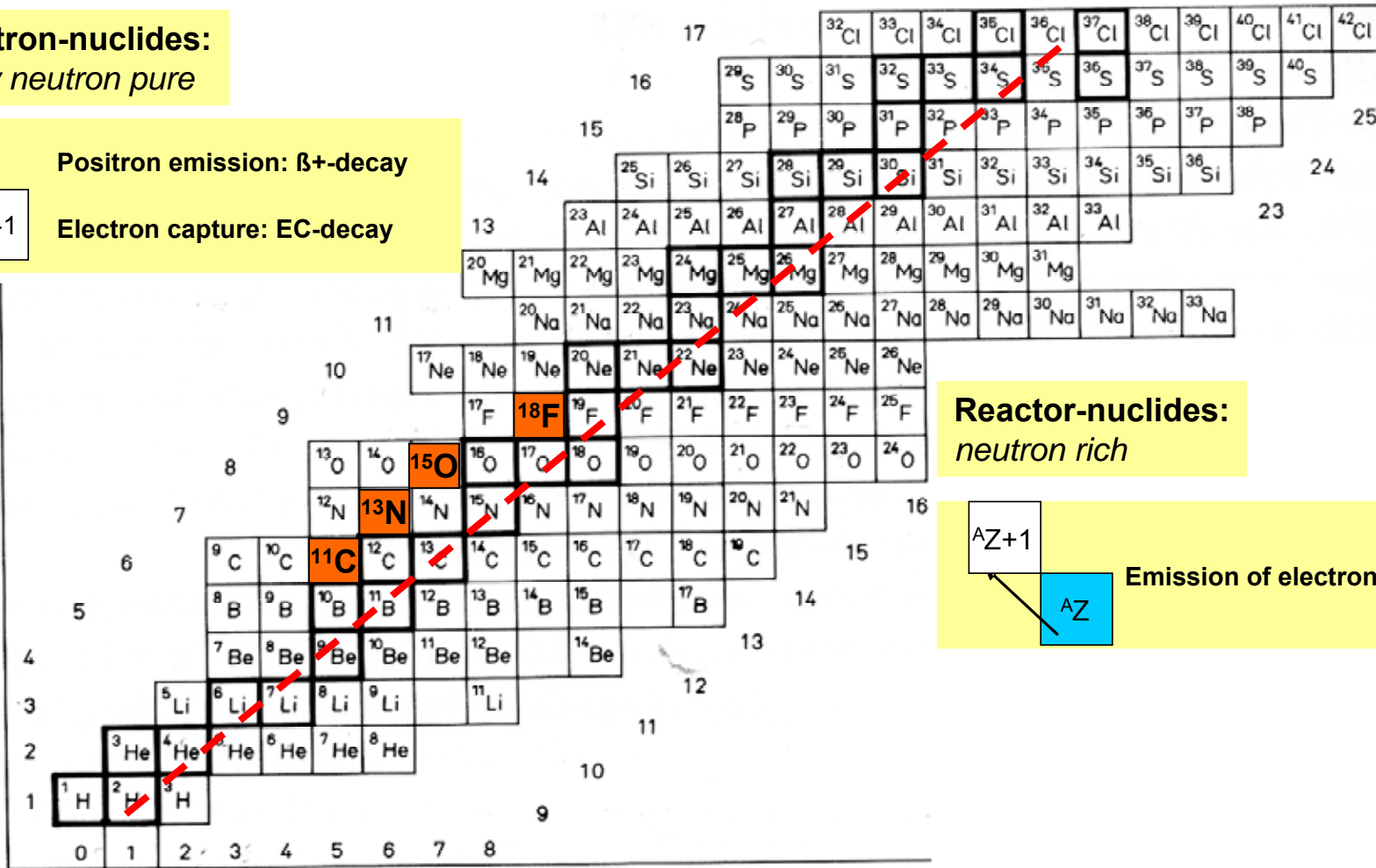
**Cyclotron-nuclides:**  
*mostly neutron pure*

**Positron emission:  $\beta^+$ -decay**

**Electron capture: EC-decay**

A diagram showing a box labeled 'AZ' with an arrow pointing to a box labeled 'AZ-1'.

Proton number  $P = Z$   $\uparrow$



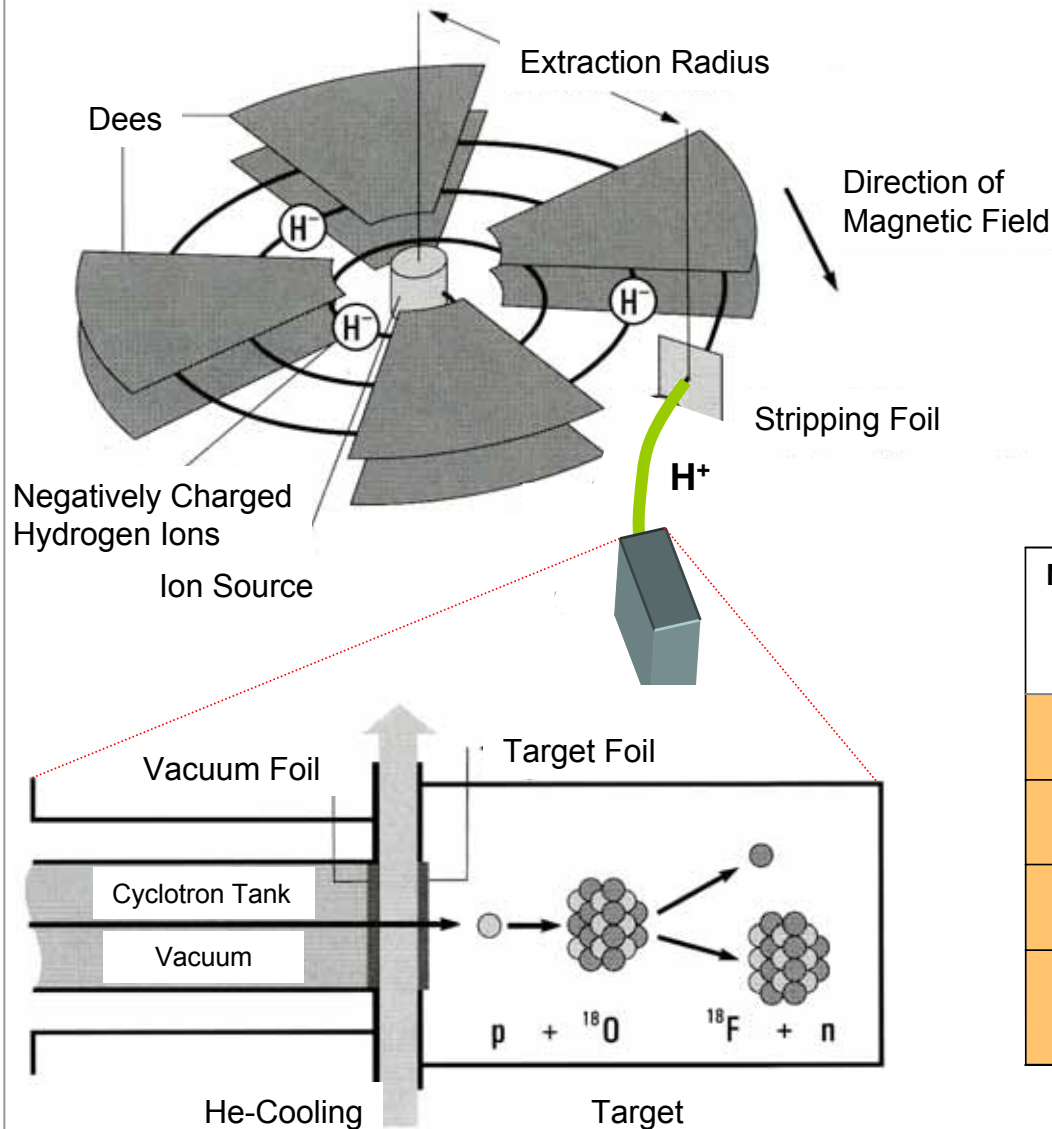
**Reactor-nuclides:**  
*neutron rich*

**Emission of electron  $\beta^-$ -decay**

A diagram showing a box labeled 'AZ+1' with an arrow pointing to a box labeled 'AZ'.

Neutron number  $N = A - Z$   $\rightarrow$

# Production of commonly used PET-Nuclides via Compact Cyclotron



Nuclide	$T_{1/2}$ (min)	Nuclear-Reaction	Energy (MeV)	Mode of decay [%]	Target product
${}^{11}\text{C}$	20.4	${}^{14}\text{N}(p,\alpha)$	13 → 3	$\beta^+$ (99.8)	${}^{11}\text{CO}_2$ ${}^{11}\text{CO}$
${}^{13}\text{N}$	10.0	${}^{16}\text{O}(p,\alpha)$	16 → 7	$\beta^+$ (100)	${}^{13}\text{NO}_2^-$ ${}^{13}\text{NO}_3^-$
${}^{15}\text{O}$	2.0	${}^{15}\text{N}(p,n)$	10 → 0	$\beta^+$ (99.9)	${}^{15}\text{O}_2$
${}^{11}\text{C}$	109.6	${}^{18}\text{O}(p,n)$	16 → 3	$\beta^+$ (97)	${}^{18}\text{F}_{\text{aq}}^-$ ${}^{18}\text{F}_2$

## Selection of Radionuclide

Half-life comparable with kinetics of physiological process ?  
(too short, too long)

Do the nuclear and physical properties fulfill the special demands ?  
(e.g. pure  $\beta^+$  - Emitter)

Labeling chemistry compatible with targeting ?  
(e.g. metalated CNS-ligands)

Patient dose acceptable ?  
(CNS-ligands: C-11 or F-18)

Nuclide availability ?  
(Generator, cyclotron, energy range)

# PET-Radionuclides

Isotope	Half-life [h]	Positron percentage branching % $\beta^+$	Maximum positron energy [MeV] $E_{\beta^+ \text{ max}}$	Intrinsic spacial resolution loss [mm]	Comments
$^{18}\text{F}$	1,8	96,9	0,63	0,7	
$^{55}\text{Co}$	17,5	76	1,50	1,6	$T_{1/2, D} = 2,6 \text{ y}$
$^{61}\text{Cu}$	3,4	61	1,22	1,5	
$^{64}\text{Cu}$	12,7	18	0,65	0,7	
$^{66}\text{Ga}$	9,5	57	4,15	-	
$^{68}\text{Ga}$	1,14	89	1,90	2,4	G: $^{68}\text{Ge} / 271\text{d}$
$^{75}\text{Br}$	1,6	71	1,72	2,2	$T_{1/2, D} = 120 \text{ d}$
$^{76}\text{Br}$	16,2	54	3,94	5,3	
$^{86}\text{Y}$	14,7	33	3,14	1,8	
$^{110\text{m}}\text{In}$	1,15	62	2,20	3,0	G: $^{110}\text{Sn} / 4,1 \text{ h}$
$^{120\text{g}}\text{I}$	1,35	56	4,59	5,4	
$^{124}\text{I}$	100,3	23	2,14	2,3	

# Resolution Limitation due to Positron Energy

**$^{18}\text{F}$**

$\langle\beta^+\rangle = 0,242 \text{ MeV}$

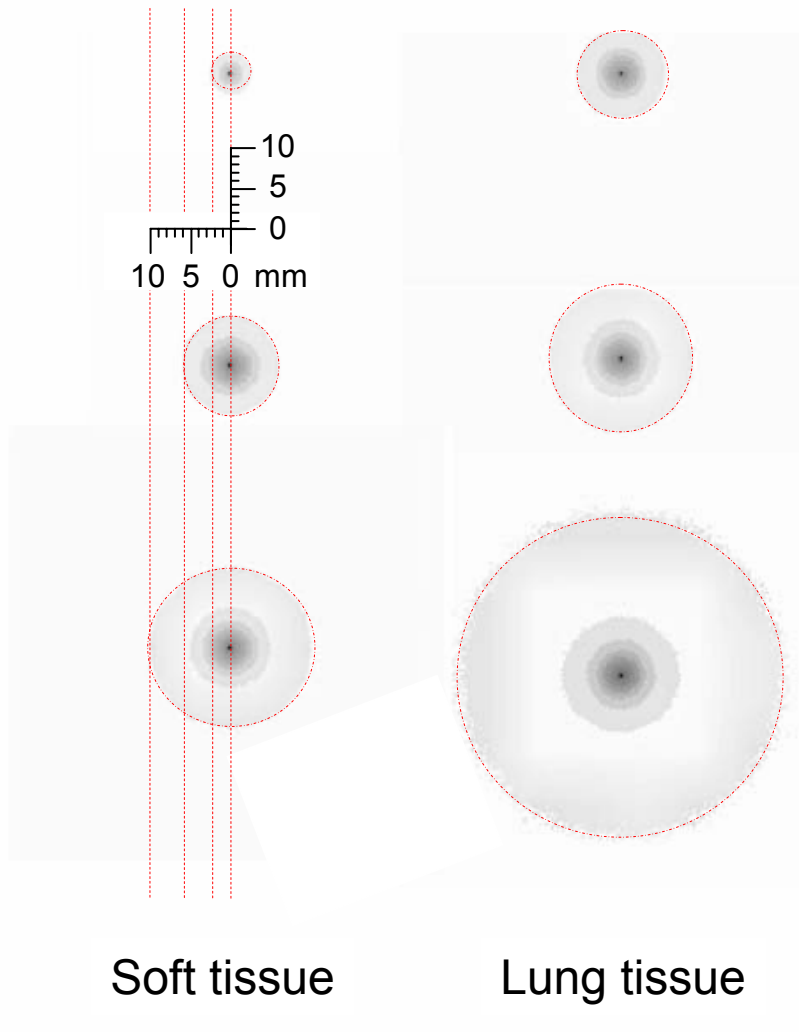
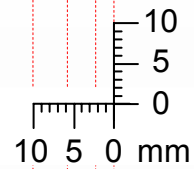
**$^{15}\text{O}$**

$\langle\beta^+\rangle = 0,735 \text{ MeV}$

**$^{82}\text{Rb}$**

$\langle\beta^+\rangle = 1.409 \text{ MeV}$

Compact bone

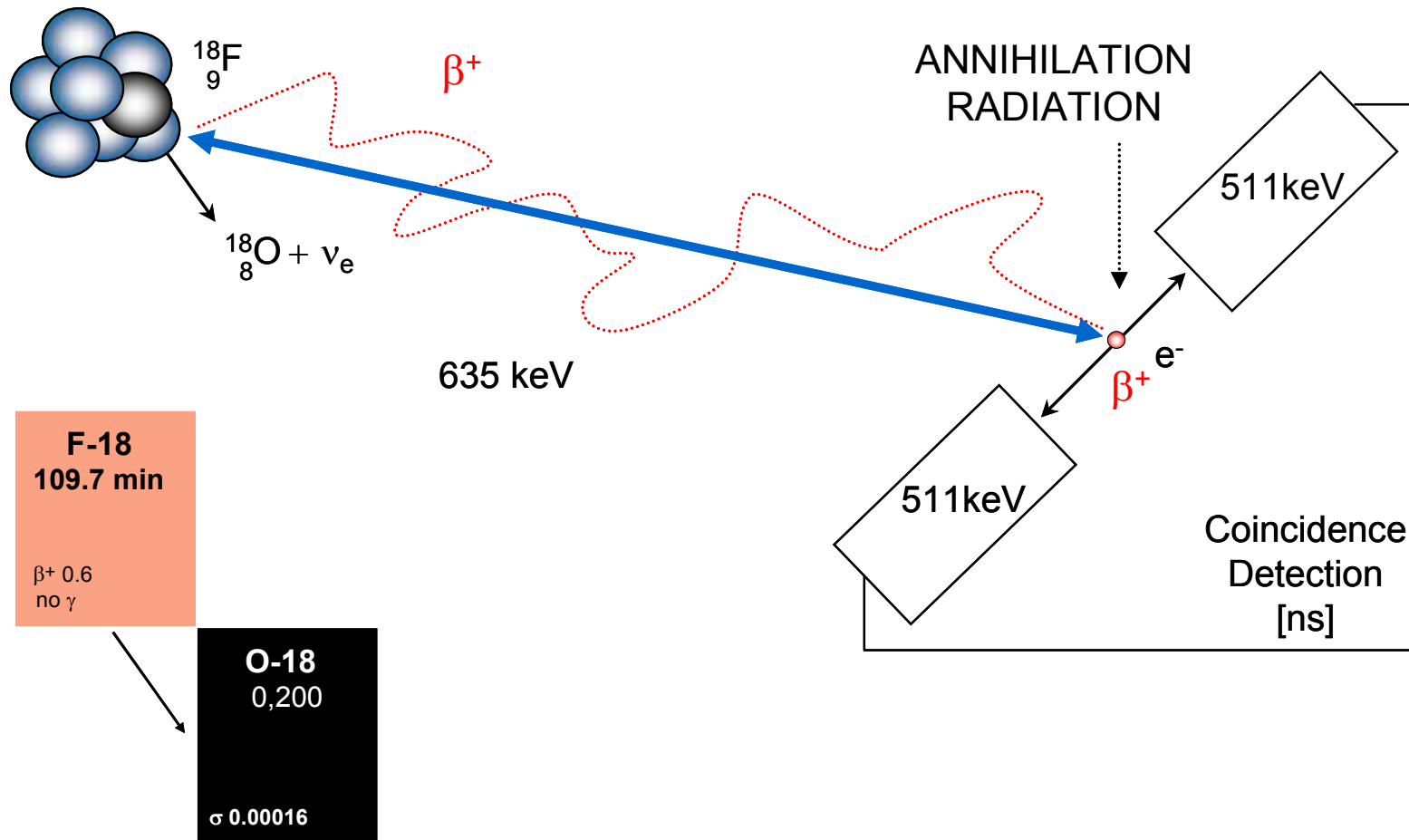


Soft tissue

Lung tissue



# Positron-Emission



## Production of F-18

Nuclear reaction	$^{18}\text{O}(p,n)^{18}\text{F}$	$^{16}\text{O}(^3\text{He},n)^{18}\text{F}$	$^{20}\text{Ne}(d,\alpha)^{18}\text{F}$	$^{18}\text{O}(p,n)^{18}\text{F}$
Target	$\text{H}_2^{18}\text{O}$	$\text{H}_2\text{O}$	Ne (0.1-0.2% $\text{F}_2$ , 18 bar)	$^{18}\text{O}_2$ (20 bar) (2. + 0.1% $\text{F}_2$ )
Energy range of bombarding particle [MeV]	<b>16 → 0</b>	36 → 0	11.2 → 0	10 → 0
Chemical form	$[^{18}\text{F}]\text{F}_{\text{aq}}^-$	$[^{18}\text{F}]\text{F}_{\text{aq}}^-$	$[^{18}\text{F}]\text{F}_2$	$[^{18}\text{F}]\text{F}_2$
Thick target yield [MBq $\mu\text{A}^{-1} \text{h}^{-1}$ ]	<b>2.200</b>	250	350-450	~350
Specific activity [TBq $\text{mmol}^{-1}$ ]	<b><math>40 \times 10^3</math></b>	$40 \times 10^3$	0.04–0.4	0.04-2

- **Mainly produced via  $^{18}\text{O}(p,n)^{18}\text{F}$ -reaction**
- **Product:**  $^{18}\text{F}_{\text{aq}}^-$  with high specific activity and up to 100% radiochemical yield, compared to  $[^{18}\text{F}]\text{F}_2$  with low specific activity and max. 50% radiochemical yield

# $^{18}\text{F}$ -Fluoride Chemistry

## Nucleophilic Substitution

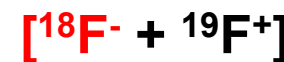
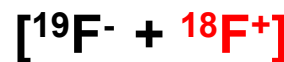


Non-diluted  
with unlabeled  
tracer  
=  
„No-carrier-added“  
(n.c.a)

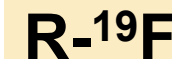


z.B.  $^{18}\text{F}$ Fluor-Choline

## Electrophilic Substitution



z.B.  $^{18}\text{F}$ Dopa

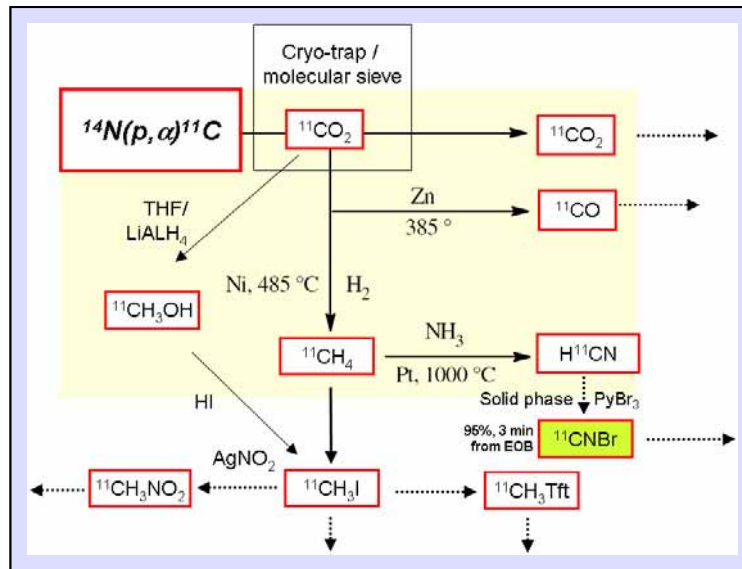


diluted  
with unlabeled  
fluorine  
=  
„carrier-added“  
(c.a)

Only for targets with  
high capacity  
(e.g. enzym  
substrates);  
not suitable saturable  
processes (e.g.  
peptide-receptor-  
ligands)

# Production Scheme: Radiopharmaceutical Production

## Cyclotron und on-line synthesis



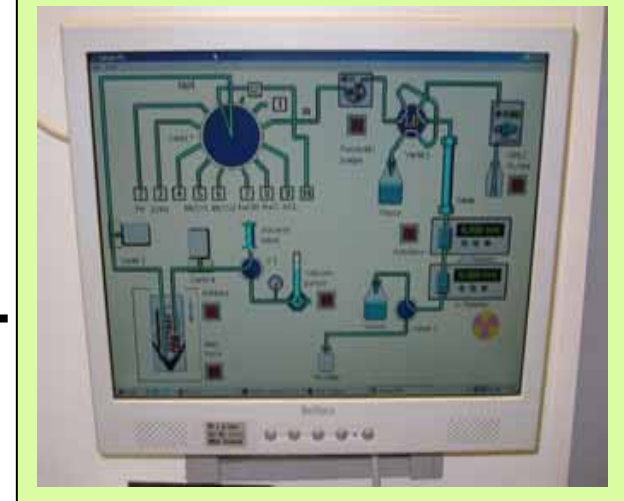
## Automatic production



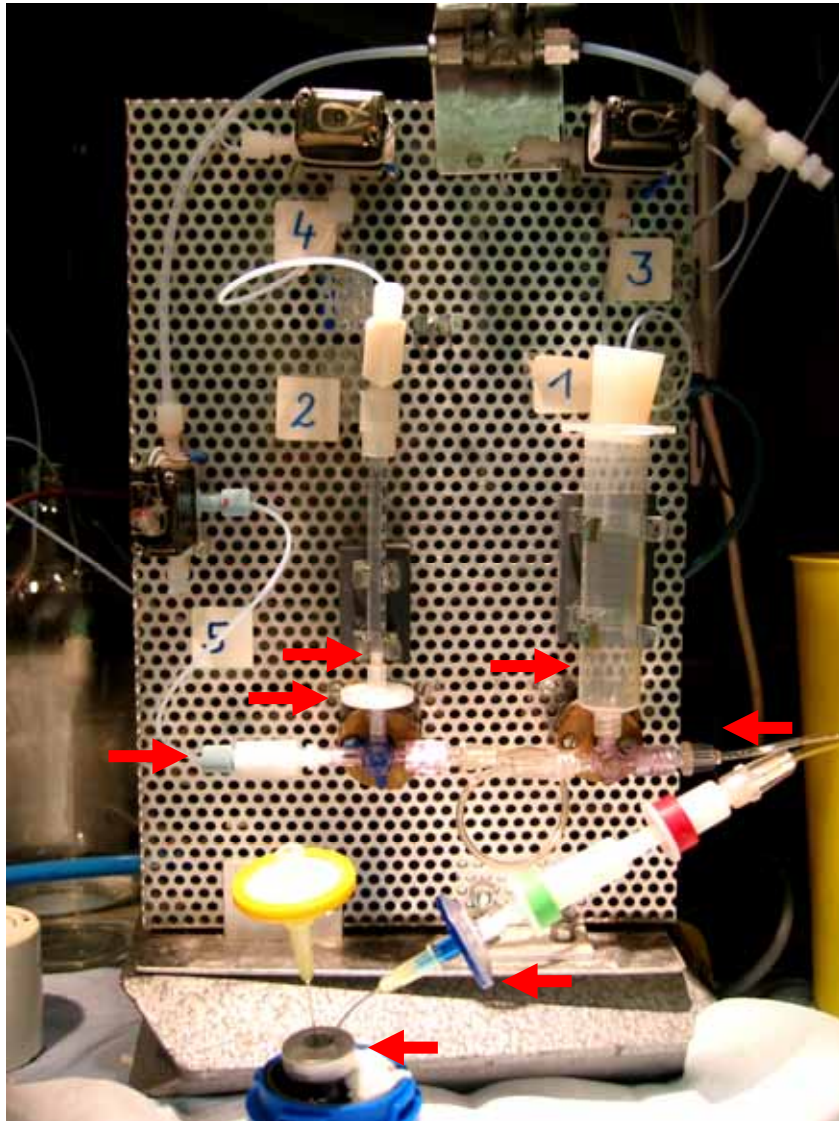
## Quality control



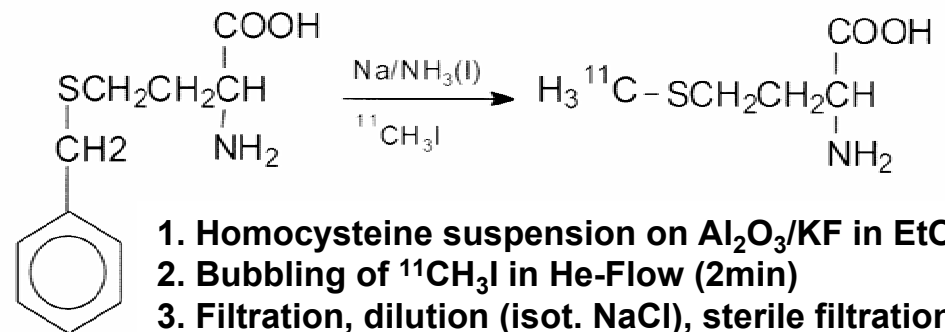
## Application



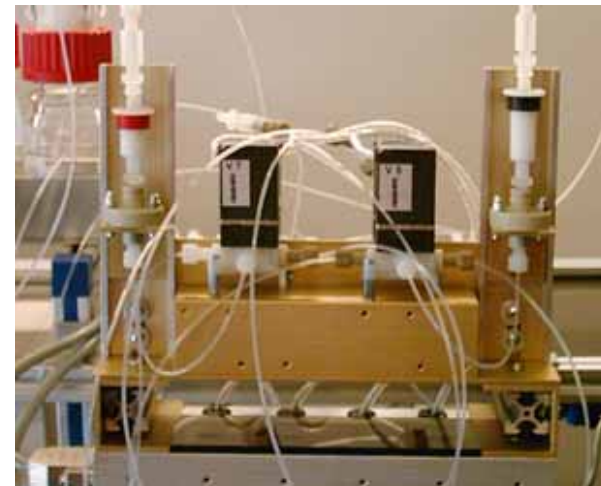
# Automatic Synthesis



## $^{11}\text{C}$ -Methionine Production



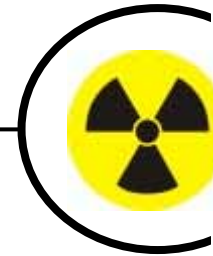
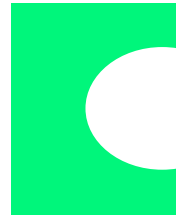
1. Homocysteine suspension on  $\text{Al}_2\text{O}_3/\text{KF}$  in EtOH
2. Bubbling of  $^{11}\text{C}\text{H}_3\text{I}$  in He-Flow (2min)
3. Filtration, dilution (isot. NaCl), sterile filtration



## Generators for Positron Emission

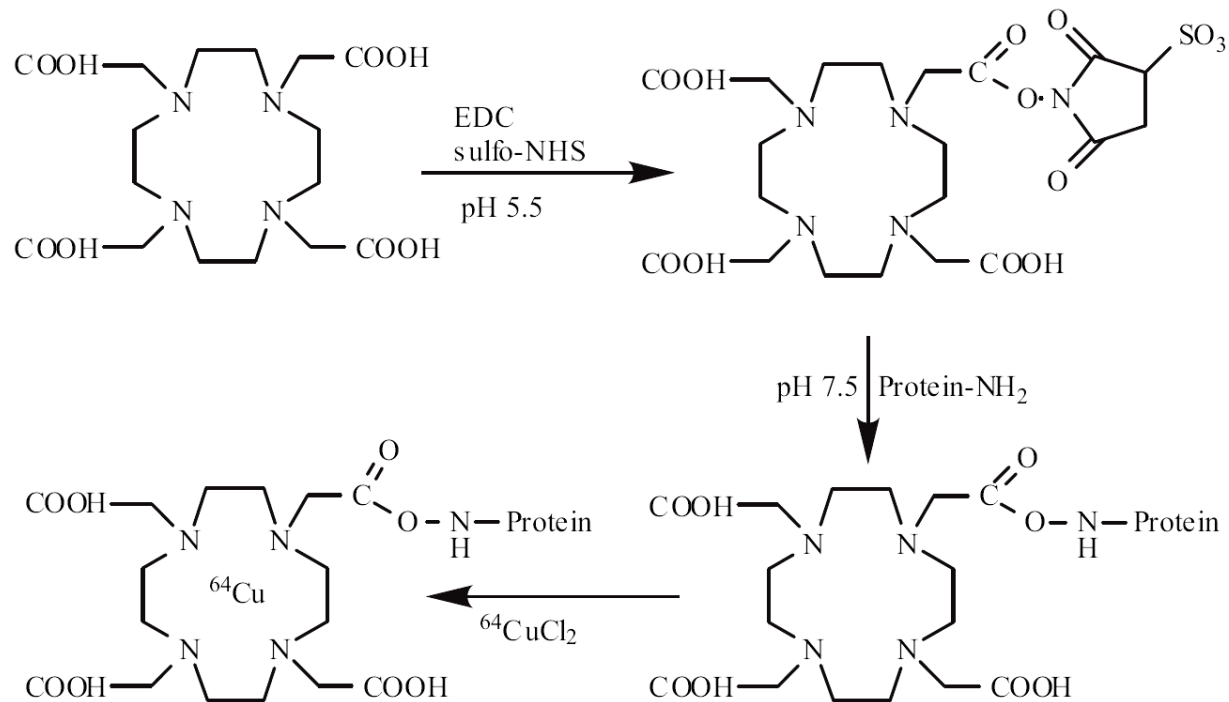
Isotope	Half-life	Mode of decay	$E_{\beta^+}$ [keV]
$^{68}\text{Ge}$	271 d	EC (100%)	
↓			
$^{68}\text{Ga}$	68 min	$\beta^+$ (90%), EC (10%)	1900
$^{62}\text{Zn}$	9.2 h	$\beta^+$ (93%), EC (7%)	660
↓			
$^{62}\text{Cu}$	9.7 min	$\beta^+$ (98%), EC(2%)	2930
$^{82}\text{Sr}$	25 d	EC (100%)	
↓			
$^{82}\text{Rb}$	1.3 min	$\beta^+$ (96%), EC (4%)	3350

# Structure of „non-isotopic“ Radiopharmaceuticals



<b>Address, Target</b>	<b>Pharmacophor, biospecific binding</b>	<b>Spacer, Linker</b>	<b>Labeling, Label</b>
Intra-/Extracellular Receptors Transporter Enzyme Antigens RNA ...	Small org. Molecules Peptidomimetics Peptide Protein Antibody Complex (Ions)	Metabolic stabile Metabolic labile Enzymatic cleavable Hydrolytic sensitive pH sensitive	Covalent Complex Statically distributed Defined bondage No-carrier-added Carrier-added

# Peptide, Protein and Macromolecule Labeling with Radiometals



In, Ga, Cu ...  
 Lu, Y, Bi, Ac ...  
 Fe, Gd, .....



# Radionuclide Production for SPECT

SPECT = Single-Photon-Emission-Computer Tomography

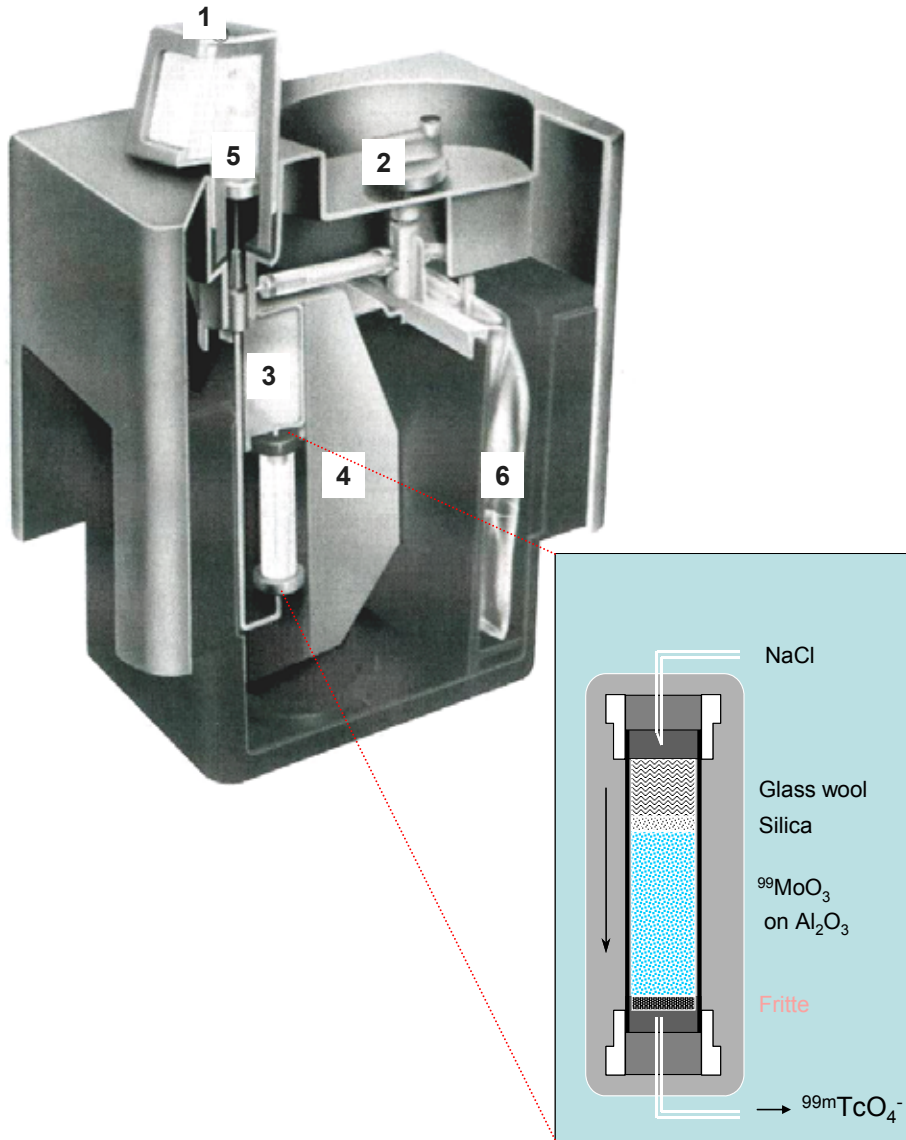
**All these nuclides are commercially produced and sold  
as radionuclide,  
generators  
or readily-prepared radiopharmaceuticals**

**Most important SPECT-Isotope is Technetium ( $^{99m}\text{Tc}$ ) !**

# SPECT - Isotopes

Radio nuclide	$T_{1/2}$	Mode of decay	Main- $\gamma$ -Lines	Productions data		
				Nuclear reaction	Energy range [MeV]	Yield [MBq/ $\mu$ Ah]
$^{67}\text{Ga}$	3.26 d	EC (100)	93 (27%)	$^{68}\text{Zn}(p,2n)$	26→18	185
$^{99}\text{Mo}$ ↓ $^{99\text{m}}\text{Tc}$	2.75 d  6.0 h	b- (100)  IT (100)	181 (6%) 740 (12%) 141 (87%)	$^{235}\text{U}(n,f)$ $^{98}\text{Mo}(n,g)$	$\sigma_{\text{th}} = 0.14\text{b}$	
$^{111}\text{In}$	2.8 d	EC (100)	173 (91%) 247 (94%)	$^{112}\text{Cd}(p,2n)$	25→18	166
$^{123}\text{I}$	13.2 h	EC (100)	159 (83%)	$^{123}\text{Te}(p,n)$ $^{124}\text{Xe}(p,x)^{123}\text{Xe}$ $^{127}\text{I}(p,5n)^{123}\text{Xe}$	14.5→10 29→23 65→45	137 414 777
$^{201}\text{Tl}$	3.06 d	EC (100)	68-82 (RL) 166 (10.2%)	$^{210}\text{Tl}(p,3n)^{201}\text{Pb}$	28→20	

# $^{99m}\text{Tc}$ -Generator (1)



## (1) Simple Handling

Insert vacuum flask and elute desired volume.

## (2) Transport-Security-valve

Prevent an elution after production and during transport

## (3) Shifted needle

Reduction of energy rich Mo-radiation

## (4) Max. protection against radiation

Protection from all side.

$^{99}\text{Mo}$ -column is covered at least with 52 mm Pb.

Supplementary shielding with overall 98 mm Pb.

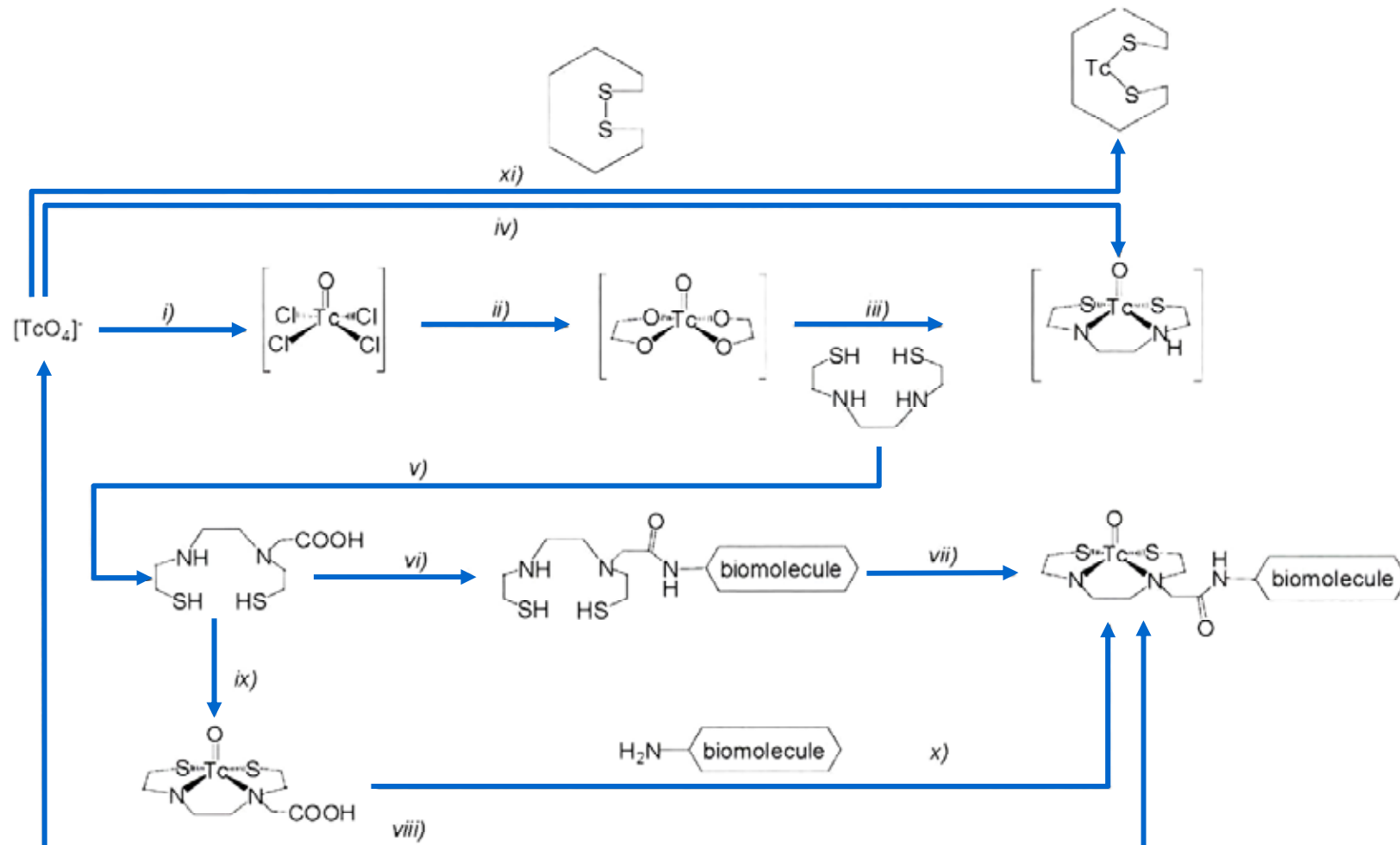
## (5) High concentrated activity

Total  $^{99m}\text{Tc}$ -activity is less than 5 mL volume.

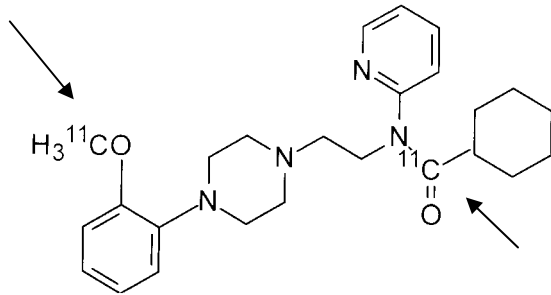
## (6) Ready for use

Sterile, closed system.

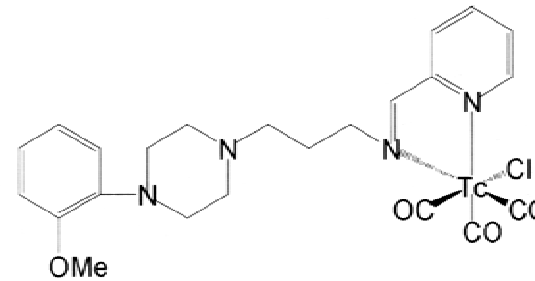
# Labeling of Tc-Radiopharmaceuticals



# Tracer Properties: Influence of the Nuclide



WAY 100638 (5-HT<sub>1A</sub>-receptor ligand)



<sup>99m</sup>Tc-WAY 100638-analog  
(as 5-HT<sub>1A</sub>-receptor ligand)

<sup>11</sup>C

<sup>18</sup>F

<sup>123</sup>I

<sup>99m</sup>Tc

<sup>68</sup>Ga / <sup>111</sup>In

Change in structure

Predictability of biological integrity

Complexity of radiopharmaceutical development

# Molecular Imaging by Radiotracer

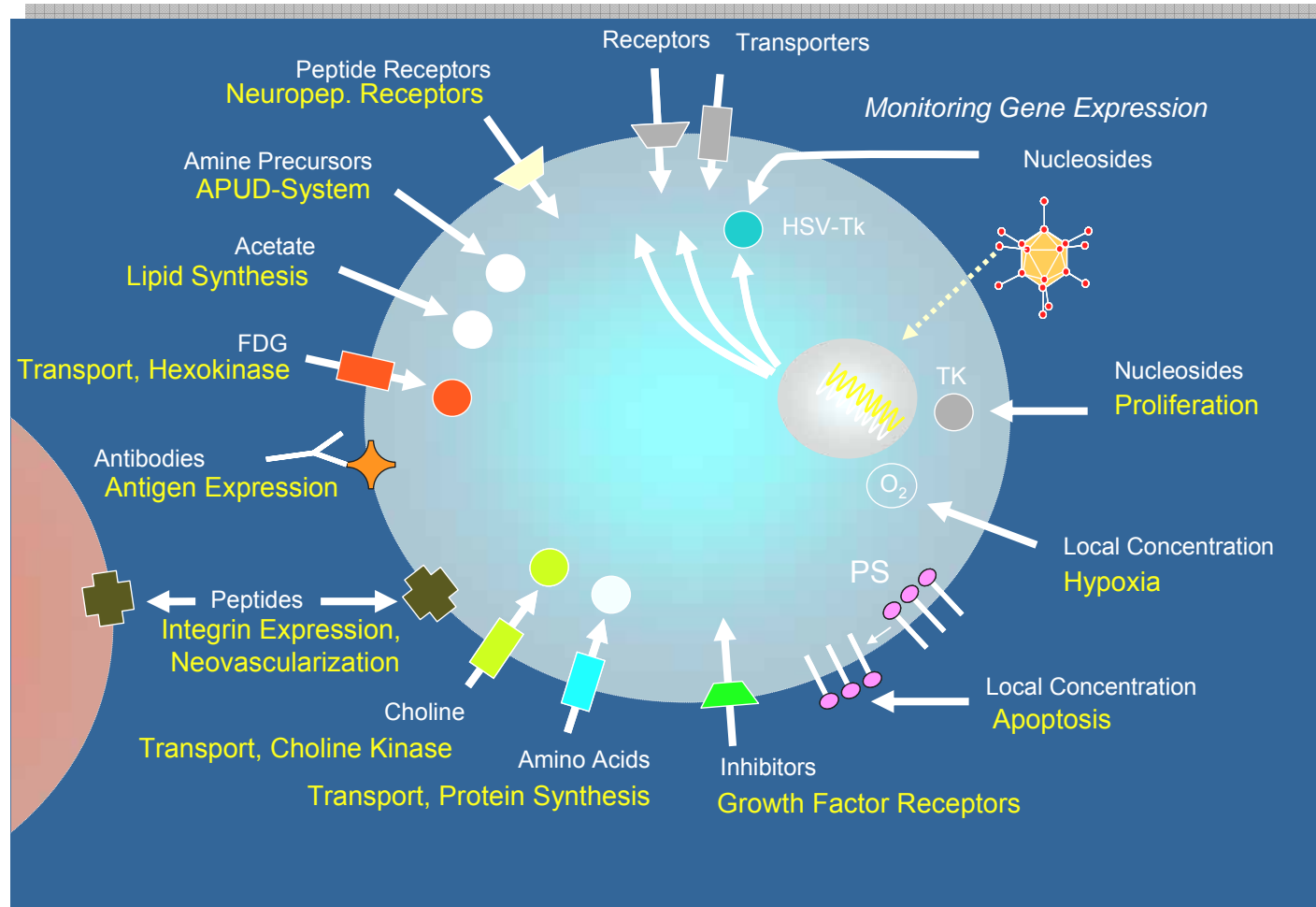
Targeting biochemical processes in living organism  
on basis of molecular interaction between tracer und target

by radiolabeled, „molecular probes“, changing their concentration at  
the target in a specific way

and suitable detection systems for non-invasive, quantitative  
and repetitive measurement

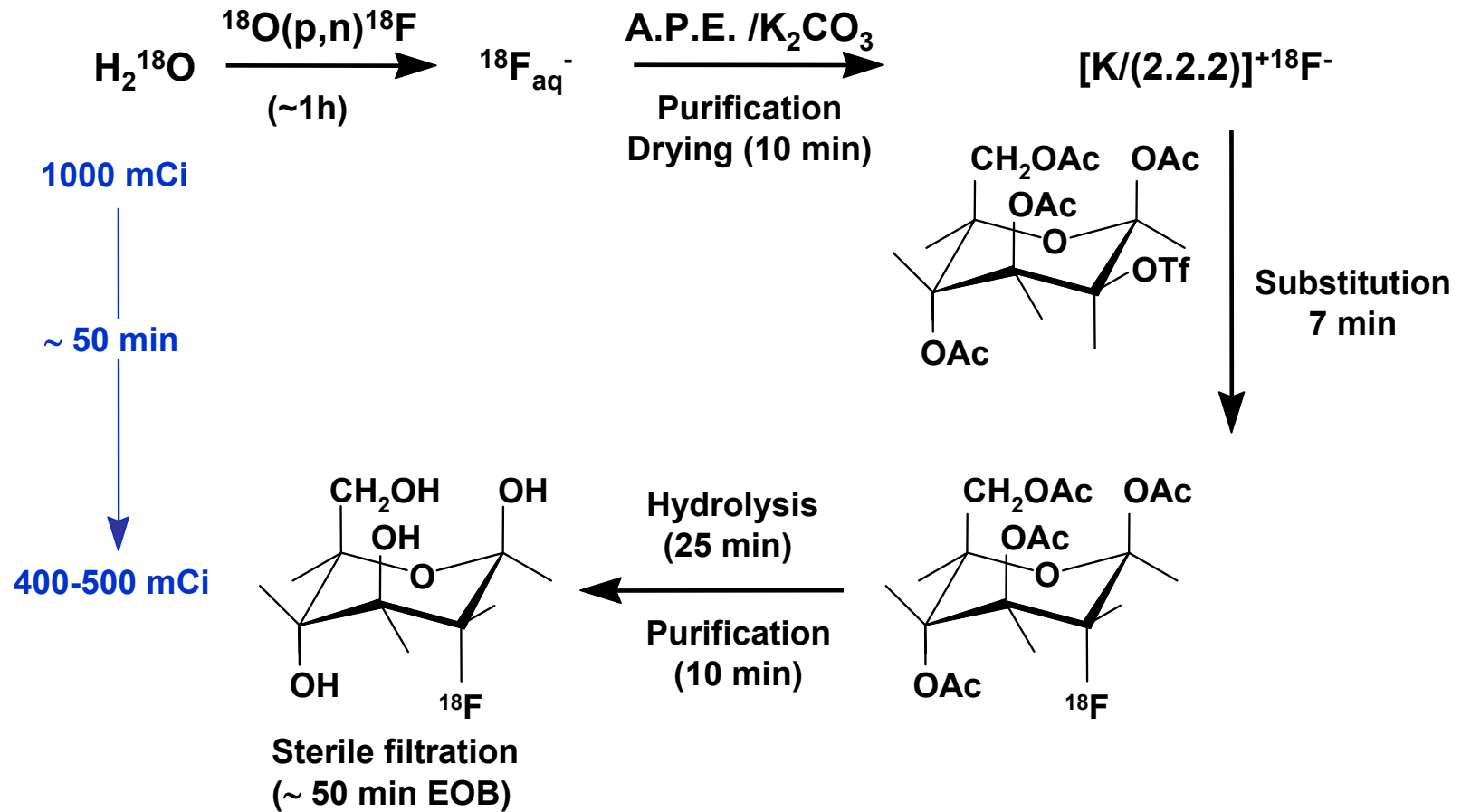
with the aim of exploring physiological processes,  
diagnostics und therapy as well as therapy monitoring

# Target Structures in Oncology



Characterization of the tumor biology by molecular imaging

# 2-[<sup>18</sup>F]Fluoro-2-Deoxy-Glucose-Synthesis ([<sup>18</sup>F]FDG)

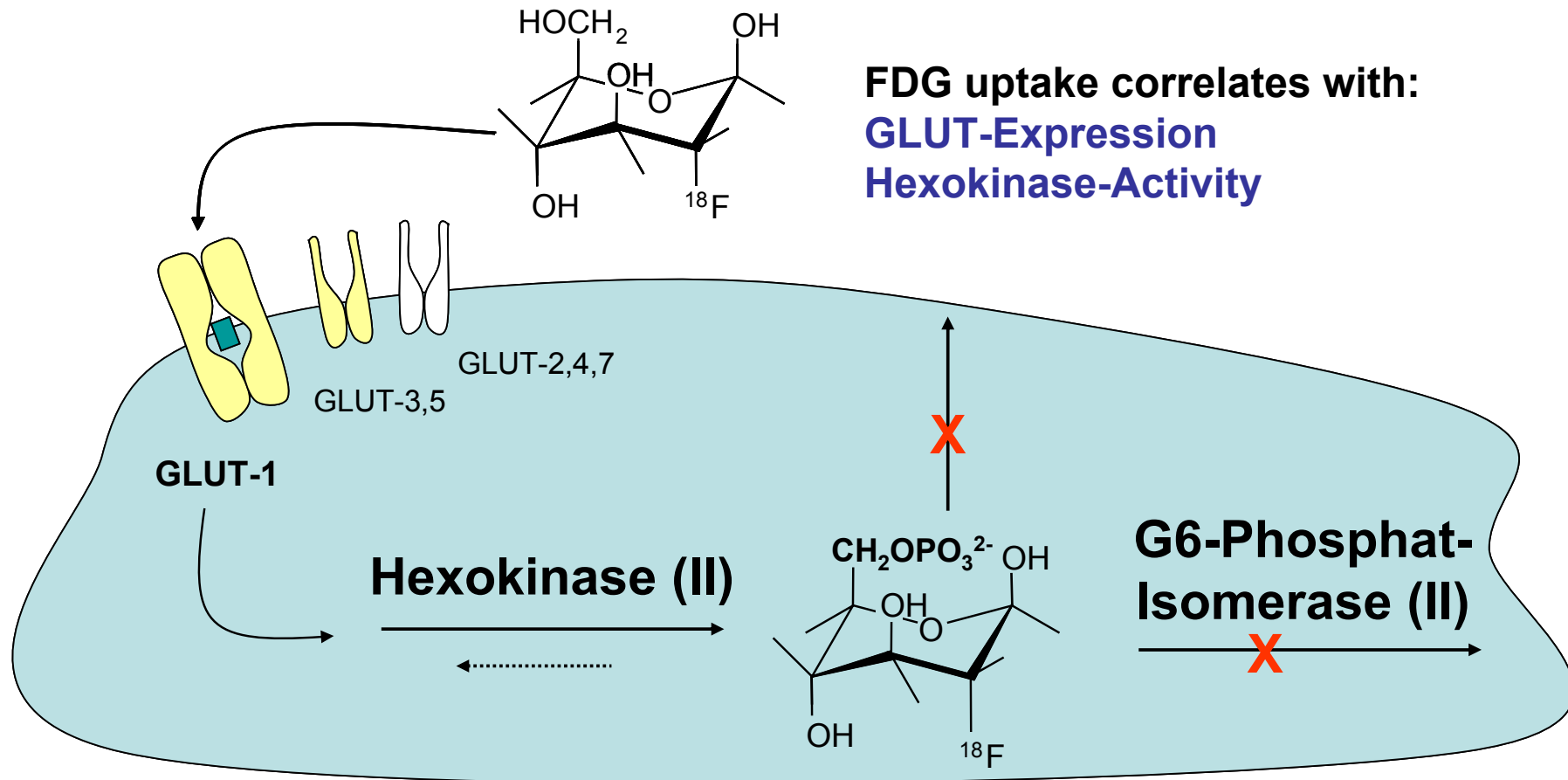




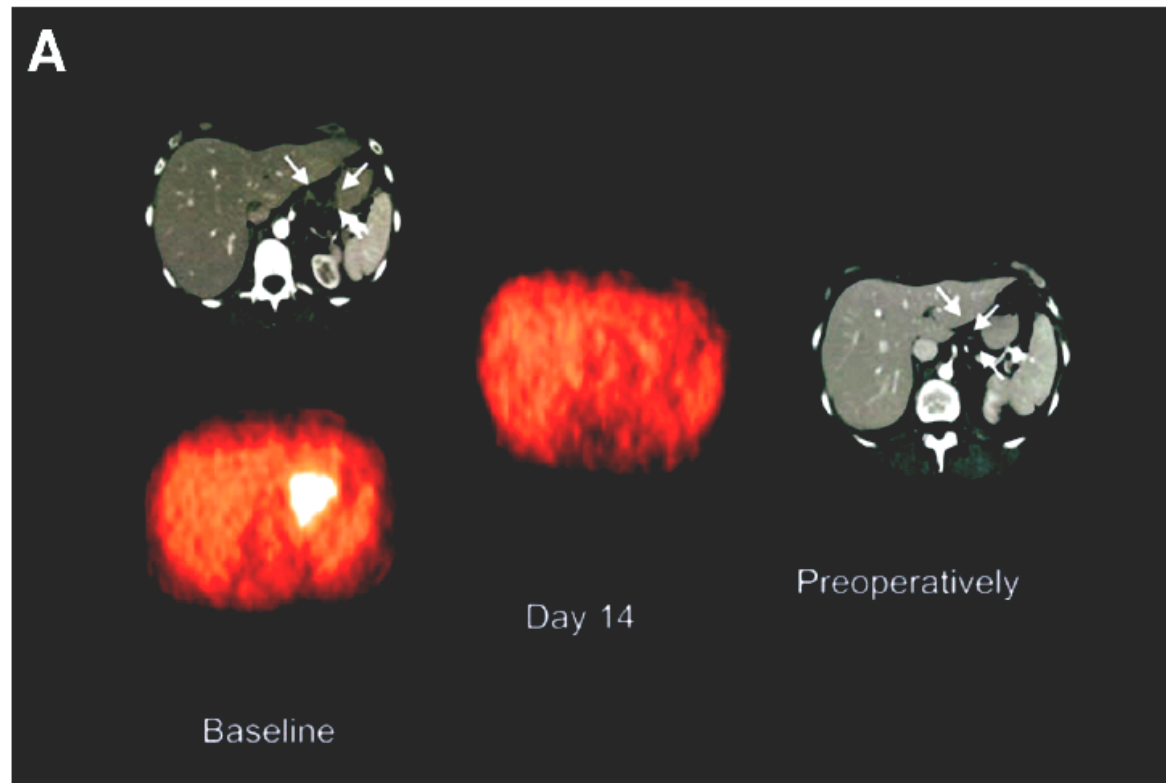
# GMP Production of FDG 2-[<sup>18</sup>F]Fluor-2-deoxy-D-Glucose, TU Munich



# Scheme of [ $^{18}\text{F}$ ]FDG Uptake

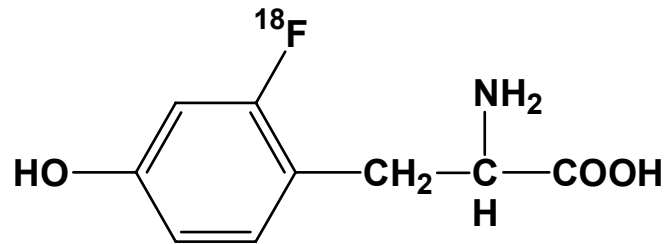


# [<sup>18</sup>F]FDG: Therapy control –gastric carcinoma-

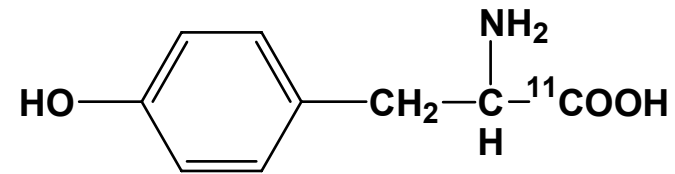


# Amino Acid Transport

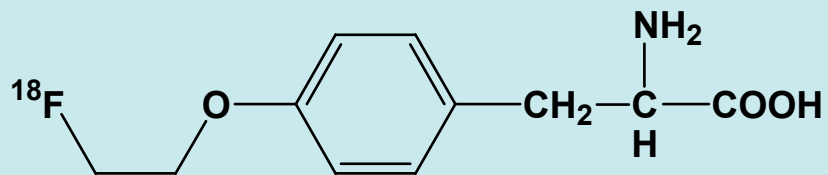
Primary target: Rate measurement of regional protein synthesis  
 But: During the short time period after injection the accumulation of tracer represent only the accumulation of amino acid by special transport systems



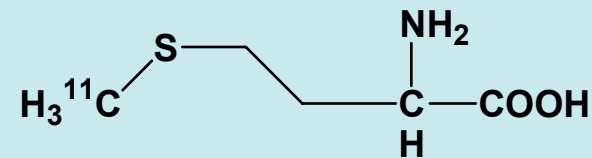
2-Fluoro-L-Tyrosin **2-[<sup>18</sup>F]Tyr**



L-Tyrosin **1-[<sup>11</sup>C]Tyr**

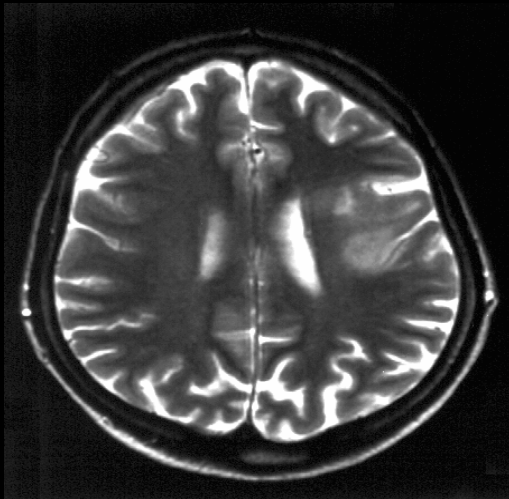


O-(2-Fluoroethyl)-L-Tyrosin **[<sup>18</sup>F]FET**

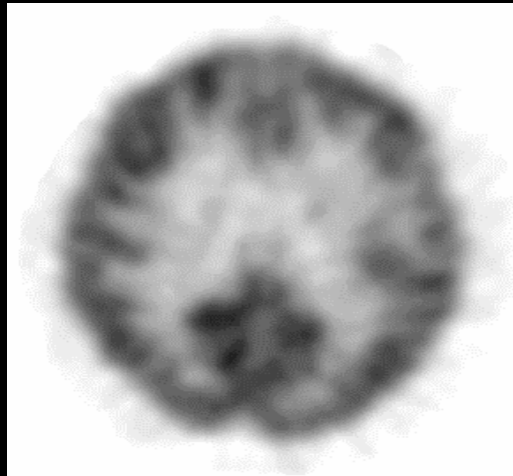


L-Methionine **[<sup>11</sup>C]MET**

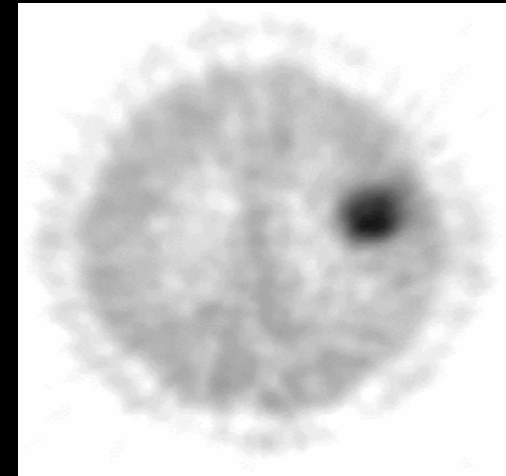
# $[^{18}\text{F}]$ FDG-PET versus $[^{11}\text{C}]$ MET-PET -Brain Tumor-



MRT (T2)



FDG-PET



$[^{11}\text{C}]$ Methionine-PET

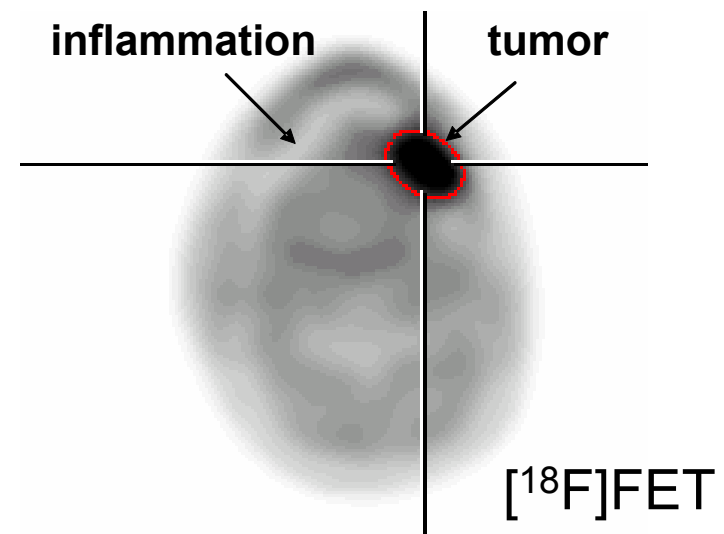
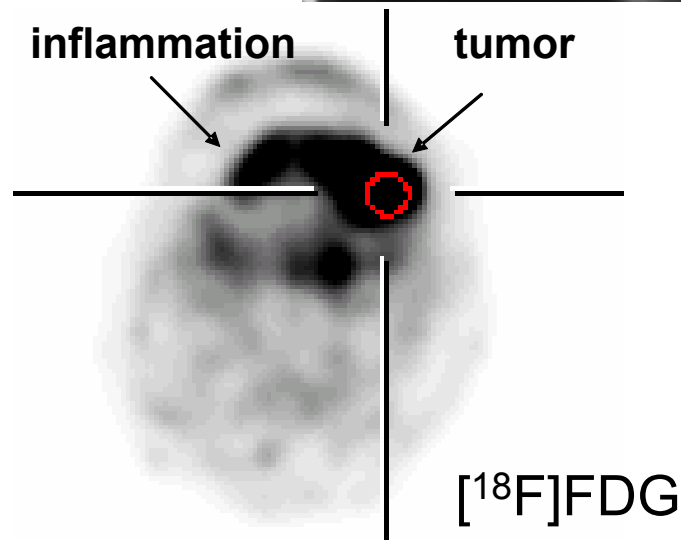
## O-(2-[ $^{18}\text{F}$ ]Fluoroethyl)-L-Tyrosin: [ $^{18}\text{F}$ ]FET (2)

FDG also accumulates in inflammation, amino acids and especially FET does not accumulate in inflammation.

Squamous cell carcinoma



Osteolyse



# Imaging of Metastatic Prostate Cancer

**$^{11}\text{C}$ -Acetate:**

**Prostate cells undergo metabolic transformation from citrate producing normal cells to citrate oxidizing malignant cells (Costello LC et al. *Urology* 1997)**

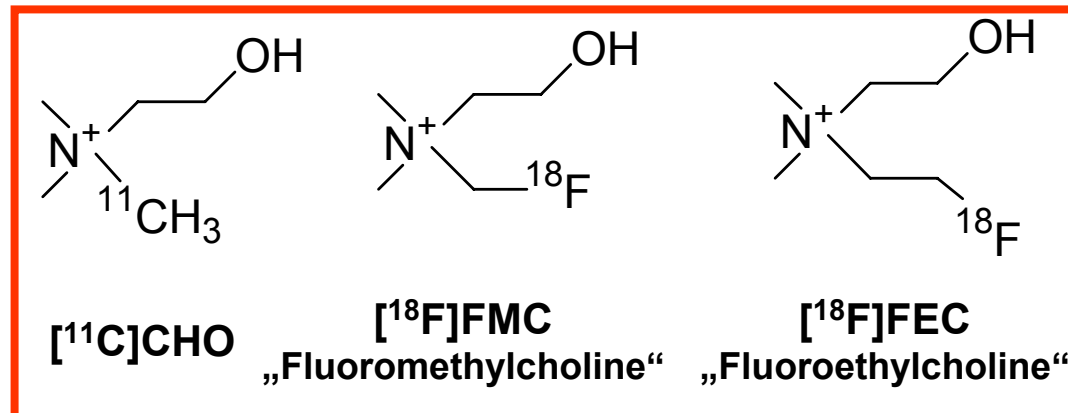
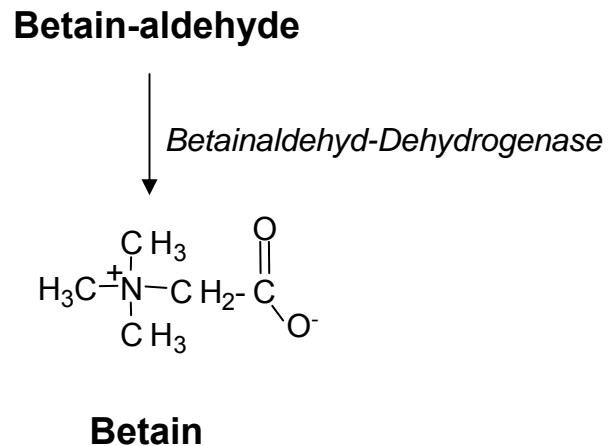
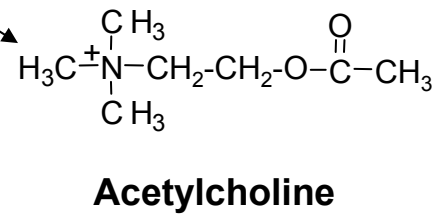
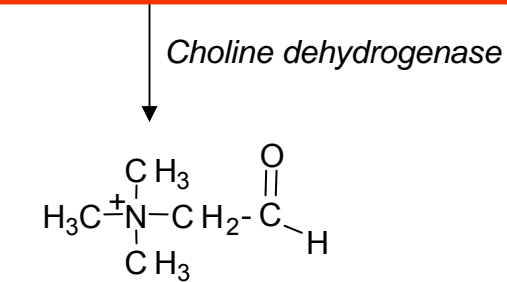
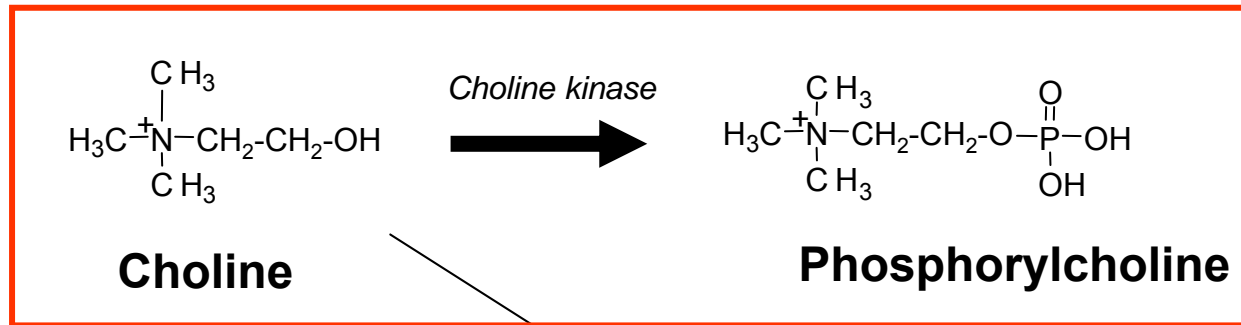
**$^{18}\text{F}/^{11}\text{C}$ -Cholines:**

**malignant transformation is associated with induction of choline kinase activity (e.g. Kotzerke et al. and refs herein; *J Nucl Med.* 2002)**

**( $^{18}\text{F}$ -Fluoride):**

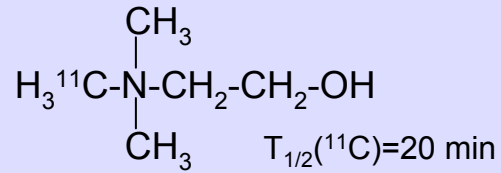
**(for bone metastasis)**

# Biochemical Model: Choline

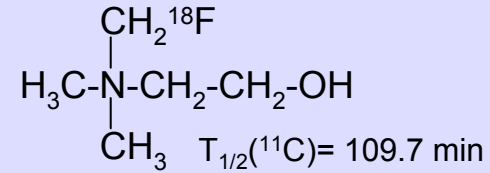




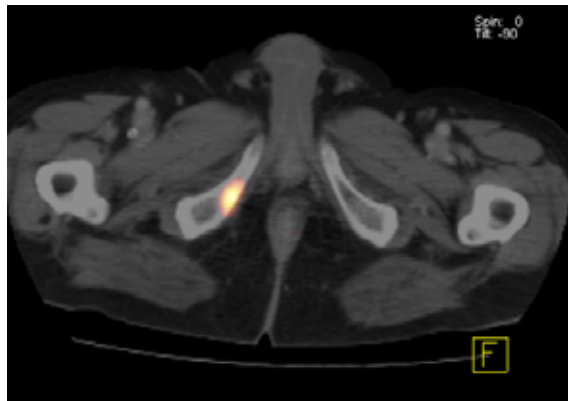
# <sup>11</sup>C-Choline-PET



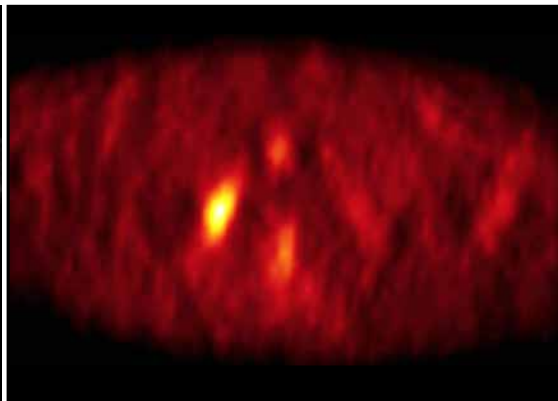
# <sup>18</sup>F-Choline-PET



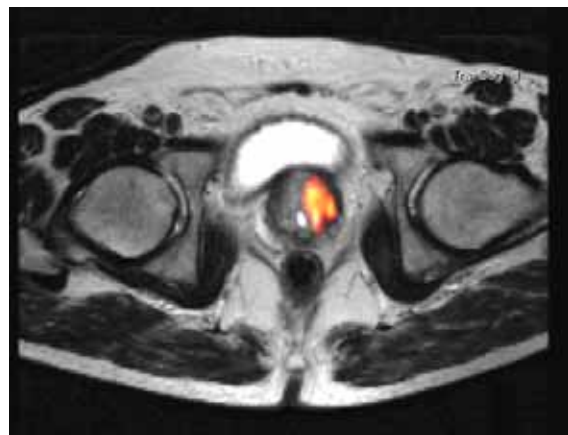
## Bladder cancer metastasis



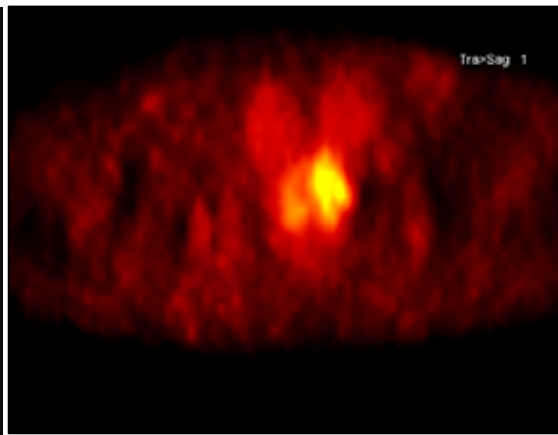
PET/CT



PET



Prostate carcinoma

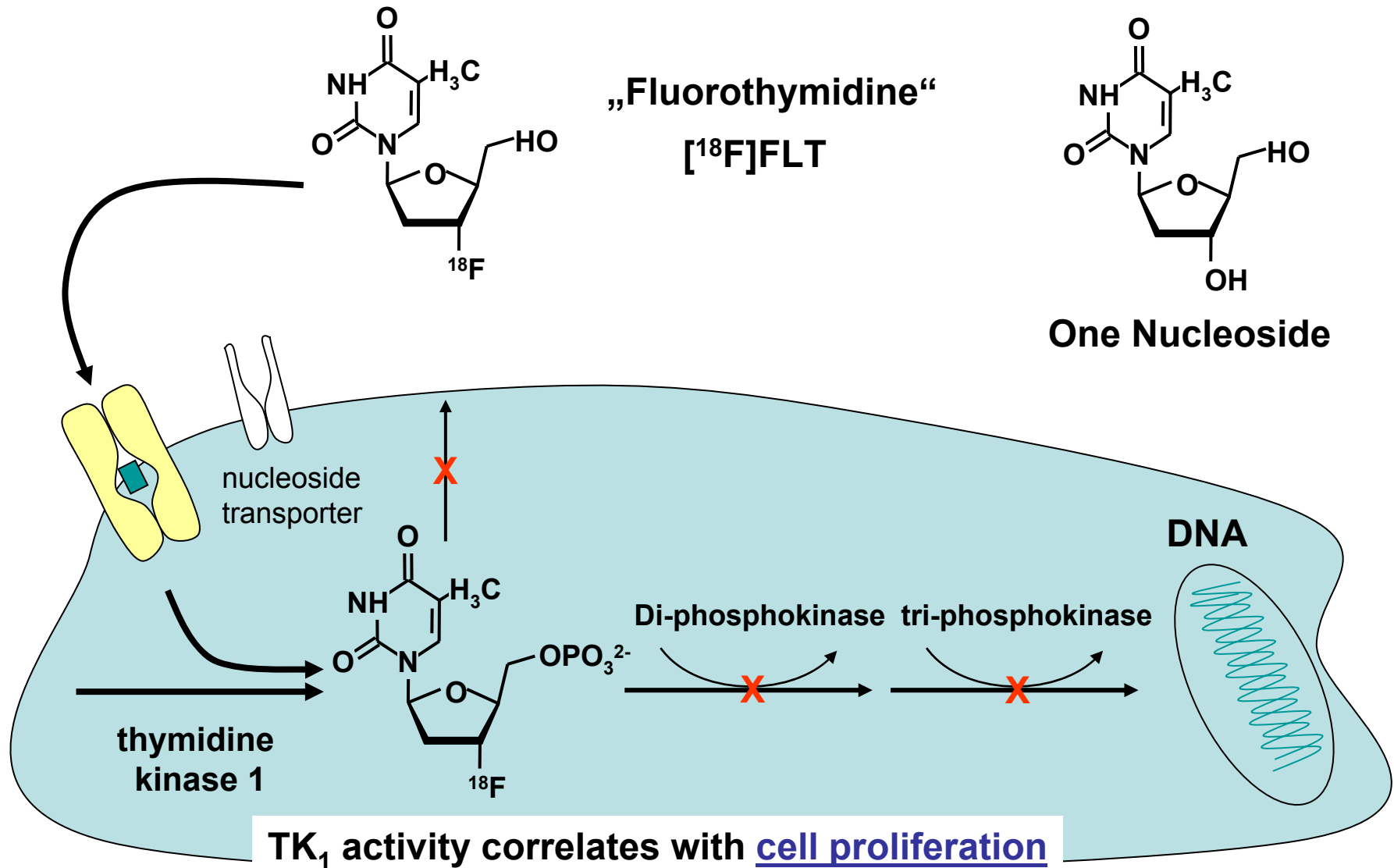


Tracer accumulation with:

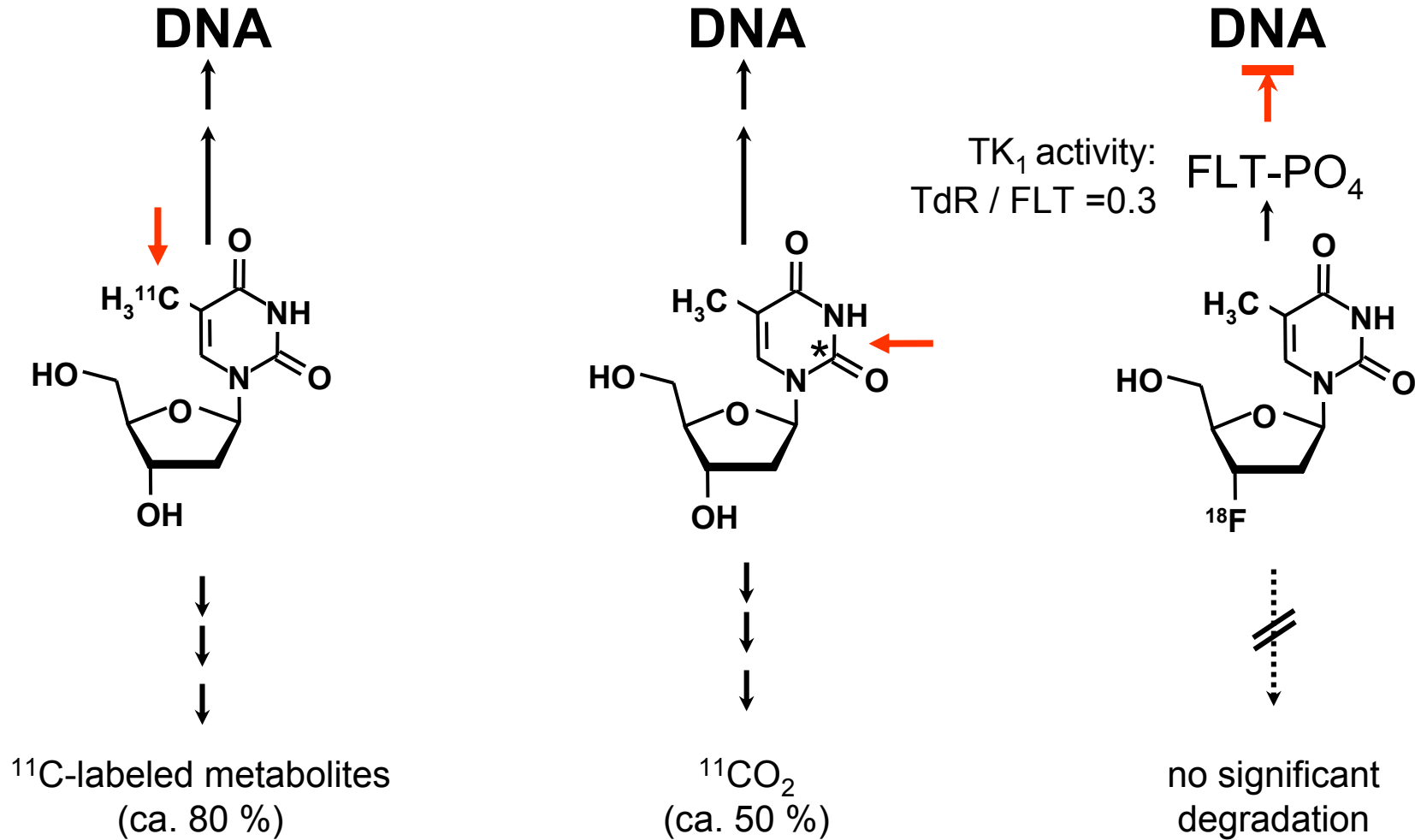
1. Cellular accumulation by choline transporter; (Signal in the first minutes after injection)

2. and followed by phosphorylation by choline kinase. (Signal by late imaging)

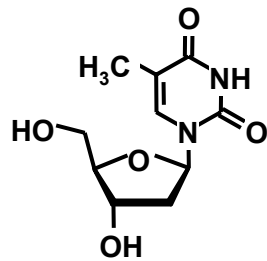
# 3'-[<sup>18</sup>F]Fluoro-3'-Deoxy-Thymidine: [<sup>18</sup>F]FLT



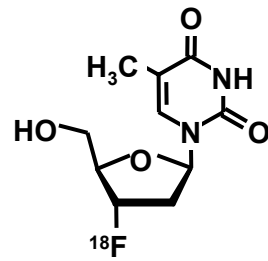
# Metabolic Scheme for [<sup>11</sup>C]Thymidine and FLT



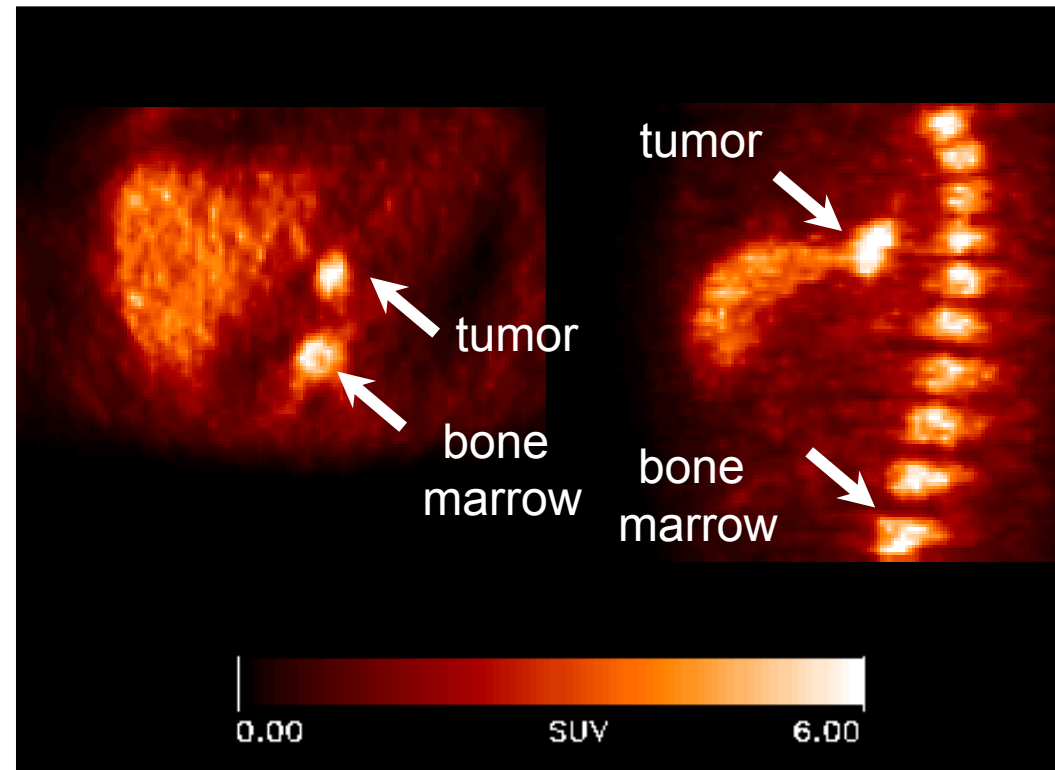
# Visualization of Cell Proliferation with $^{18}\text{F}$ -thymidine (FLT) in Esophageal Cancer



thymidine

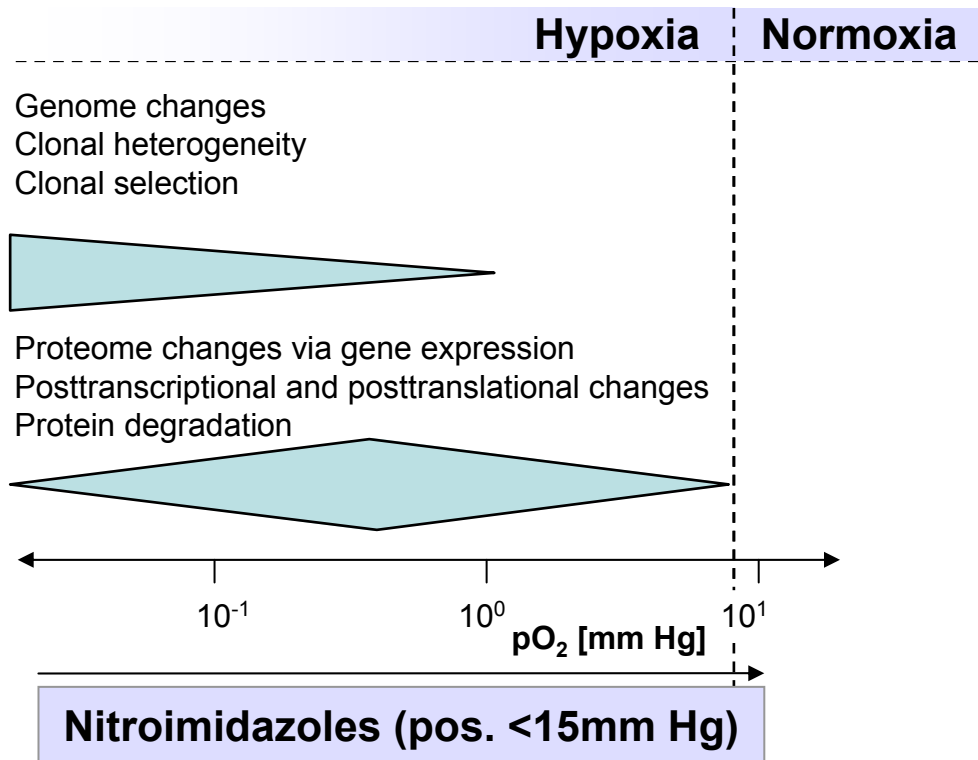


[ $^{18}\text{F}$ ]FLT

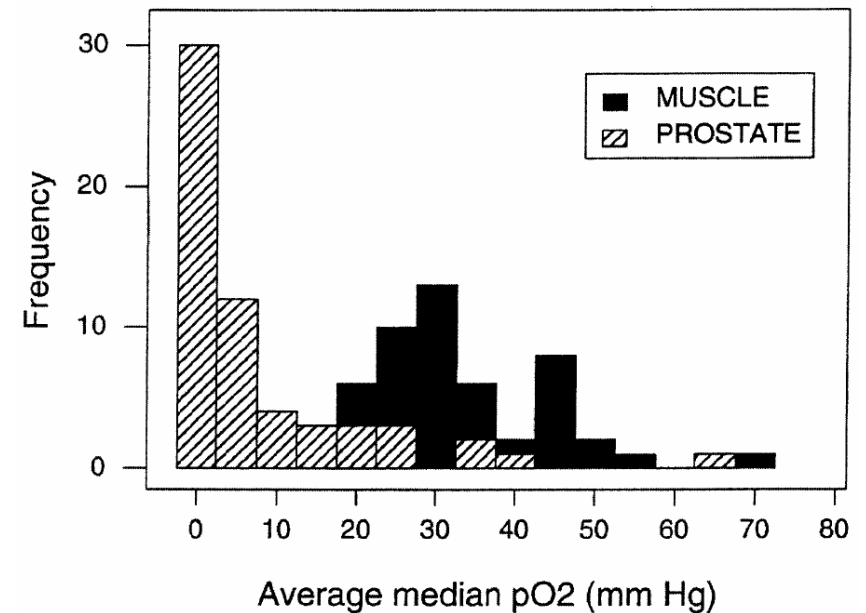


# Critical O<sub>2</sub> Levels

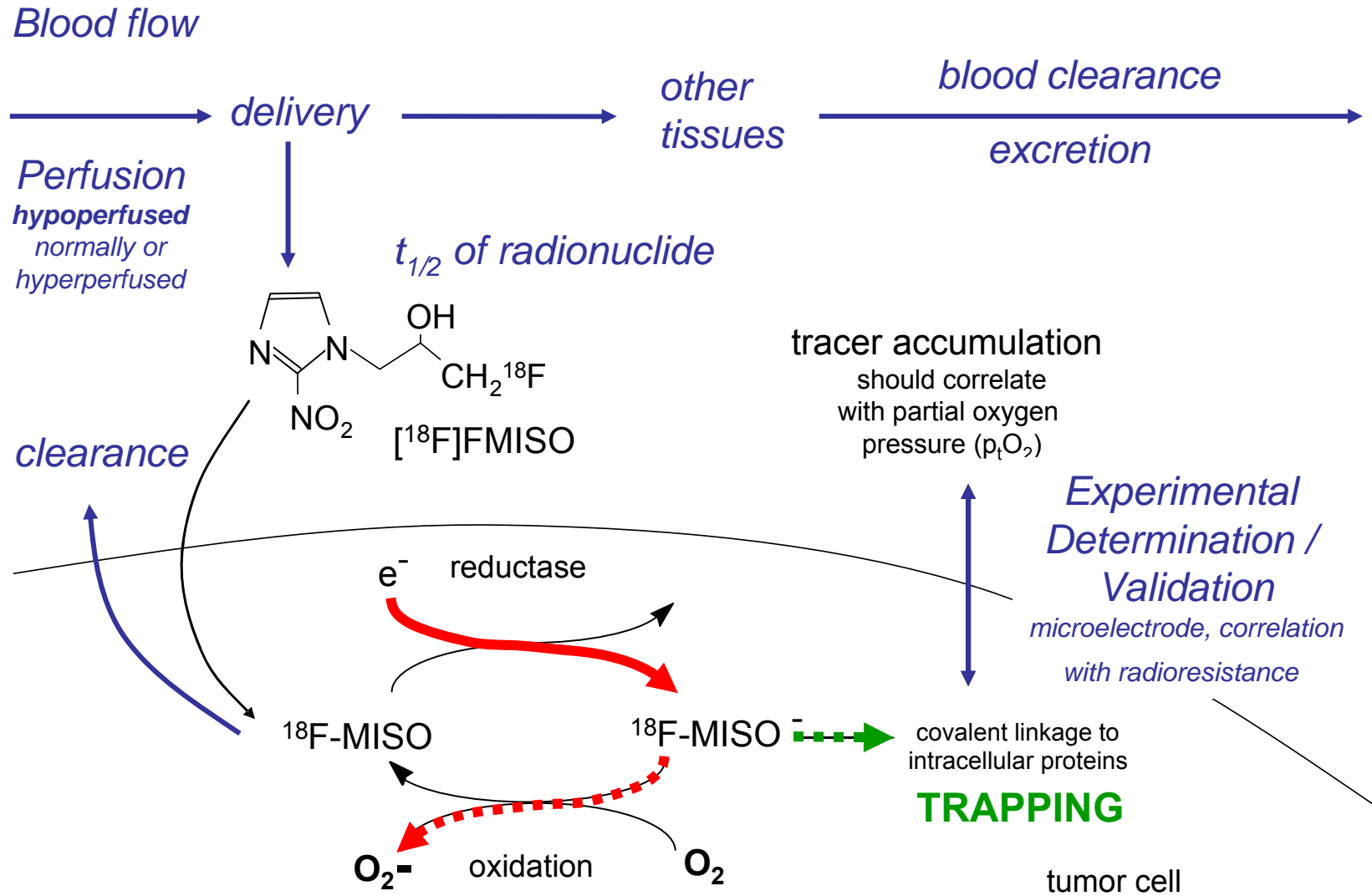
Aggressiveness ↑  
Tumor Progression



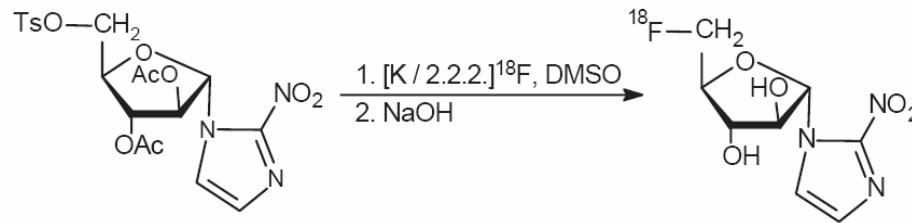
Distribution of medium pO<sub>2</sub> levels for prostatic tumor tissue versus muscle



# The Mechanism of Non-Invasive Detection of Tumor Hypoxia

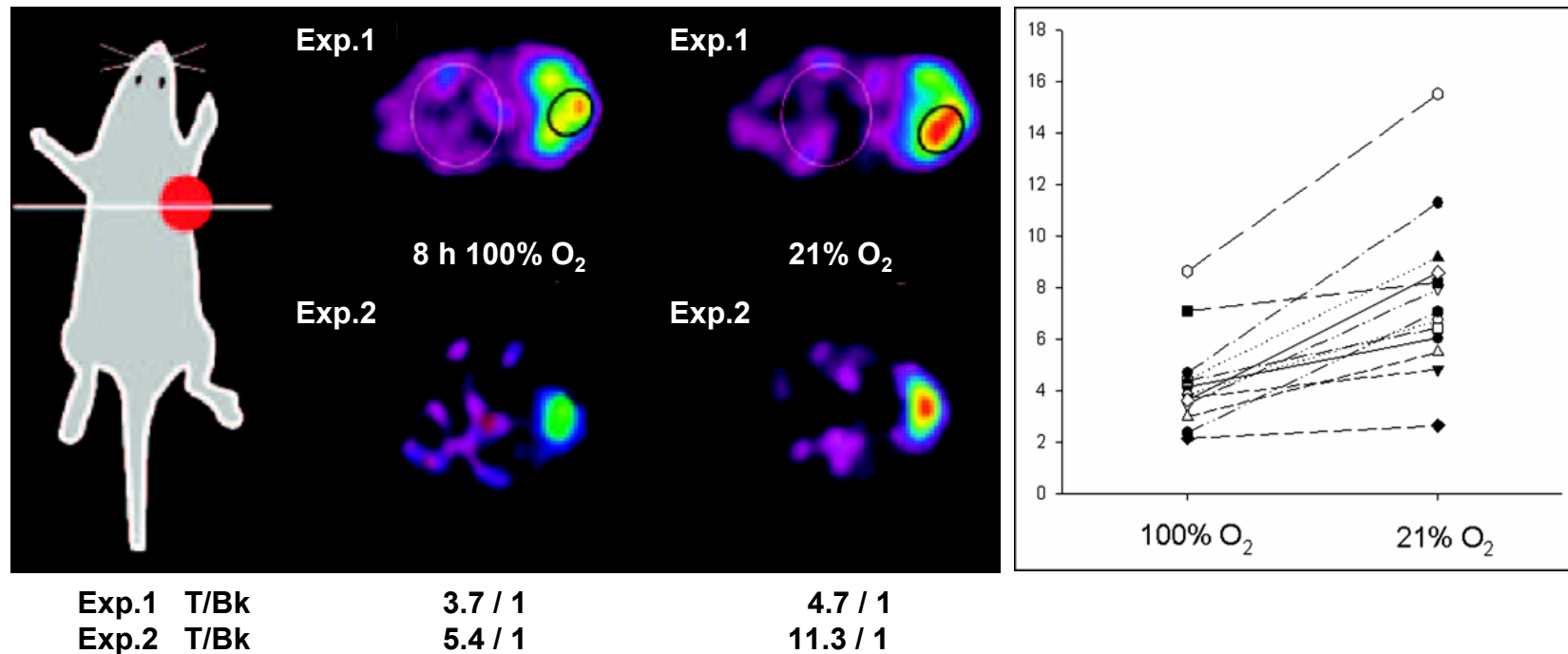


# Evaluation of [<sup>18</sup>F]FAZA

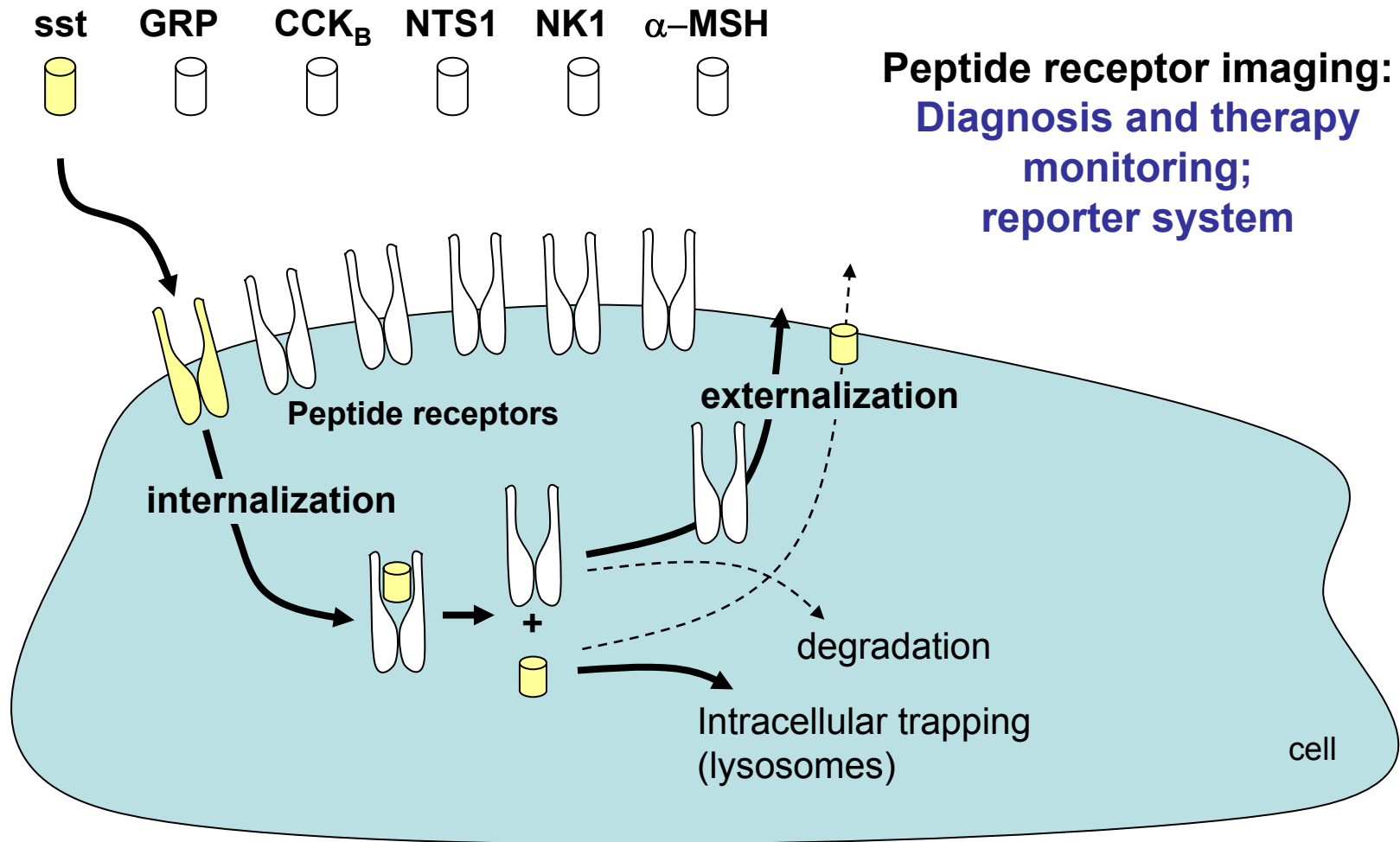


Synthesis of [<sup>18</sup>F]FAZA:  
 Radiochemical Yield: 20 ± 4%, 50 min  
 (Reischl et al., 2005)

Serial, transaxiale PET images -nude mice- with A431 tumors.



# Peptide Receptor Imaging: PRI





## Targets for Radiolabeled Peptides in Human Tumor Tissue

Somatostatin-R

neuroendocrine tumors, small cell lung cancer, medullary thyroid carcinoma, lymphoma (NHL)

Integrins

melanoma, breast tumor, osteosarcoma, glioblastoma

VIP-R

adenocarcinomas, small cell lung cancer, neuroendocrine tumors, lymphoma

CCK-B-R

medullary thyroid carcinoma, small cell lung cancer, stromal ovarian cancer, astrocytoma

Substance P-R

medullary thyroid cancer, small cell lung cancer, breast tumors

Bombesin/ GRP-R

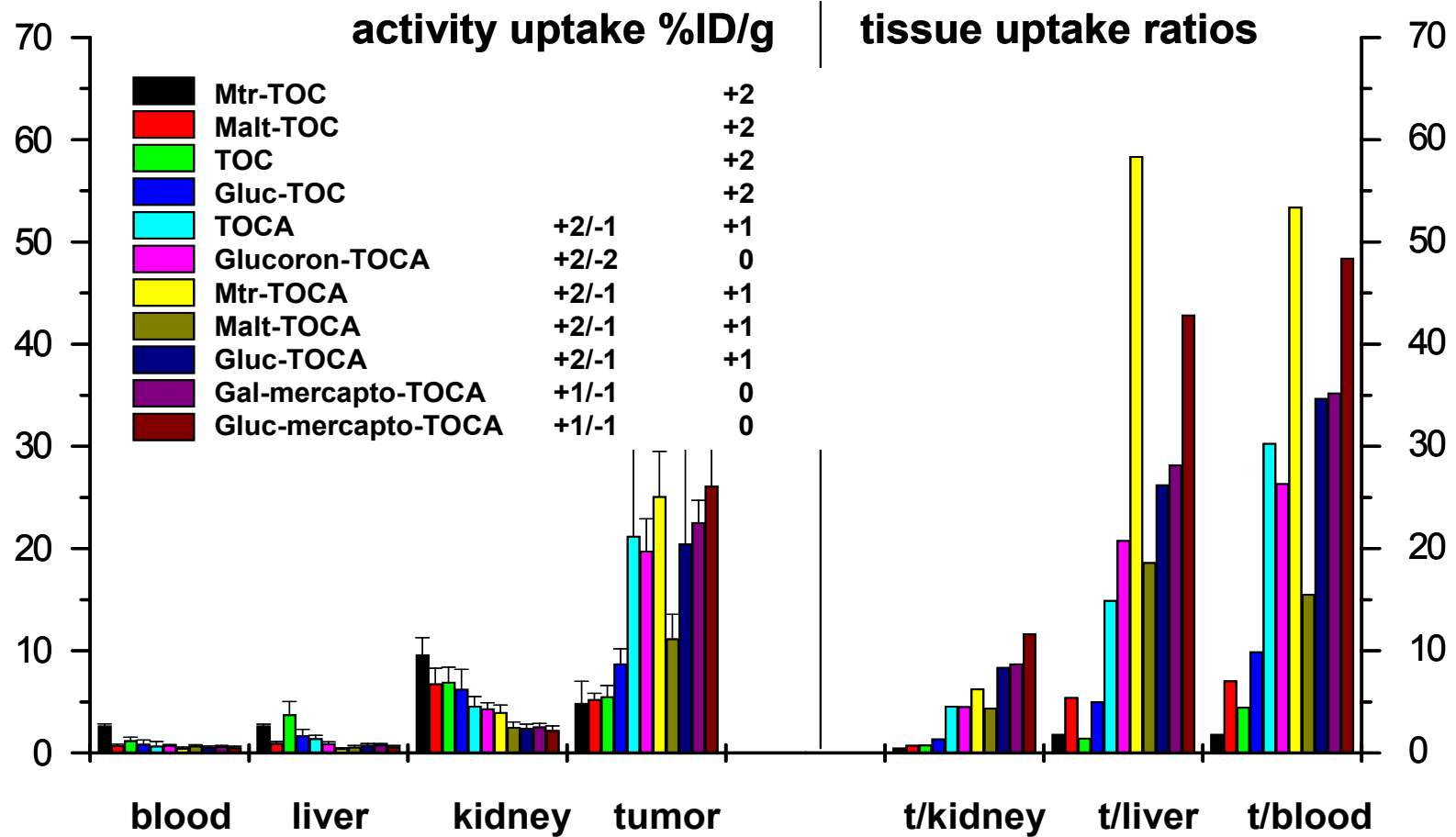
colon cancer, small cell lung cancer, glioblastoma

Neurotensin-R

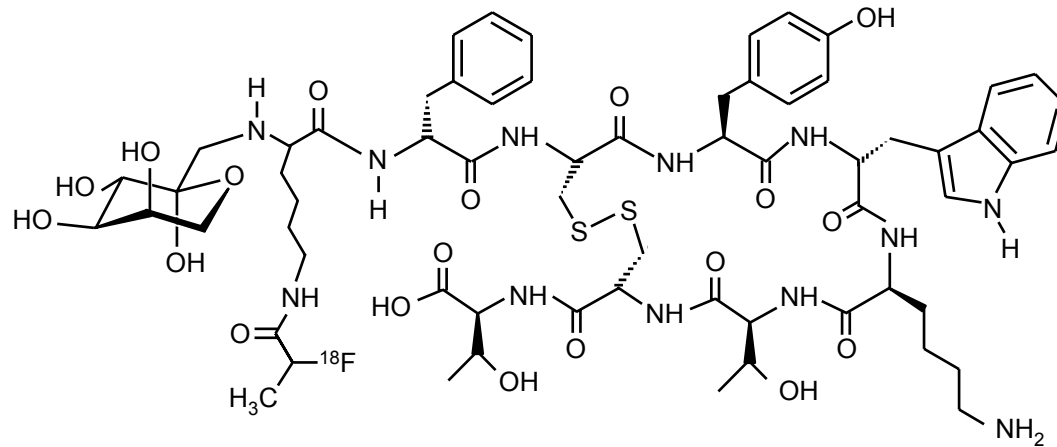
pancreatic cancer, prostate cancer, small cell lung cancer

# Influence of the Carbohydrate on the Biodistribution of Octreotides/-tates

(Mice, AR42J, n=3-5, 60 min p.i.)



# Chemical Structure of Gluc-FP<sup>[18F]</sup>-TOCA

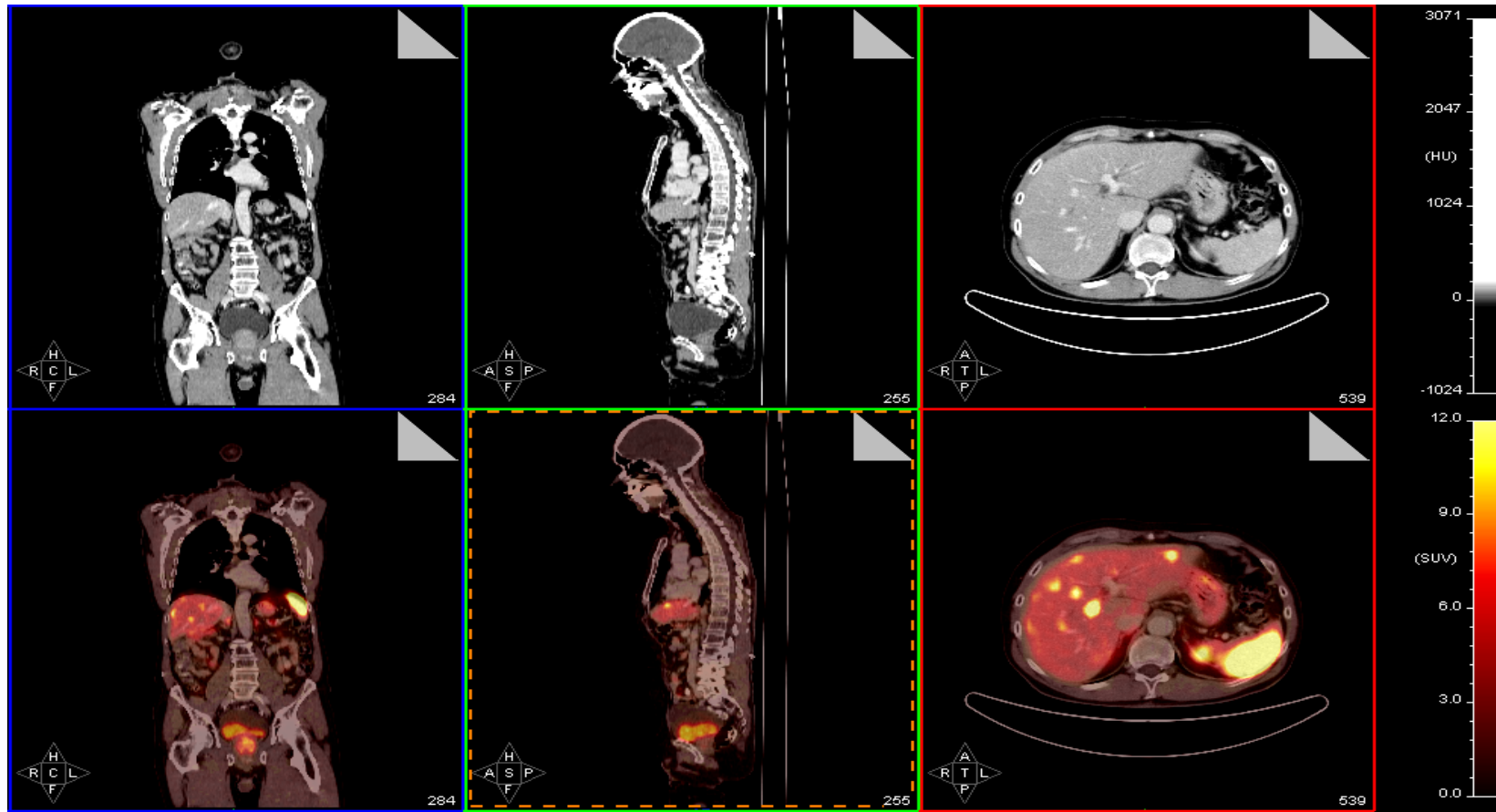


**Gluc-Lys([<sup>18</sup>F]FP)-TOCA**

[<sup>18</sup>F]FP = 2-[<sup>18</sup>F]Fluoropropionic acid

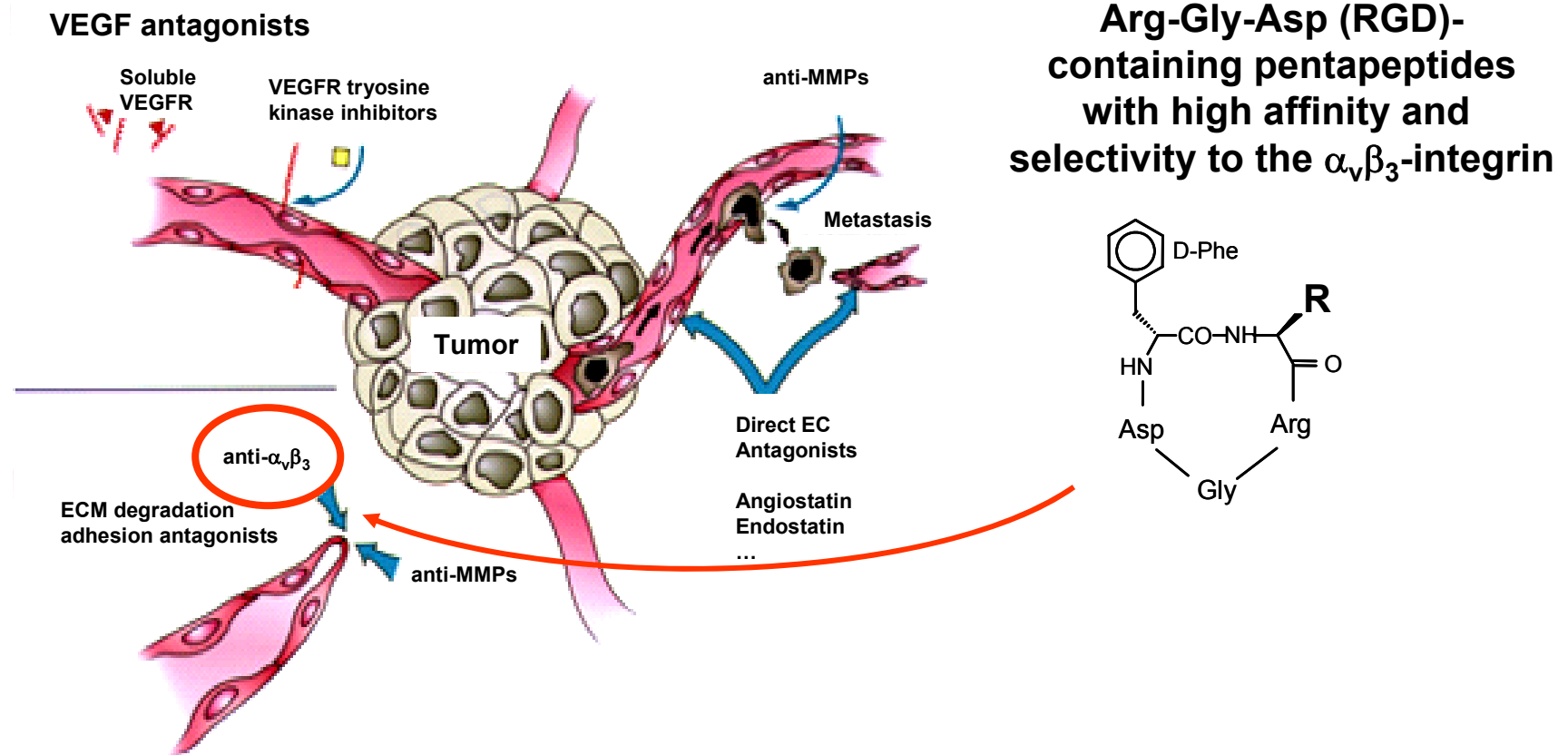
TOCA = Tyr<sub>3</sub>-octreotate, -DPhe-Cys-Tyr-DTrp-Lys-Thr-Cys-Thr-OH

# Gluc-FP[<sup>18</sup>F]-TOCA

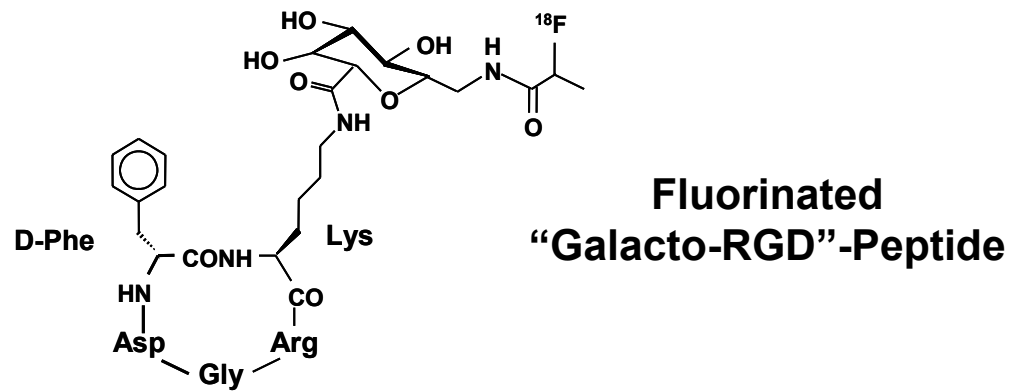


Male patient, 50 yrs, carcinoid with multiple metastases

# Imaging of Neoangiogenesis

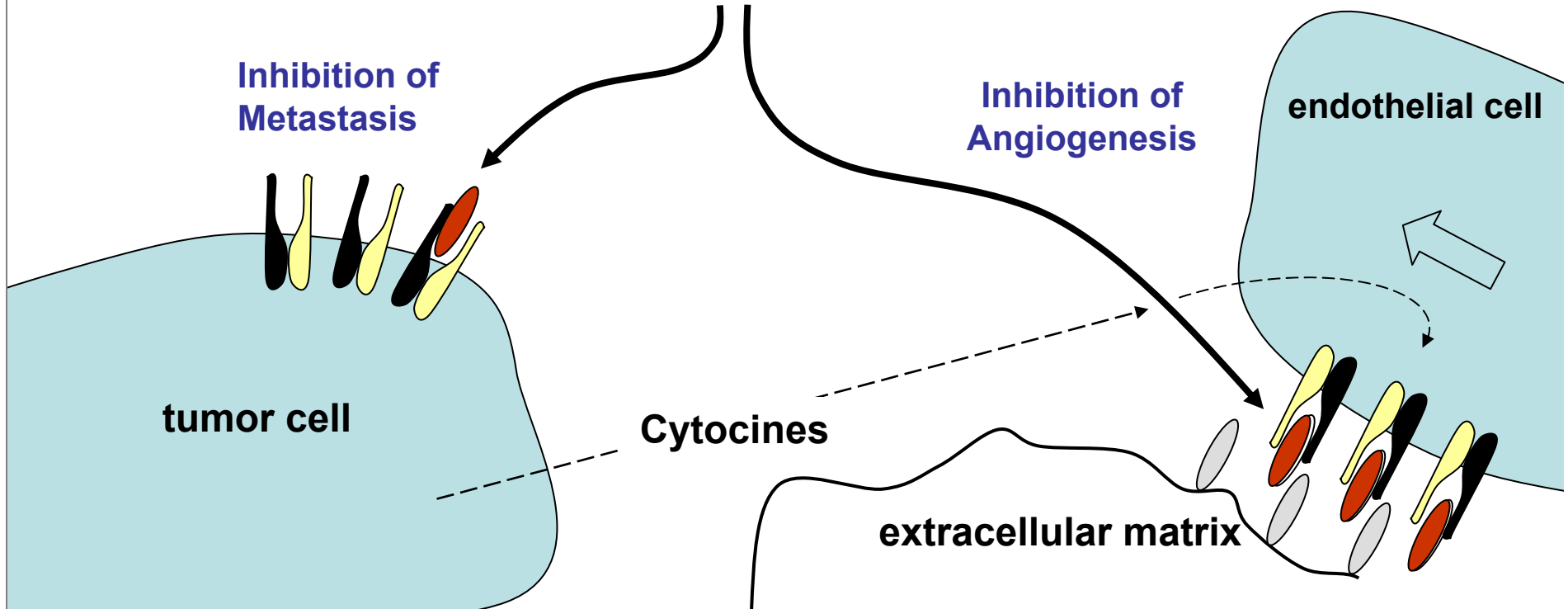


# Carbohydrated RGD-Peptide : [<sup>18</sup>F]Galacto-RGD

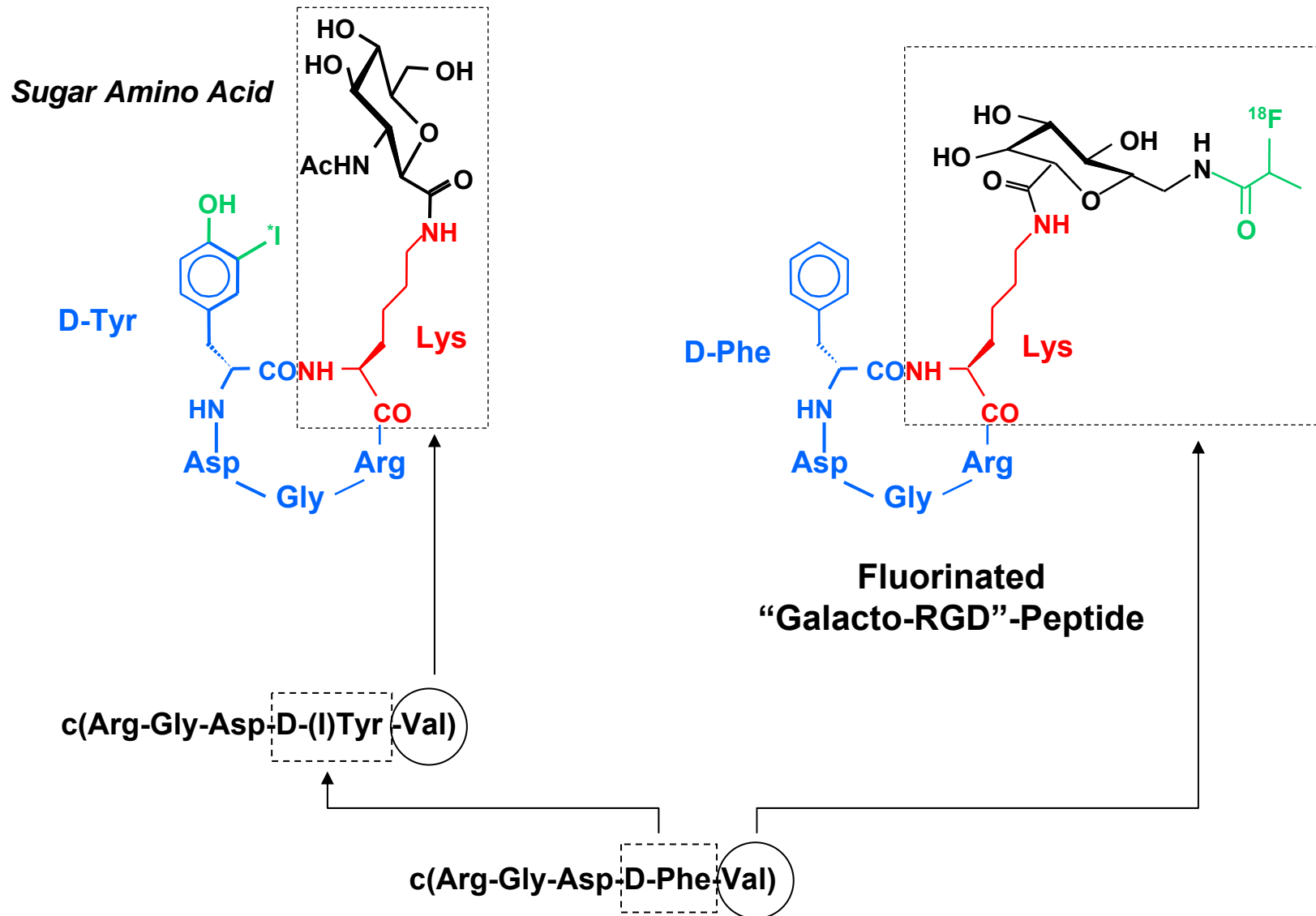


**Inhibition of Metastasis**

**Inhibition of Angiogenesis**

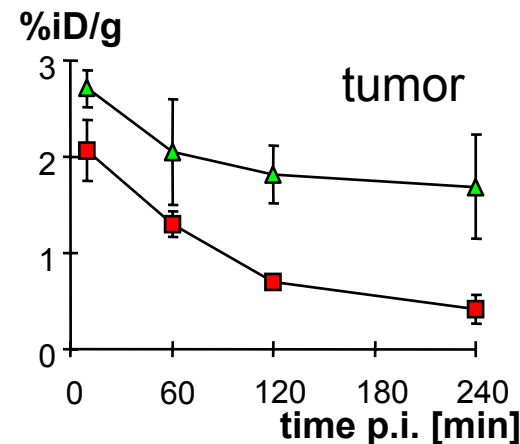
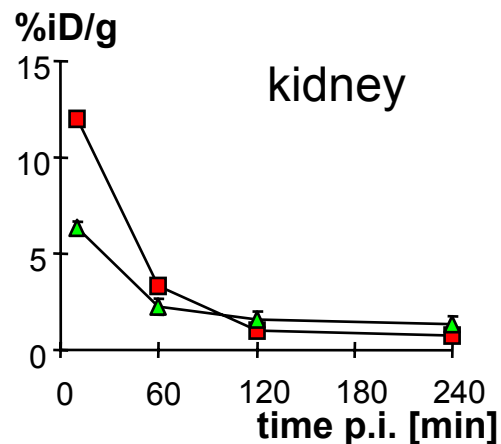
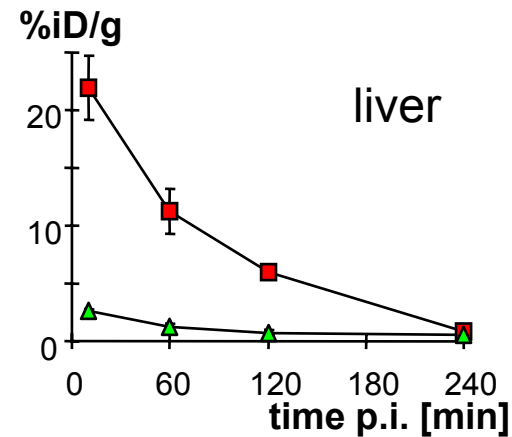
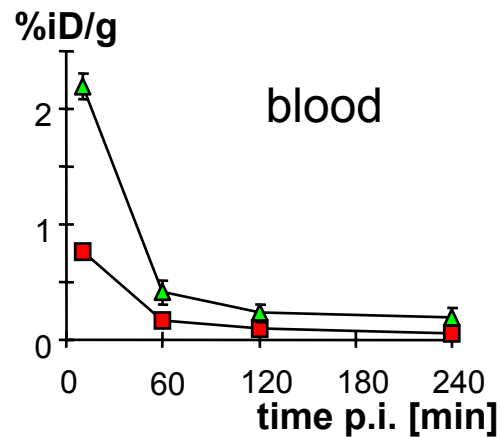


# Carbohydrated RGD-Peptides with Improved Pharmacokinetics



# Comparison of the Pharmacokinetics in Selected Tissues

- *c(Arg-Gly-Asp-D-(l)Tyr -Val)*: **Log P = -1.89**
- ▲ I-Gluco-RGD: **Log P = -2.45**

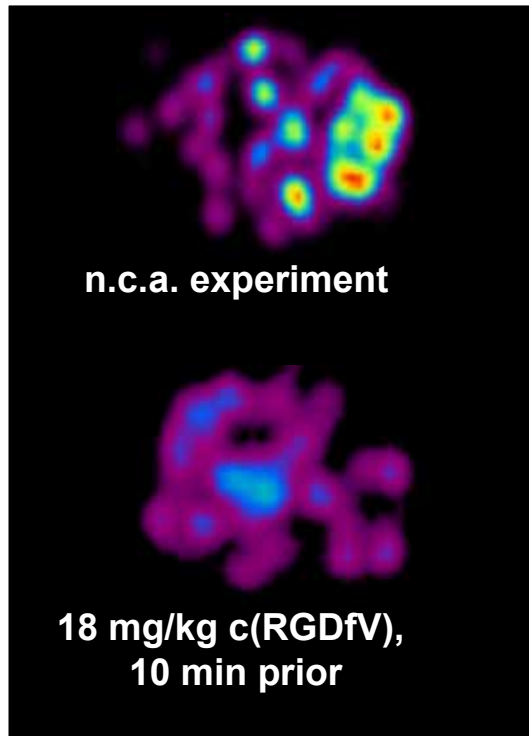


BALB/c mice,  
osteosarcoma model;  
comparable data obtained  
with M21melanoma bearing  
mice

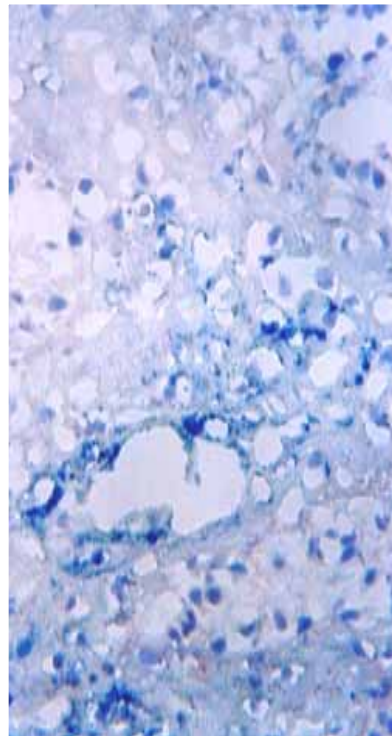
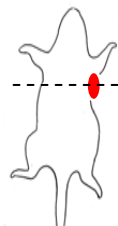


# Non-invasive Monitoring of $\alpha_v\beta_3$ Expression on the Tumor Vasculature

nude mouse bearing a human squamous cell carcinoma at the right shoulder

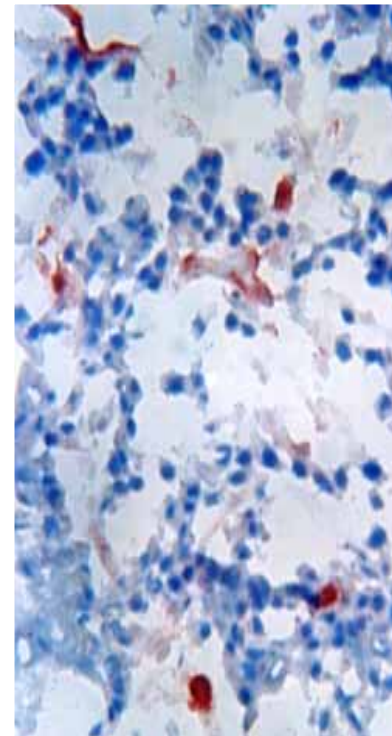


1.5h p.i



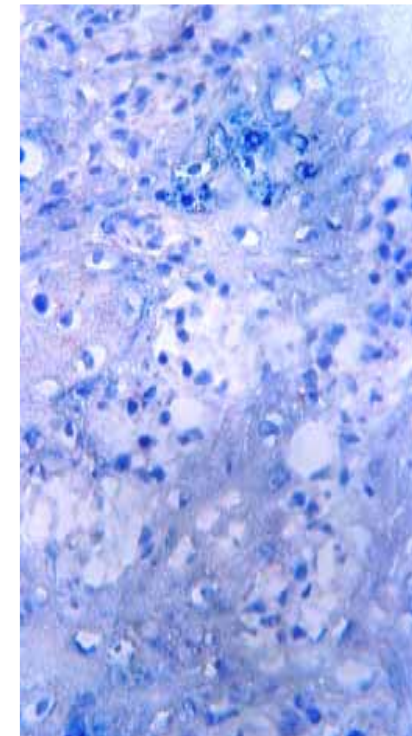
anti human  $\alpha_v\beta_3$   
MAb LM609

no expression  
of  $\alpha_v\beta_3$  on cells



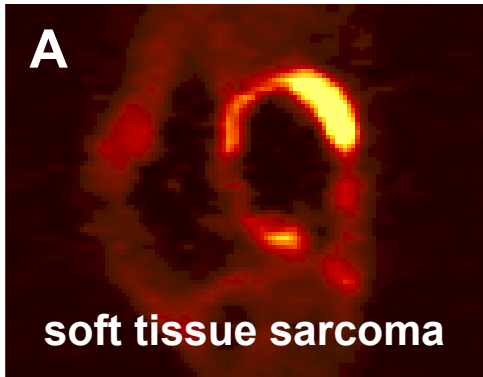
anti murine  $\beta_3$   
MAb 2C9.G2

expression of murine  
 $\beta_3$  on vasculature

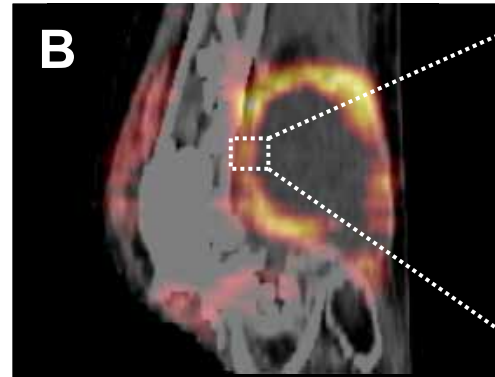


control  
(unspecific MAb)

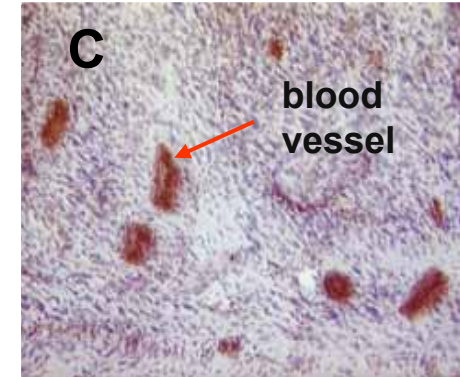
# Determination of $\alpha_v\beta_3$ -Expression in vivo



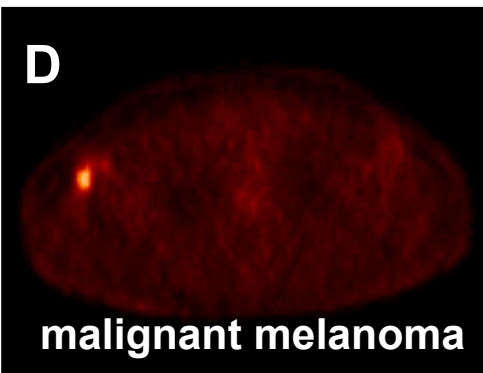
sagittal section, 170 min p.i. ,  
circular tracer uptake,  
max. SUV=10



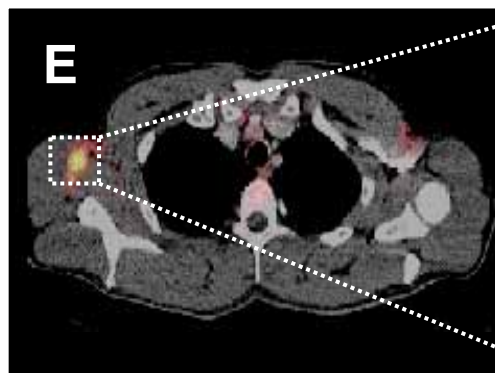
PET/CT image fusion;  
uptake corresponds with  
the tumor-wall



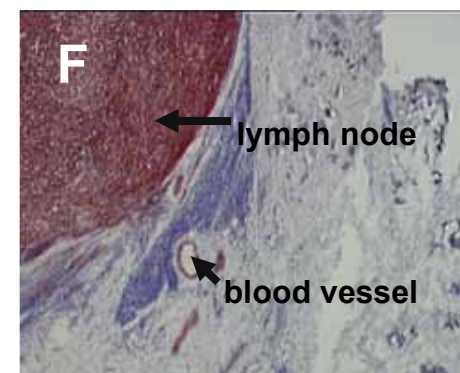
Immunohistochemistry,  
MAb LM609, staining of  
blood vessels



axial section, 140 min p,i,  
uptake in the lymph node

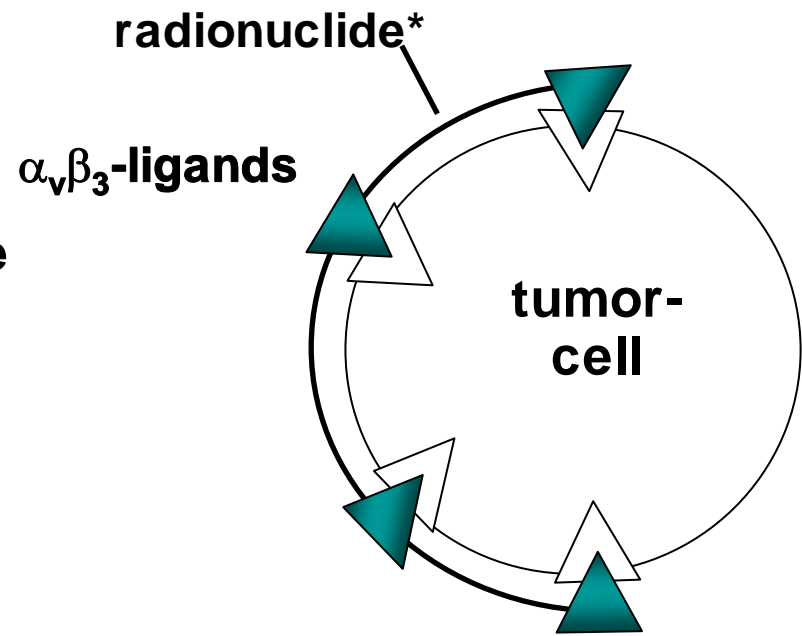
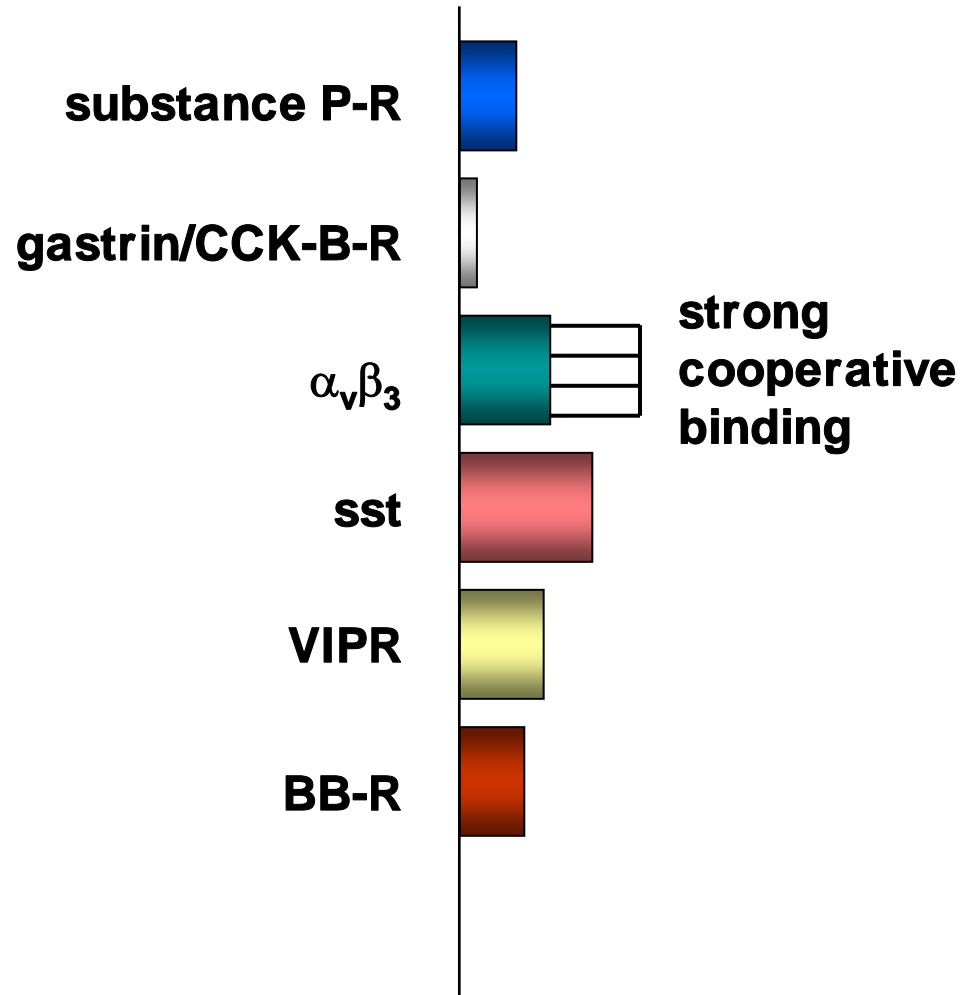


PET/CT image fusion

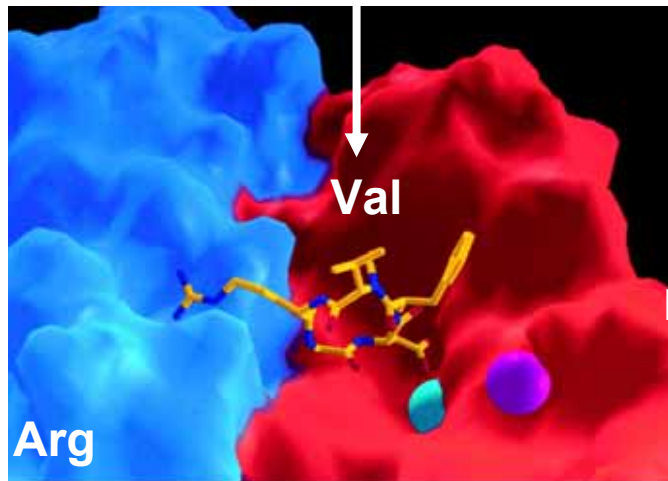


Immunohistochemistry, focal  
MAB LM609, staining of  
tumor cells and blood vessels

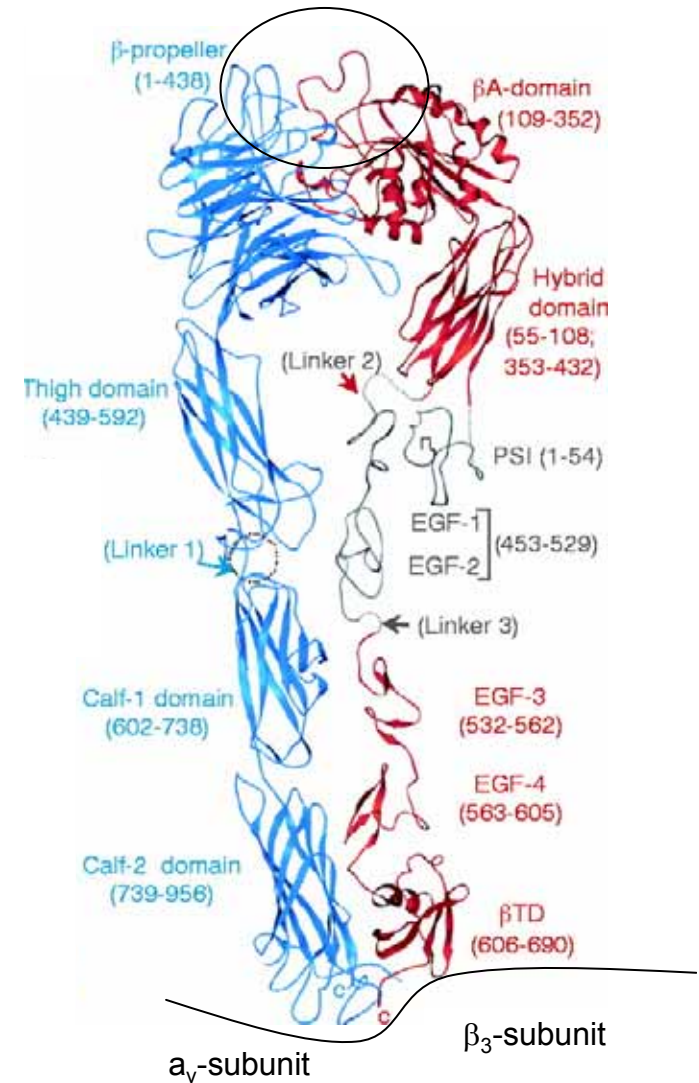
# Multiple-Ligand-Tumortargeting (MLT)



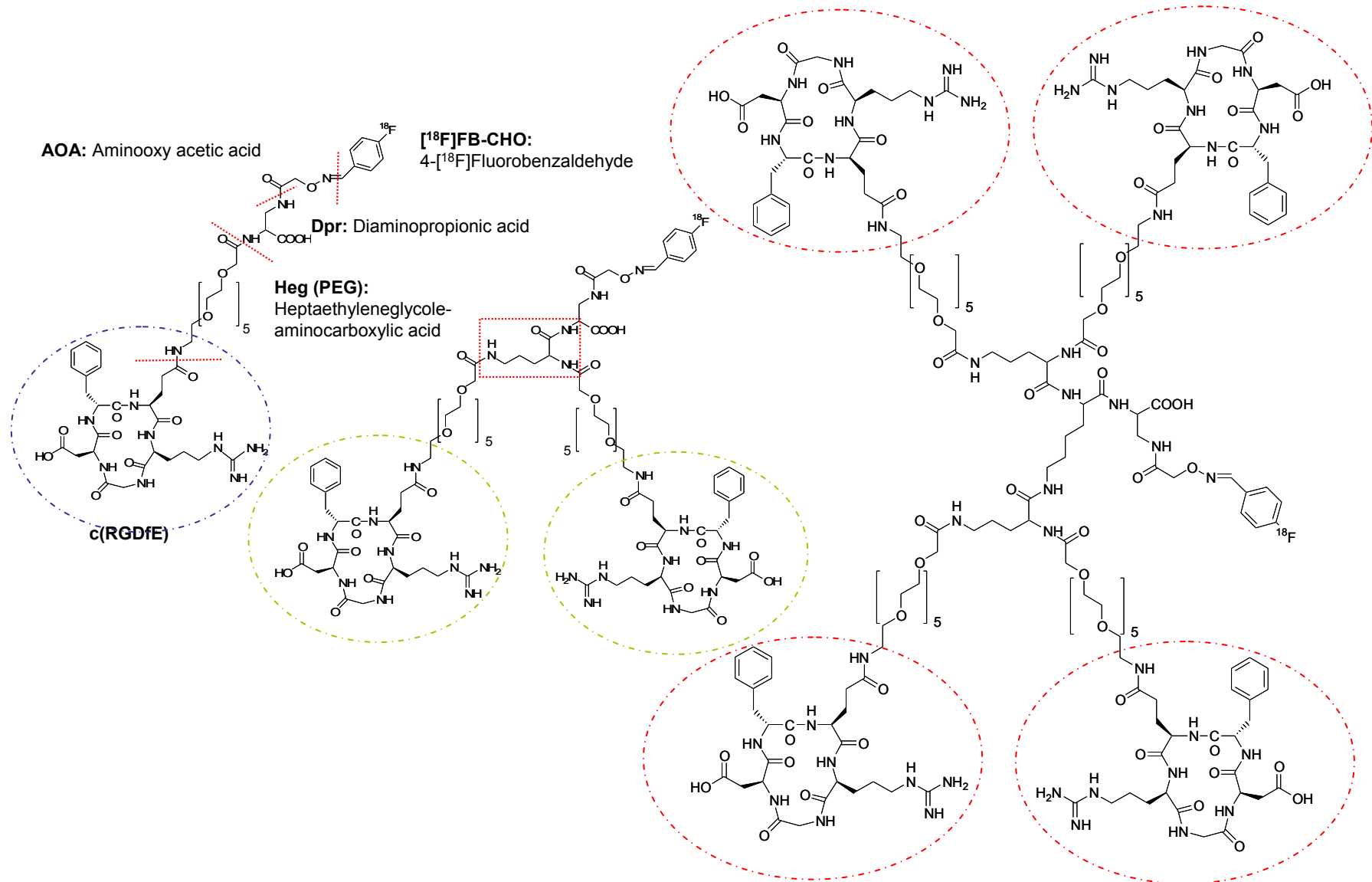
# Structure of the Extracellular Domain of $\alpha_v\beta_3$



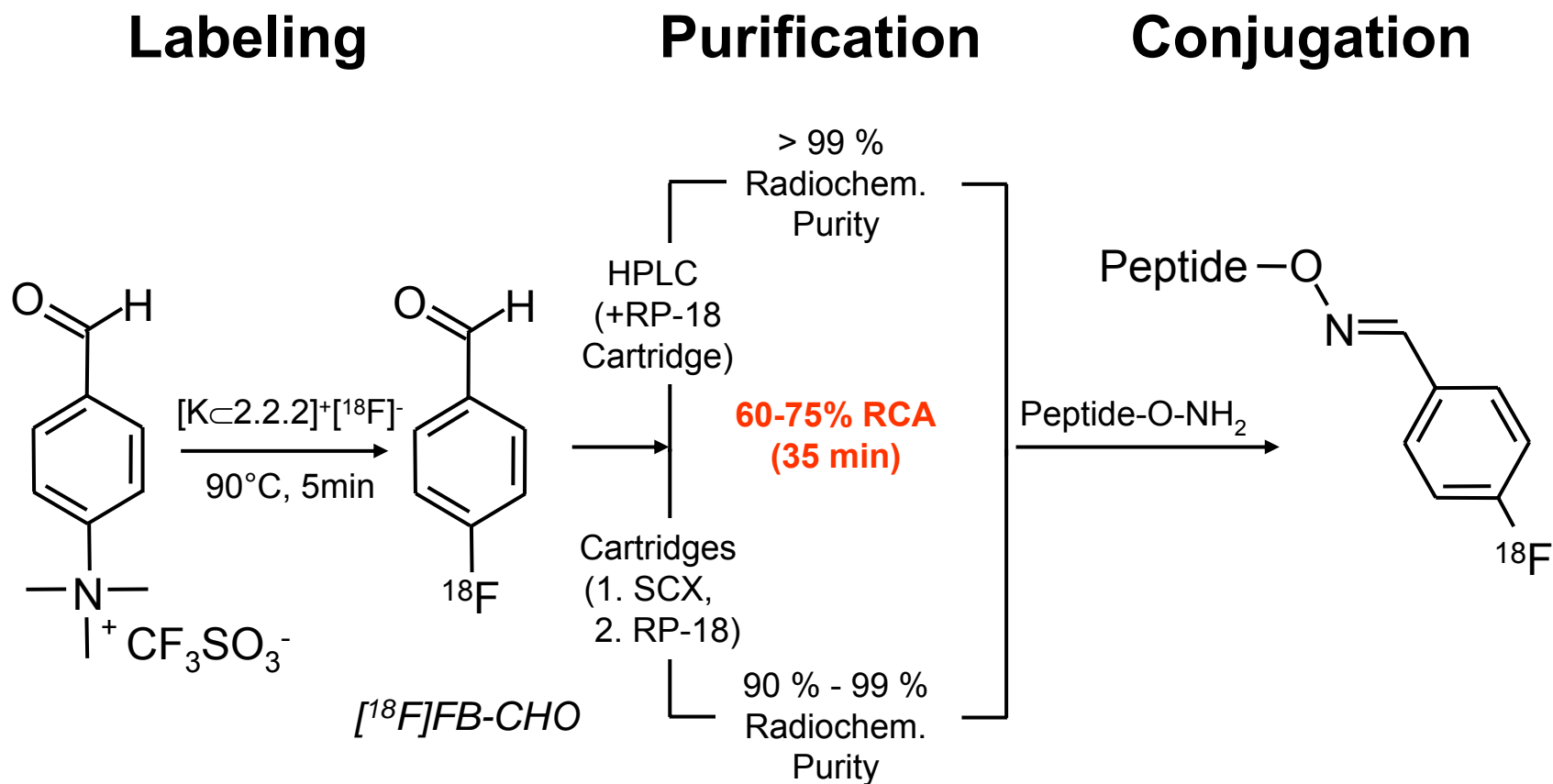
J.-P. Xiong, et. al, Science 2001.



# Multimeric [<sup>18</sup>F]c(RGDfE)-Peptides

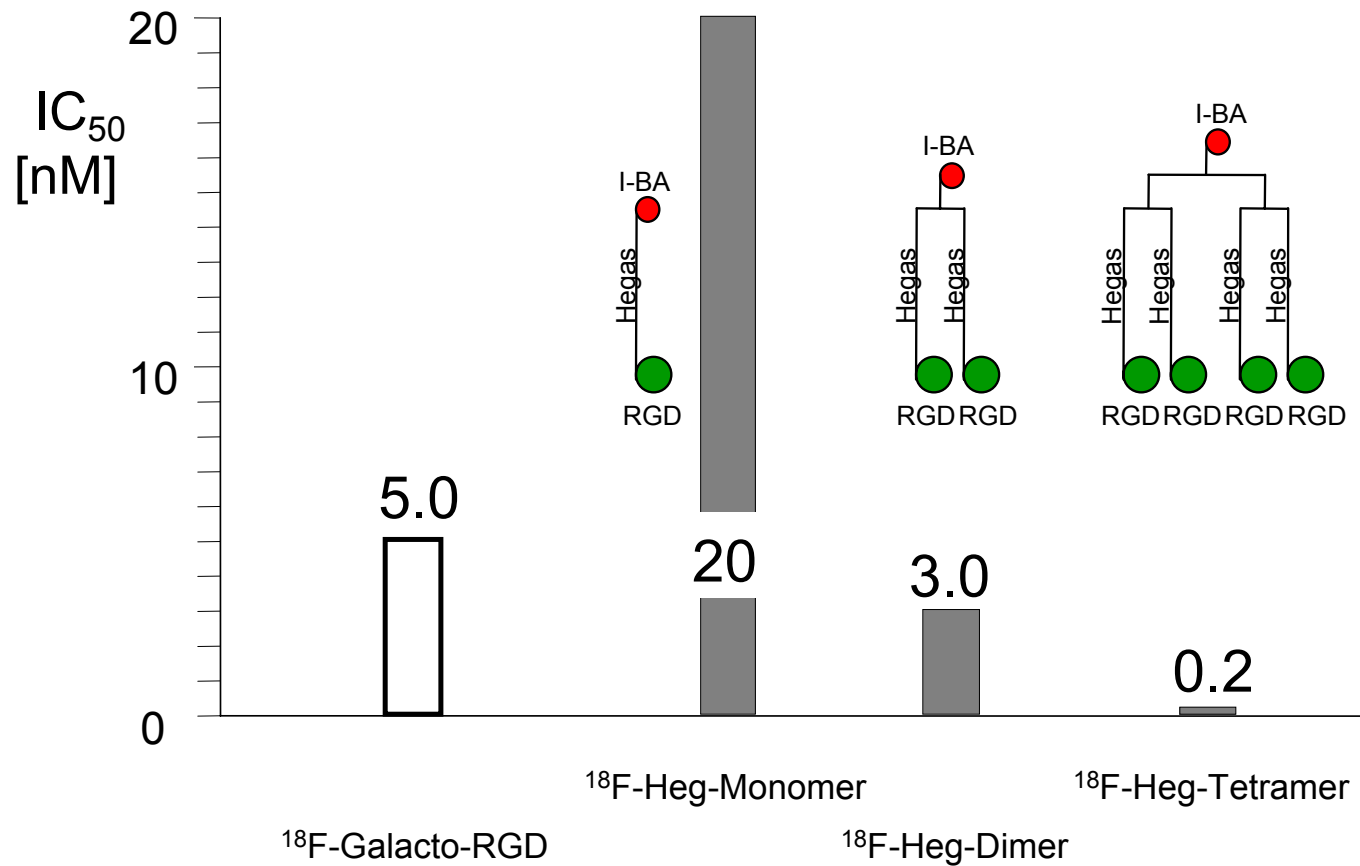


# $^{18}\text{F}$ -Labeling via Oxime Formation



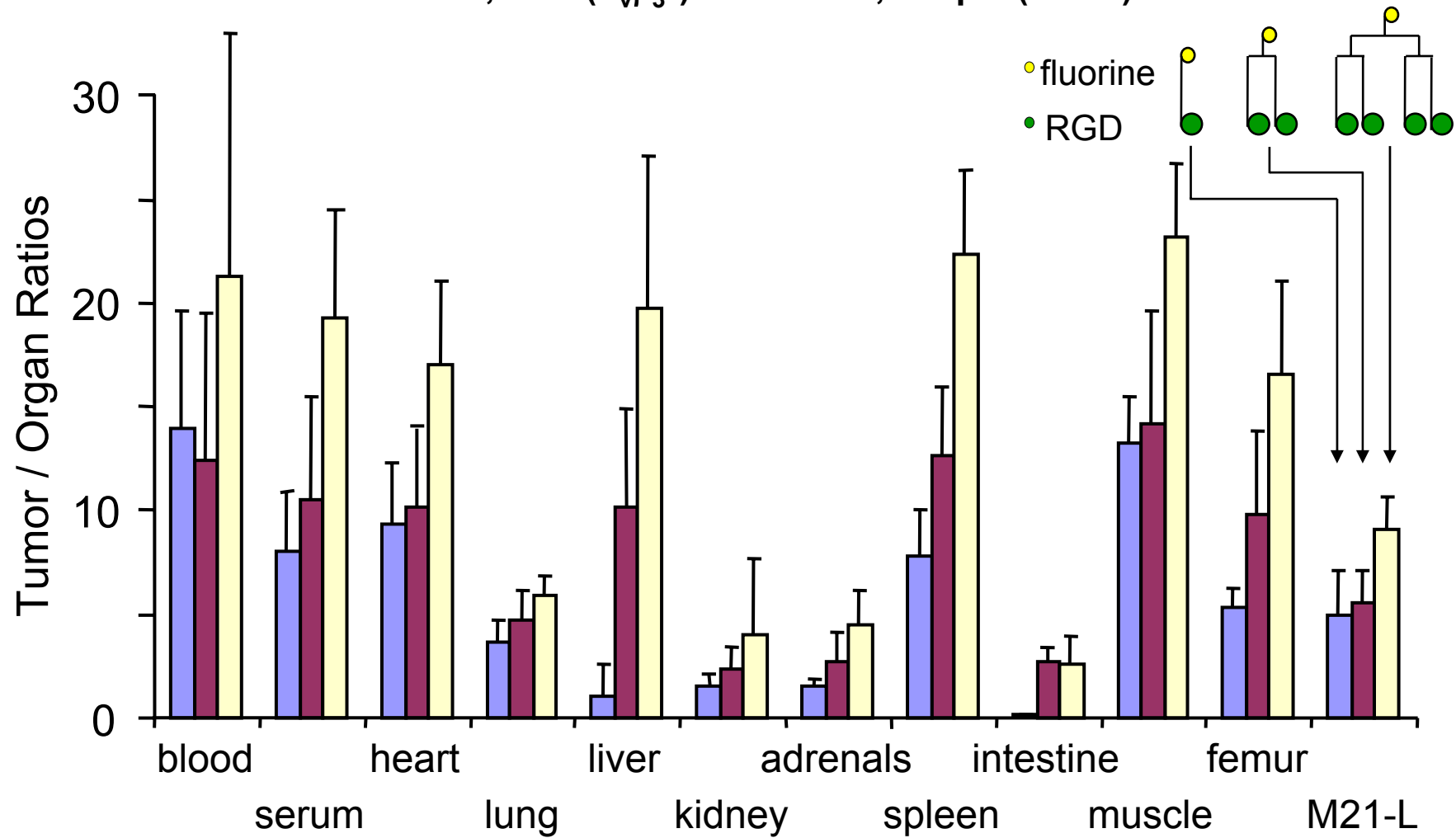
Route suitable for a variety of radiolabeled aldehydes and ketones

# Binding Affinities of Multimeric RGD-Peptide Constructs



# Tumor to Organ Ratios

Nude Mice, M21-( $\alpha_v\beta_3^+$ )-Melanoma, 2 h p.i. (n=3-5)



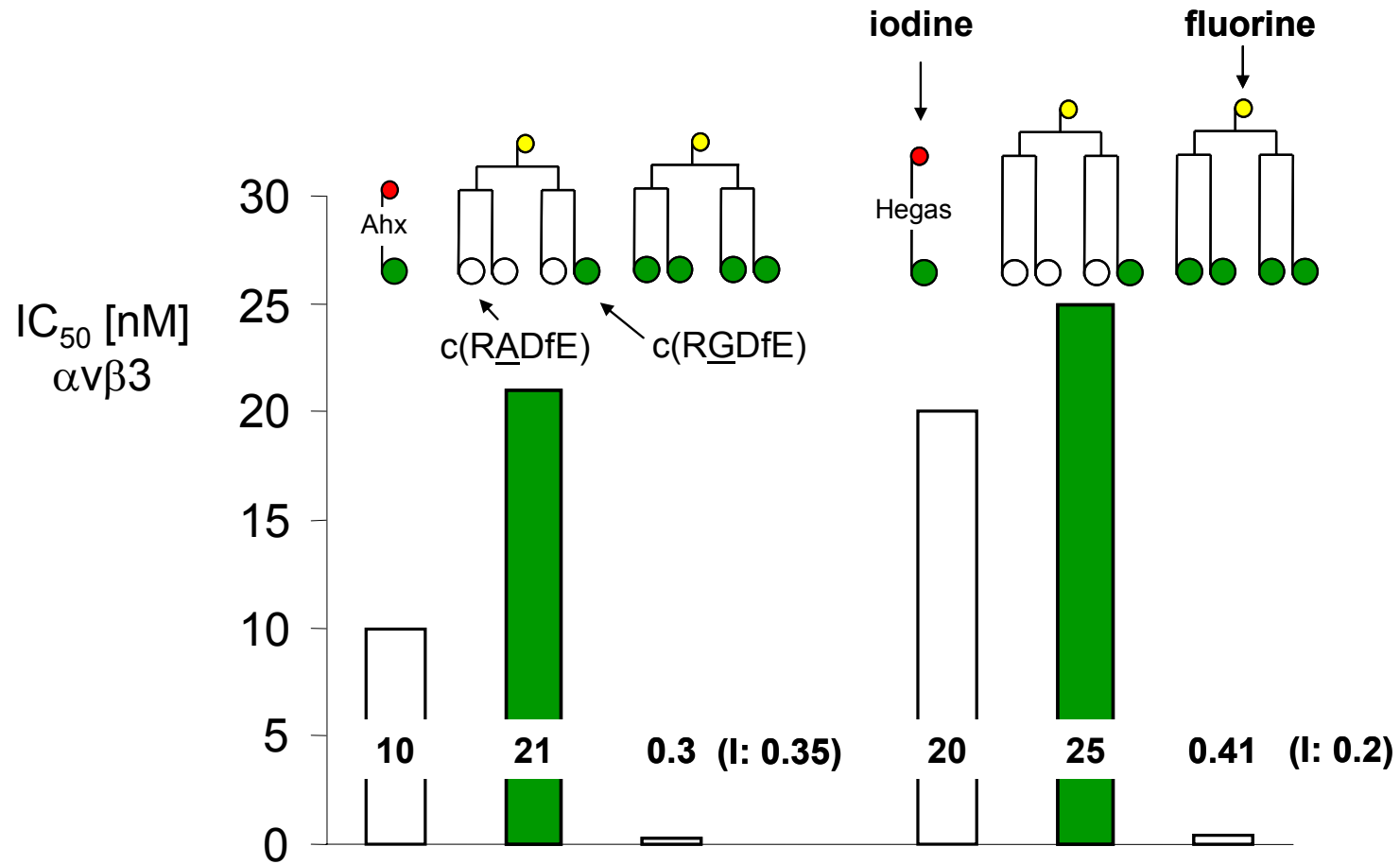


# PET Imaging of [<sup>18</sup>F]RGD-Mono-, Di- and Tetramers

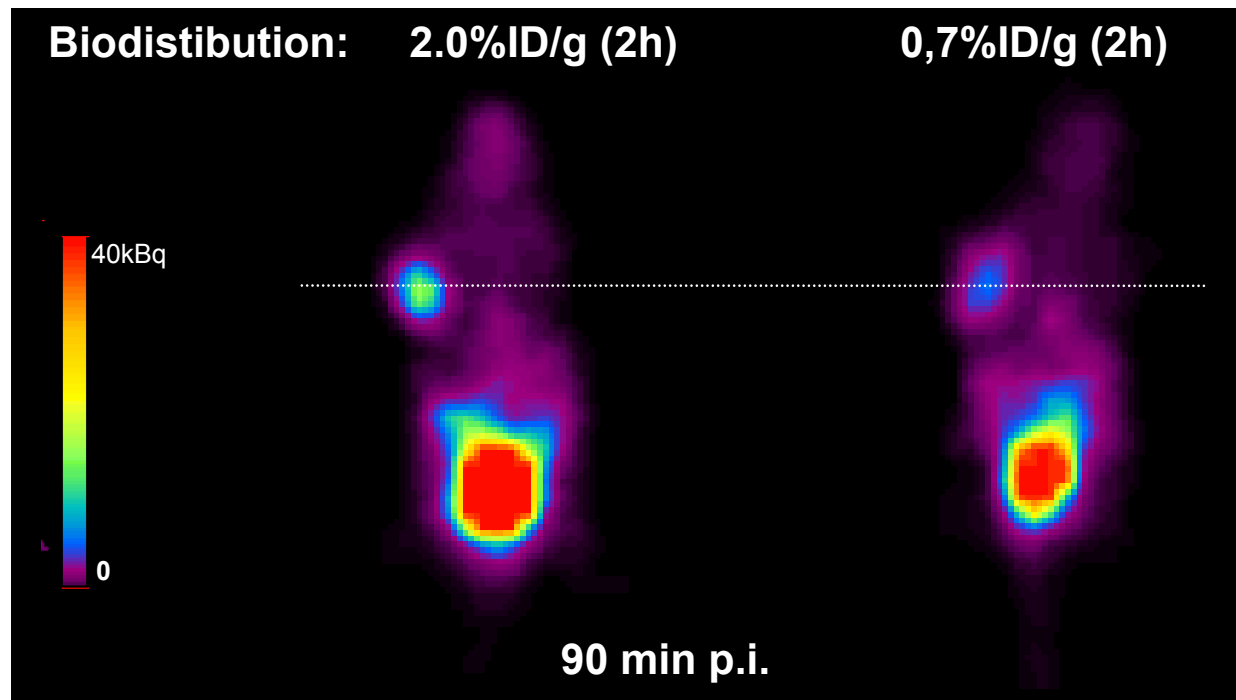
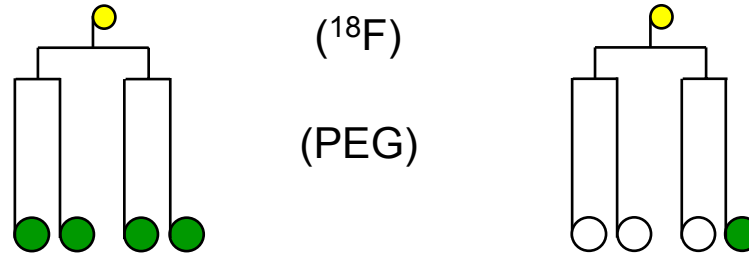


ECAT Exact HR<sup>+</sup>, 90 min p.i.

# Affinities of Multimeric RGD-Peptides with/without RAD-Sequences



# PET Imaging of Tetrameric [<sup>18</sup>F]RGD with and without „Knockout“ Sequences



# Radiopharmaceutical Chemistry and Development of Radiopharmaceuticals

***Triple T***

**Target**

**+ Tracer**

**+ Technology**

---

**= Suitable Radiopharmaceutical  
and Contrast Agent**



# Imaging with PET and SPECT

**Thorsten Poethko**

Nuklearmedizinische Klinik und Poliklinik  
und  
Institut für Radiochemie  
Technische Universität München



# Basics of Radionuclide Production

**Knowledge of production process**

**Purification**

**Recovery of target material**

**Analytical methods (quality control)**

# Radionuclide Production

- (A) **Cyclotron** (ca. 250 world-wide)  
**(Ion accelerator)**
- (B) **Reactor** (ca. 250 Research reactors world-wide)
- 
- (C) **Generators**

# General Aspect

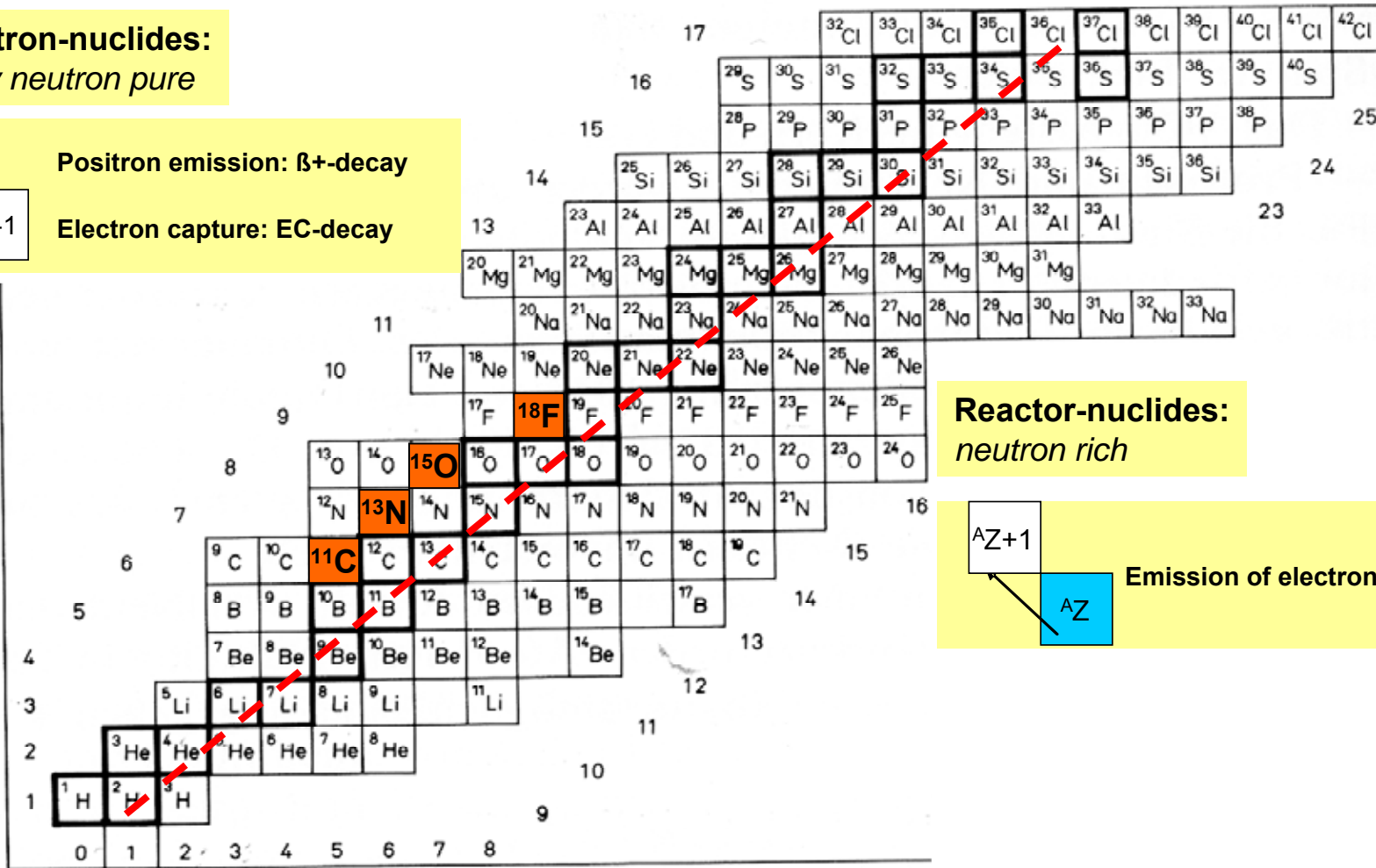
**Cyclotron-nuclides:**  
*mostly neutron pure*

**Positron emission:  $\beta^+$ -decay**

**Electron capture: EC-decay**

A diagram showing a box labeled 'AZ' with an arrow pointing to a box labeled 'AZ-1'.

Proton number  $P = Z$   $\uparrow$



**Reactor-nuclides:**  
*neutron rich*

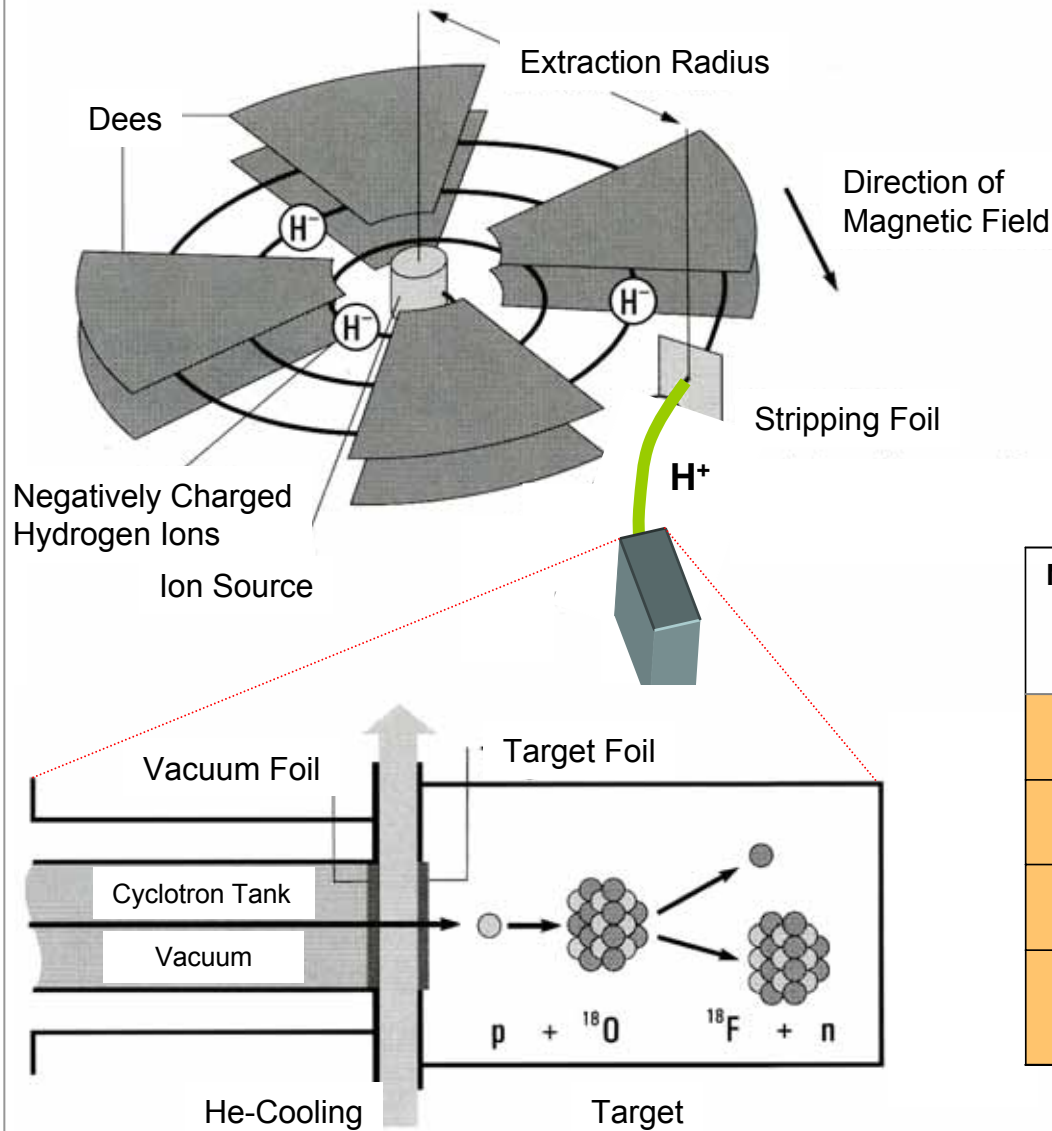
**Emission of electron  $\beta$ -decay**

A diagram showing a box labeled 'AZ' with an arrow pointing to a box labeled 'AZ+1'.

Neutron number  $N = A - Z$   $\rightarrow$



# Production of commonly used PET-Nuclides via Compact Cyclotron



Nuclide	$T_{1/2}$ (min)	Nuclear-Reaction	Energy (MeV)	Mode of decay [%]	Target product
${}^{11}\text{C}$	20.4	${}^{14}\text{N}(p,\alpha)$	$13 \rightarrow 3$	$\beta^+$ (99.8)	${}^{11}\text{CO}_2$ ${}^{11}\text{CO}$
${}^{13}\text{N}$	10.0	${}^{16}\text{O}(p,\alpha)$	$16 \rightarrow 7$	$\beta^+$ (100)	${}^{13}\text{NO}_2^-$ ${}^{13}\text{NO}_3^-$
${}^{15}\text{O}$	2.0	${}^{15}\text{N}(p,n)$	$10 \rightarrow 0$	$\beta^+$ (99.9)	${}^{15}\text{O}_2$
${}^{11}\text{C}$	109.6	${}^{18}\text{O}(p,n)$	$16 \rightarrow 3$	$\beta^+$ (97)	${}^{18}\text{F}_{\text{aq}}^-$ ${}^{18}\text{F}_2$

## Selection of Radionuclide

Half-life comparable with kinetics of physiological process ?  
(too short, too long)

Do the nuclear and physical properties fulfill the special demands ?  
(e.g. pure  $\beta^+$  - Emitter)

Labeling chemistry compatible with targeting ?  
(e.g. metalated CNS-ligands)

Patient dose acceptable ?  
(CNS-ligands: C-11 or F-18)

Nuclide availability ?  
(Generator, cyclotron, energy range)

# PET-Radionuclides

Isotope	Half-life [h]	Positron percentage branching % $\beta^+$	Maximum positron energy [MeV] $E_{\beta^+ \max}$	Intrinsic spacial resolution loss [mm]	Comments
$^{18}\text{F}$	1,8	96,9	0,63	0,7	
$^{55}\text{Co}$	17,5	76	1,50	1,6	$T_{1/2, D} = 2,6 \text{ y}$
$^{61}\text{Cu}$	3,4	61	1,22	1,5	
$^{64}\text{Cu}$	12,7	18	0,65	0,7	
$^{66}\text{Ga}$	9,5	57	4,15	-	
$^{68}\text{Ga}$	1,14	89	1,90	2,4	G: $^{68}\text{Ge} / 271\text{d}$
$^{75}\text{Br}$	1,6	71	1,72	2,2	$T_{1/2, D} = 120 \text{ d}$
$^{76}\text{Br}$	16,2	54	3,94	5,3	
$^{86}\text{Y}$	14,7	33	3,14	1,8	
$^{110\text{m}}\text{In}$	1,15	62	2,20	3,0	G: $^{110}\text{Sn} / 4,1 \text{ h}$
$^{120\text{g}}\text{I}$	1,35	56	4,59	5,4	
$^{124}\text{I}$	100,3	23	2,14	2,3	

# Resolution Limitation due to Positron Energy

**$^{18}\text{F}$**

$\langle\beta^+\rangle = 0,242 \text{ MeV}$

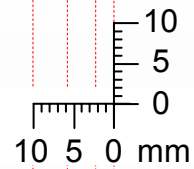
**$^{15}\text{O}$**

$\langle\beta^+\rangle = 0,735 \text{ MeV}$

**$^{82}\text{Rb}$**

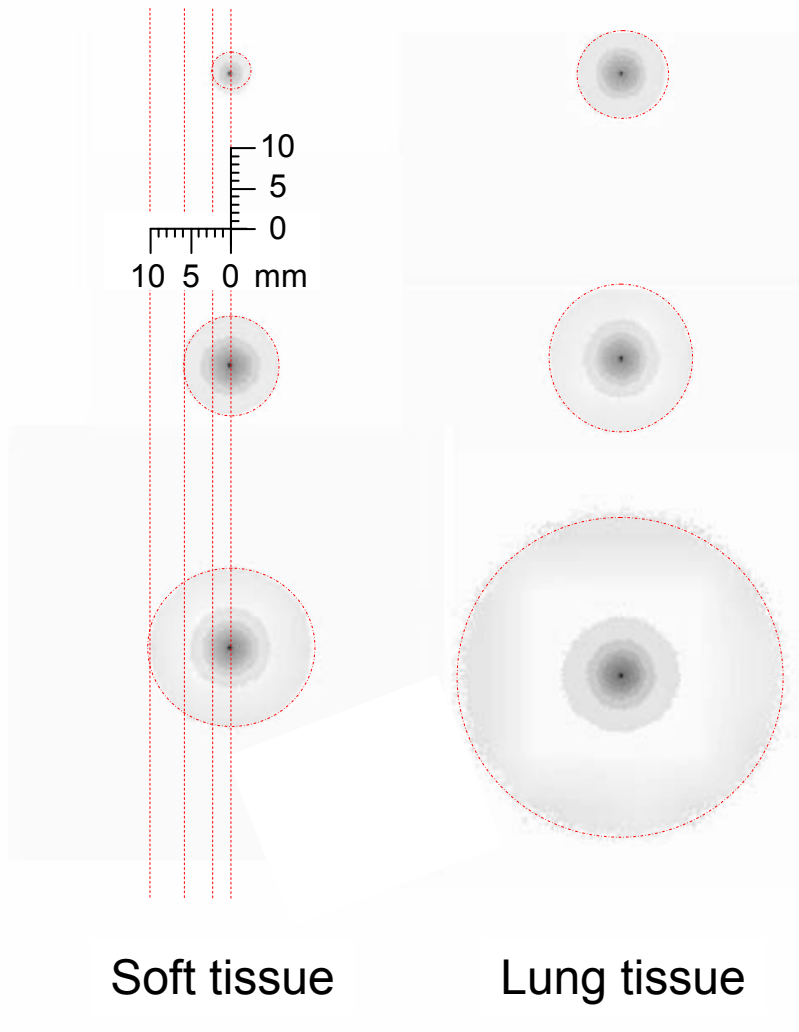
$\langle\beta^+\rangle = 1.409 \text{ MeV}$

Compact bone

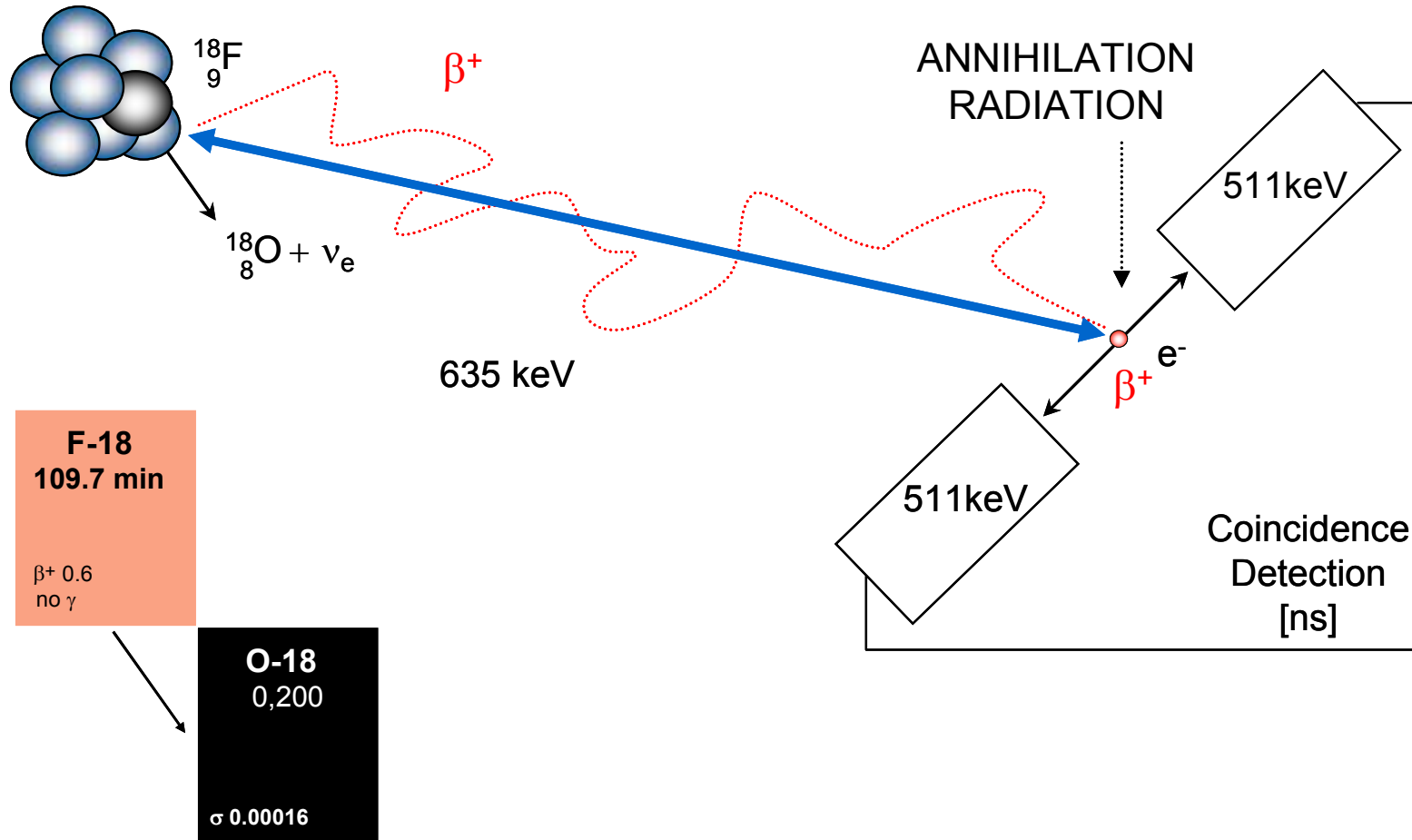


Soft tissue

Lung tissue



# Positron-Emission



## Production of F-18

Nuclear reaction	$^{18}\text{O}(p,n)^{18}\text{F}$	$^{16}\text{O}(^3\text{He},n)^{18}\text{F}$	$^{20}\text{Ne}(d,\alpha)^{18}\text{F}$	$^{18}\text{O}(p,n)^{18}\text{F}$
Target	$\text{H}_2^{18}\text{O}$	$\text{H}_2\text{O}$	Ne (0.1-0.2% $\text{F}_2$ , 18 bar)	$^{18}\text{O}_2$ (20 bar) (2. + 0.1% $\text{F}_2$ )
Energy range of bombarding particle [MeV]	16 → 0	36 → 0	11.2 → 0	10 → 0
Chemical form	$[^{18}\text{F}]\text{F}_{\text{aq}}^-$	$[^{18}\text{F}]\text{F}_{\text{aq}}^-$	$[^{18}\text{F}]\text{F}_2$	$[^{18}\text{F}]\text{F}_2$
Thick target yield [MBq $\mu\text{A}^{-1} \text{h}^{-1}$ ]	2.200	250	350-450	~350
Specific activity [TBq $\text{mmol}^{-1}$ ]	$40 \times 10^3$	$40 \times 10^3$	0.04–0.4	0.04-2

- **Mainly produced via  $^{18}\text{O}(p,n)^{18}\text{F}$ -reaction**
- **Product:**  $^{18}\text{F}_{\text{aq}}^-$  with high specific activity and up to 100% radiochemical yield, compared to  $[^{18}\text{F}]\text{F}_2$  with low specific activity and max. 50% radiochemical yield

# $^{18}\text{F}$ -Fluoride Chemistry

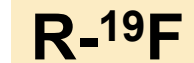
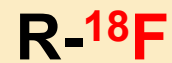
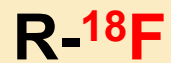
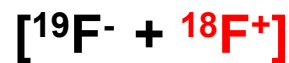
## Nucleophilic Substitution

## Electrophilic Substitution



Non-diluted  
with unlabeled  
tracer  
=  
„No-carrier-added“  
(n.c.a)

diluted  
with unlabeled  
fluorine  
=  
„carrier-added“  
(c.a)



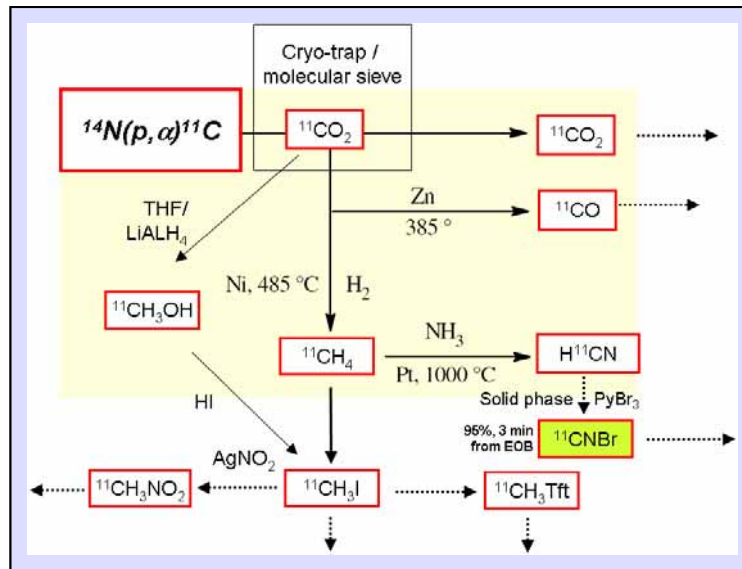
z.B.  $[^{18}\text{F}]\text{Fluor-Choline}$

z.B.  $[^{18}\text{F}]\text{Dopa}$

Only for targets with  
high capacity  
(e.g. enzym  
substrates);  
not suitable saturable  
processes (e.g.  
peptide-receptor-  
ligands)

# Production Scheme: Radiopharmaceutical Production

## Cyclotron und on-line synthesis



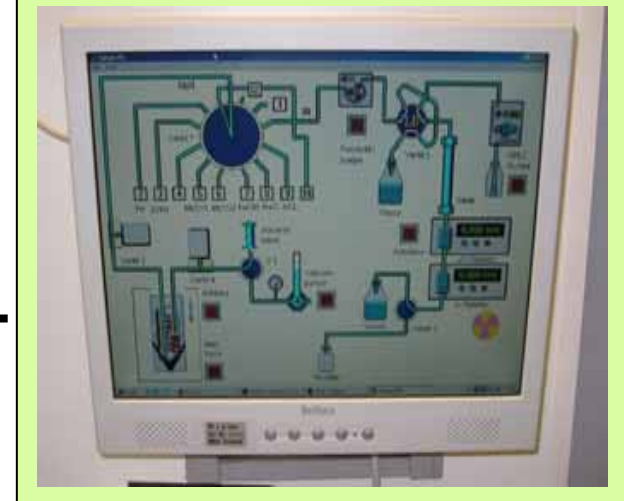
## Automatic production



## Quality control

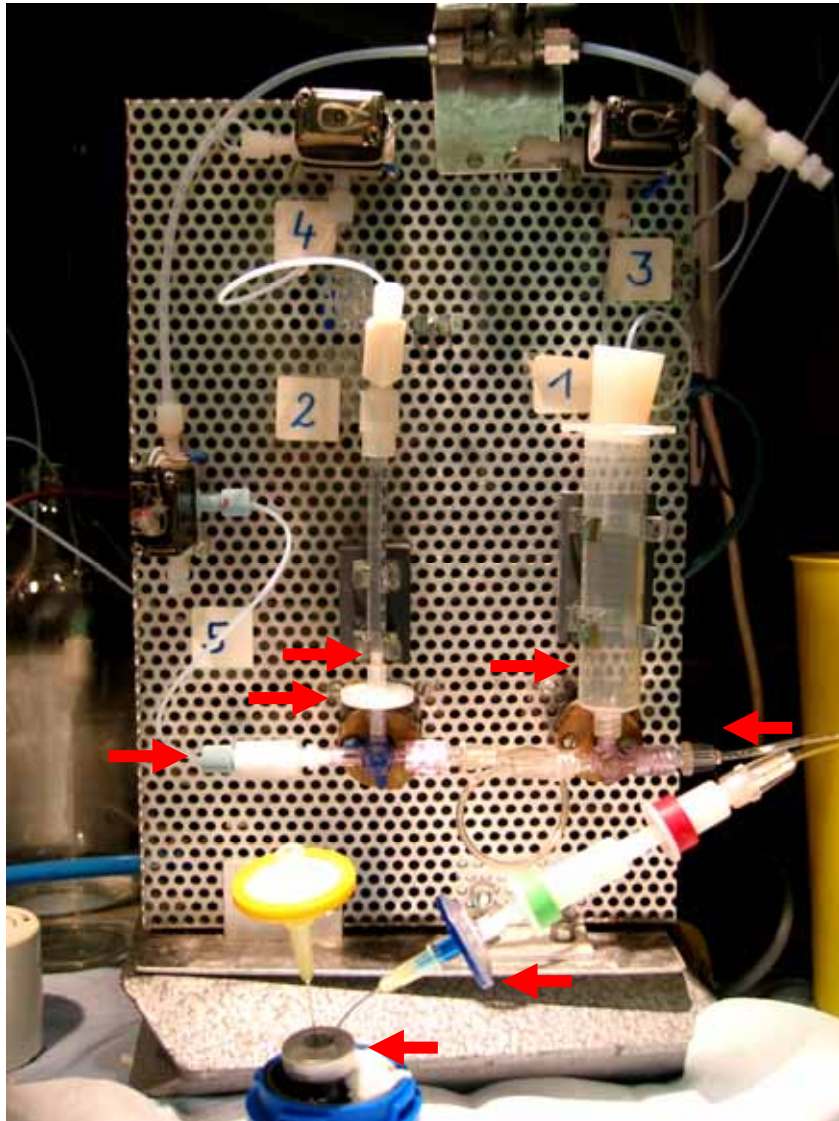


## Application

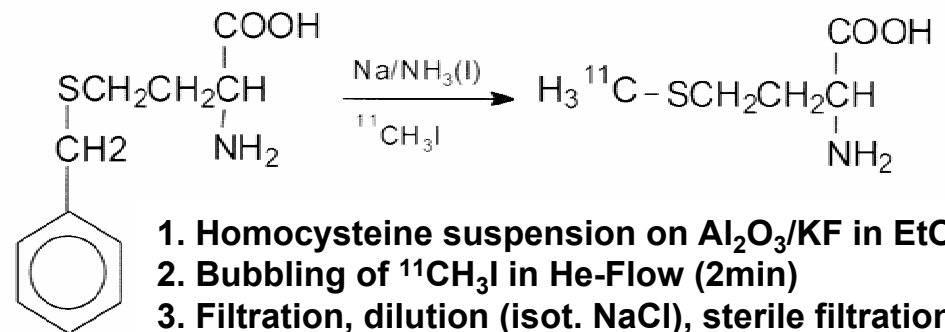




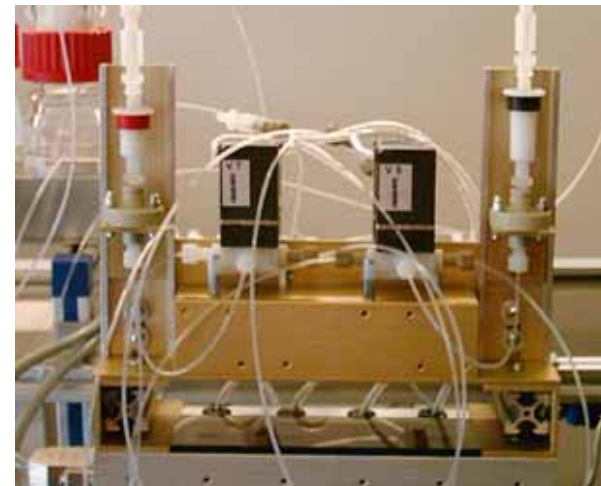
# Automatic Synthesis



## $^{11}\text{C}$ -Methionine Production



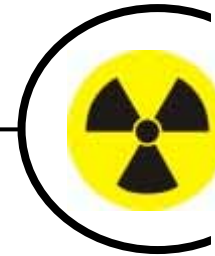
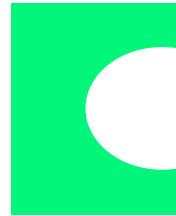
1. Homocysteine suspension on  $\text{Al}_2\text{O}_3/\text{KF}$  in EtOH
2. Bubbling of  $^{11}\text{CH}_3\text{I}$  in He-Flow (2min)
3. Filtration, dilution (isot. NaCl), sterile filtration



## Generators for Positron Emission

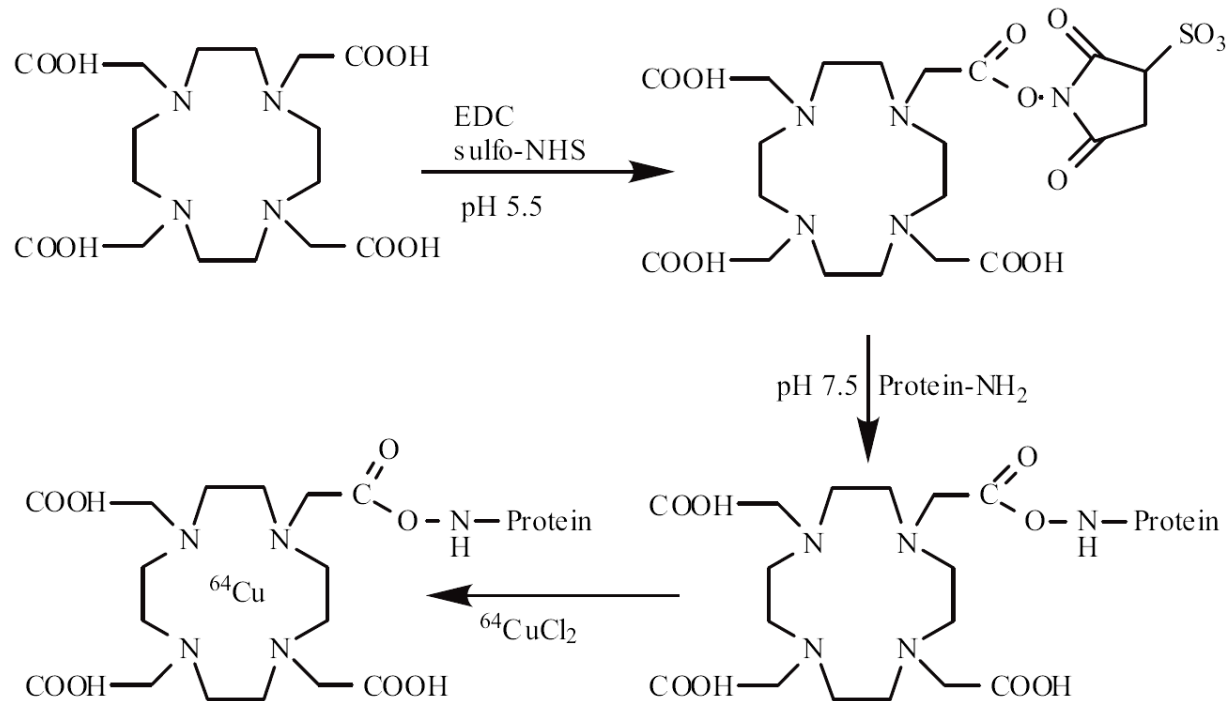
Isotope	Half-life	Mode of decay	$E_{\beta^+}$ [keV]
$^{68}\text{Ge}$	271 d	EC (100%)	
↓			
$^{68}\text{Ga}$	68 min	$\beta^+$ (90%), EC (10%)	1900
$^{62}\text{Zn}$	9.2 h	$\beta^+$ (93%), EC (7%)	660
↓			
$^{62}\text{Cu}$	9.7 min	$\beta^+$ (98%), EC(2%)	2930
$^{82}\text{Sr}$	25 d	EC (100%)	
↓			
$^{82}\text{Rb}$	1.3 min	$\beta^+$ (96%), EC (4%)	3350

# Structure of „non-isotopic“ Radiopharmaceuticals



<b>Address, Target</b>	<b>Pharmacophor, biospecific binding</b>	<b>Spacer, Linker</b>	<b>Labeling, Label</b>
Intra-/Extracellular Receptors Transporter Enzyme Antigens RNA ...	Small org. Molecules Peptidomimetics Peptide Protein Antibody Complex (Ions)	Metabolic stabile Metabolic labile Enzymatic cleavable Hydrolytic sensitive pH sensitive	Covalent Complex Statically distributed Defined bondage No-carrier-added Carrier-added

# Peptide, Protein and Macromolecule Labeling with Radiometals



In, Ga, Cu ...

Lu, Y, Bi, Ac ...

Fe, Gd, .....

# Radionuclide Production for SPECT

SPECT = Single-Photon-Emission-Computer Tomography

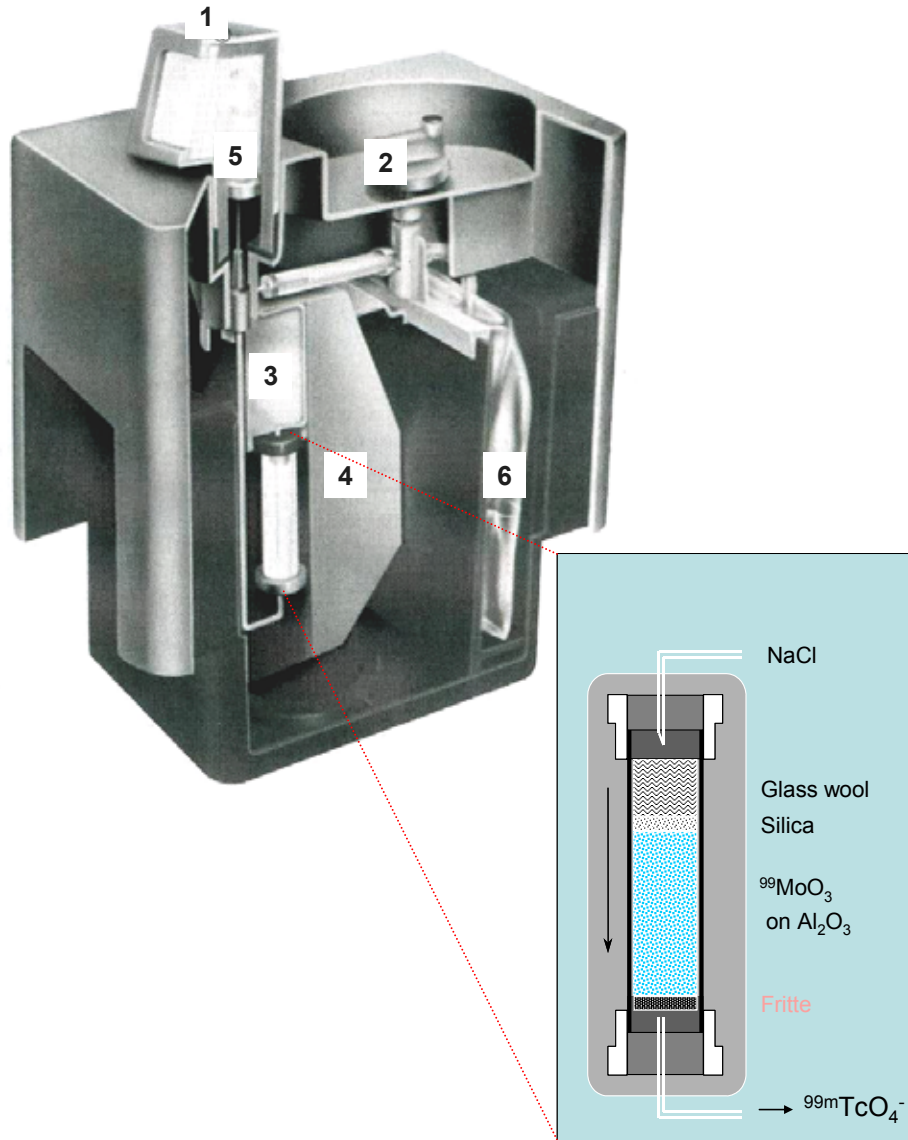
**All these nuclides are commercially produced and sold  
as radionuclide,  
generators  
or readily-prepared radiopharmaceuticals**

**Most important SPECT-Isotope is Technetium ( $^{99m}\text{Tc}$ ) !**

# SPECT - Isotopes

Radio nuclide	$T_{1/2}$	Mode of decay	Main- $\gamma$ -Lines	Productions data		
				Nuclear reaction	Energy range [MeV]	Yield [MBq/ $\mu$ Ah]
$^{67}\text{Ga}$	3.26 d	EC (100)	93 (27%)	$^{68}\text{Zn}(p,2n)$	26 $\rightarrow$ 18	185
$^{99}\text{Mo}$ ↓ $^{99\text{m}}\text{Tc}$	2.75 d  6.0 h	b- (100)  IT (100)	181 (6%) 740 (12%) 141 (87%)	$^{235}\text{U}(n,f)$ $^{98}\text{Mo}(n,g)$	$\sigma_{\text{th}} = 0.14\text{b}$	
$^{111}\text{In}$	2.8 d	EC (100)	173 (91%) 247 (94%)	$^{112}\text{Cd}(p,2n)$	25 $\rightarrow$ 18	166
$^{123}\text{I}$	13.2 h	EC (100)	159 (83%)	$^{123}\text{Te}(p,n)$ $^{124}\text{Xe}(p,x)^{123}\text{Xe}$ $^{127}\text{I}(p,5n)^{123}\text{Xe}$	14.5 $\rightarrow$ 10 29 $\rightarrow$ 23 65 $\rightarrow$ 45	137 414 777
$^{201}\text{Tl}$	3.06 d	EC (100)	68-82 (RL) 166 (10.2%)	$^{210}\text{Tl}(p,3n)^{201}\text{Pb}$	28 $\rightarrow$ 20	

# $^{99m}\text{Tc}$ -Generator (1)



## (1) Simple Handling

Insert vacuum flask and elute desired volume.

## (2) Transport-Security-valve

Prevent an elution after production and during transport

## (3) Shifted needle

Reduction of energy rich Mo-radiation

## (4) Max. protection against radiation

Protection from all side.

$^{99}\text{Mo}$ -column is covered at least with 52 mm Pb.

Supplementary shielding with overall 98 mm Pb.

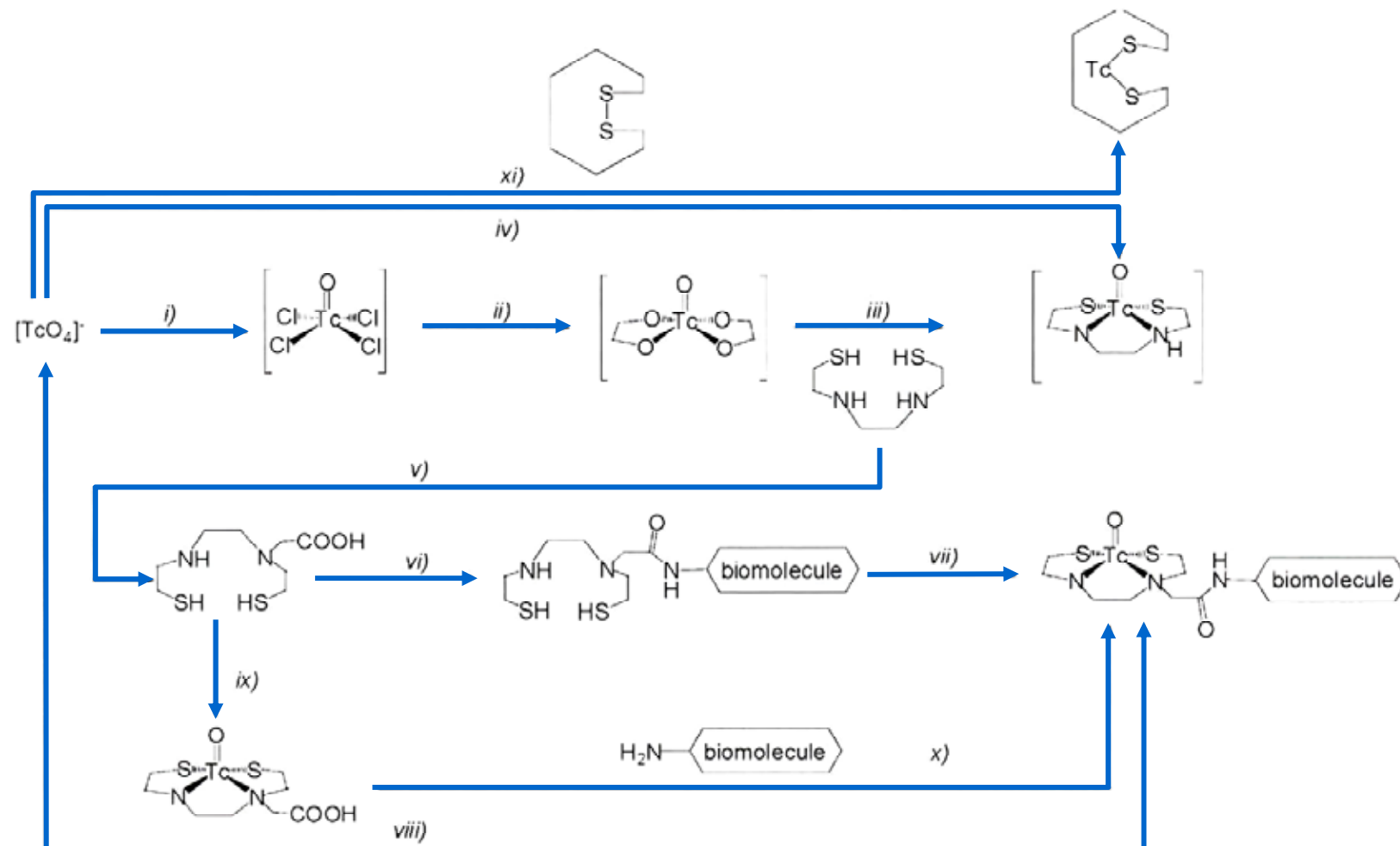
## (5) High concentrated activity

Total  $^{99m}\text{Tc}$ -activity is less than 5 mL volume.

## (6) Ready for use

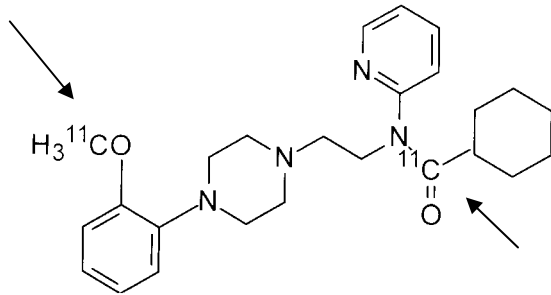
Sterile, closed system.

# Labeling of Tc-Radiopharmaceuticals

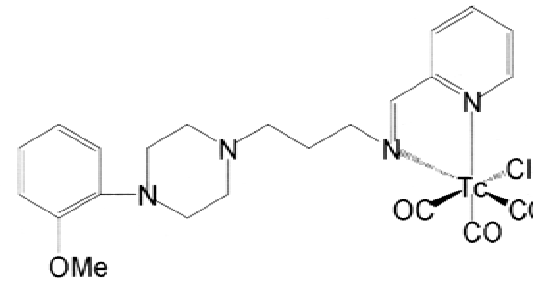




# Tracer Properties: Influence of the Nuclide



WAY 100638 (5-HT<sub>1A</sub>-receptor ligand)



<sup>99m</sup>Tc-WAY 100638-analog  
(as 5-HT<sub>1A</sub>-receptor ligand)

<sup>11</sup>C

<sup>18</sup>F

<sup>123</sup>I

<sup>99m</sup>Tc

<sup>68</sup>Ga / <sup>111</sup>In

Change in structure

Predictability of biological integrity

Complexity of radiopharmaceutical development

# Molecular Imaging by Radiotracer

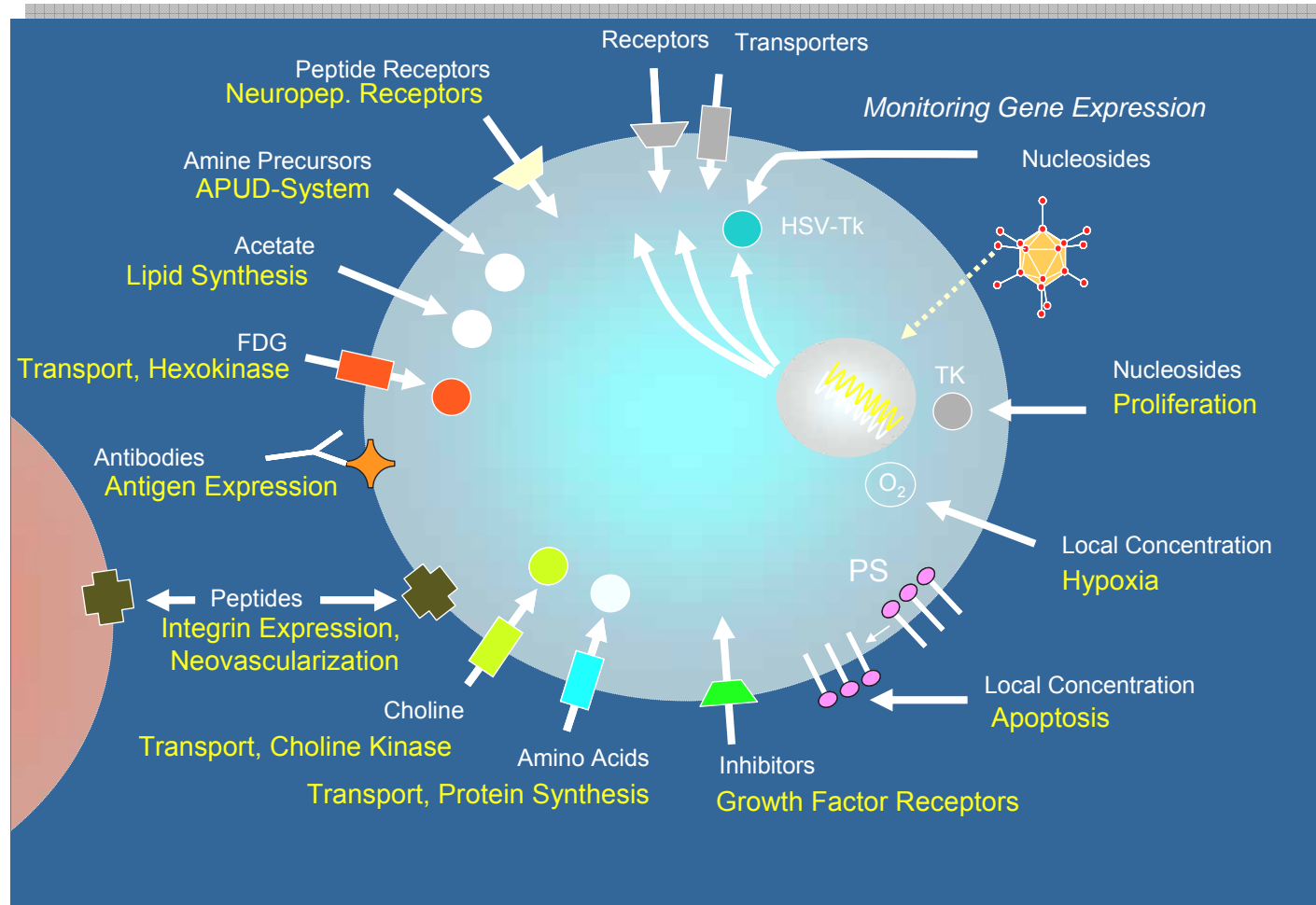
Targeting biochemical processes in living organism  
on basis of molecular interaction between tracer und target

by radiolabeled, „molecular probes“, changing their concentration at  
the target in a specific way

and suitable detection systems for non-invasive, quantitative  
and repetitive measurement

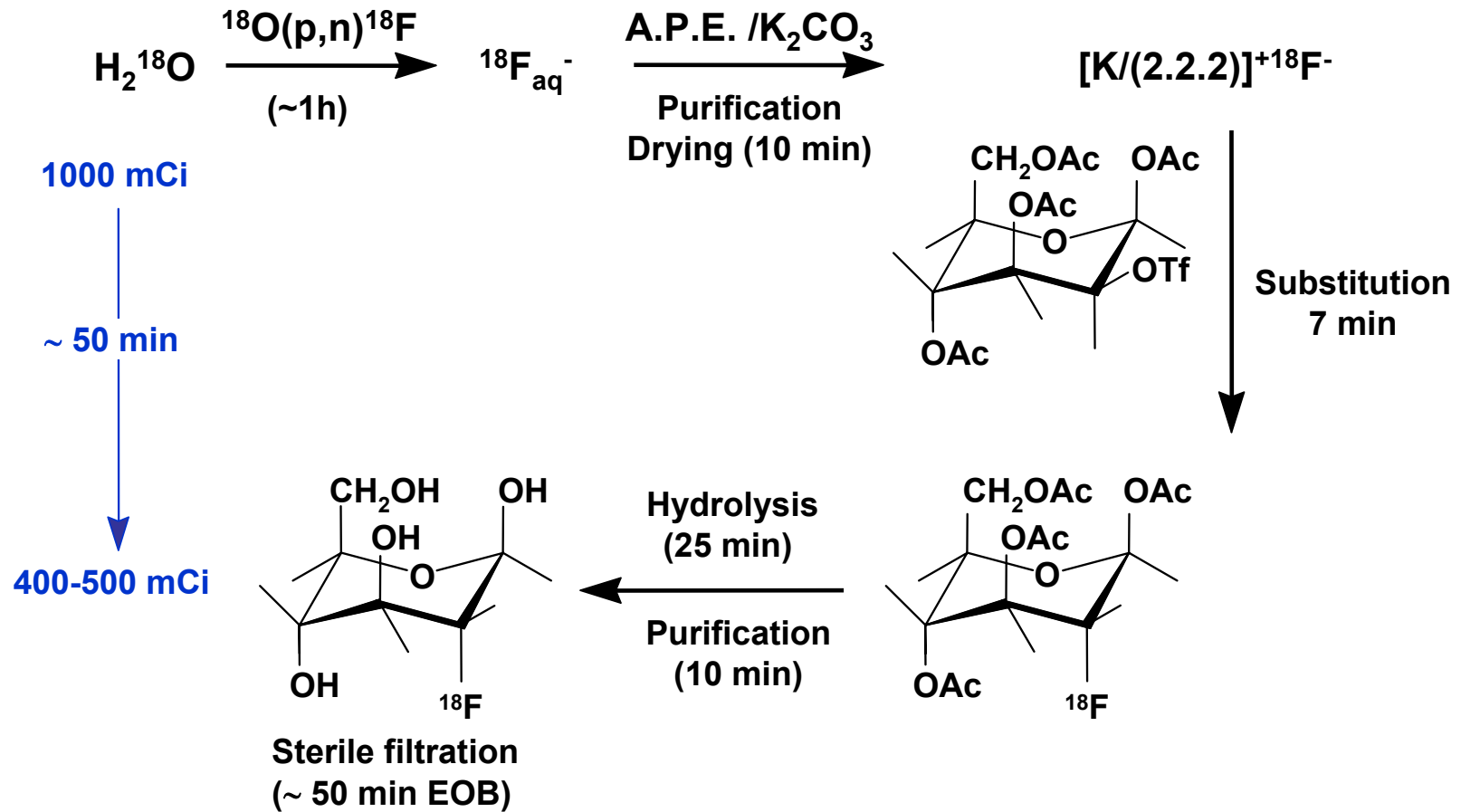
with the aim of exploring physiological processes,  
diagnostics und therapy as well as therapy monitoring

# Target Structures in Oncology



Characterization of the tumor biology by molecular imaging

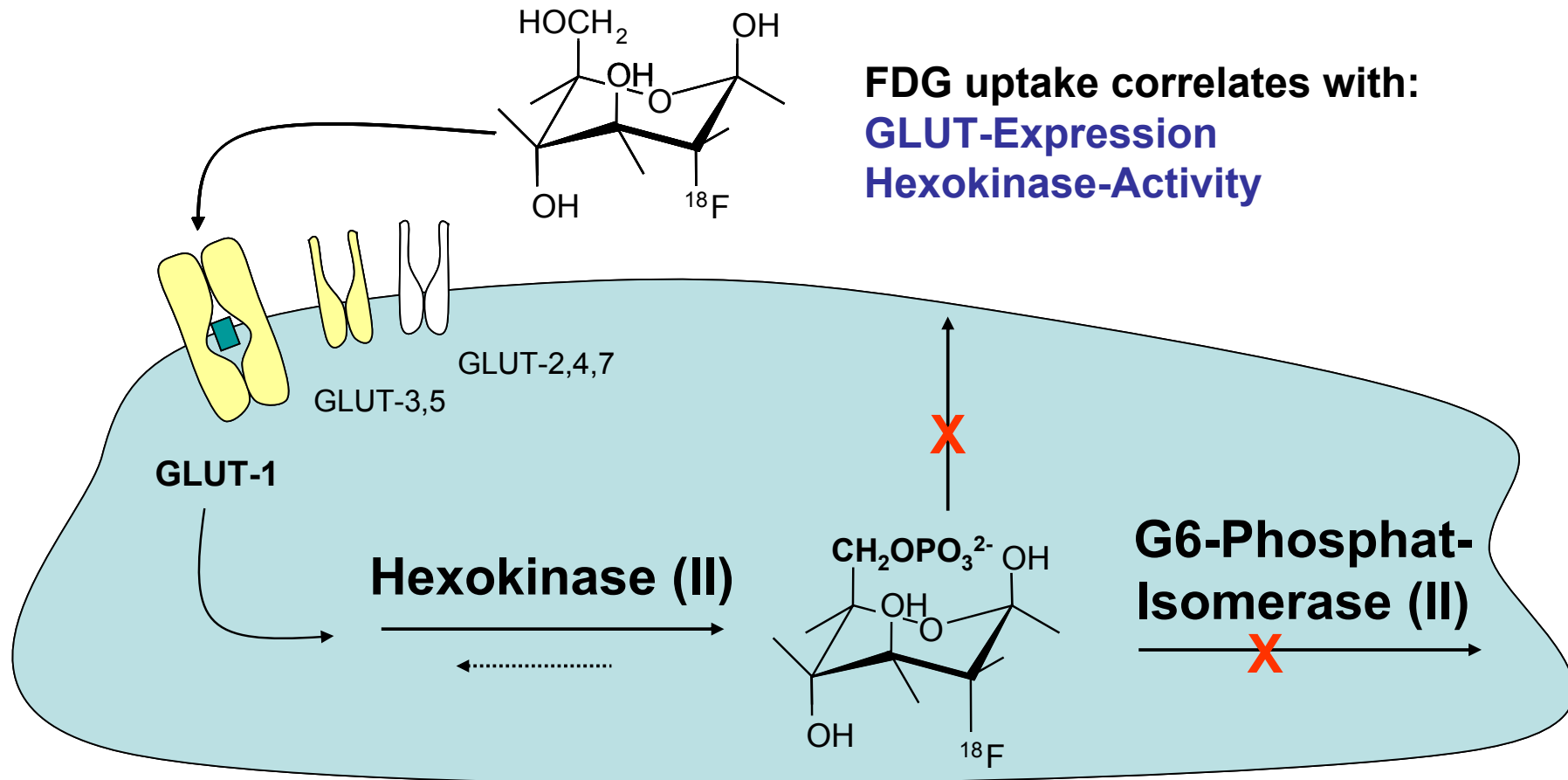
# 2-[<sup>18</sup>F]Fluoro-2-Deoxy-Glucose-Synthesis ([<sup>18</sup>F]FDG)



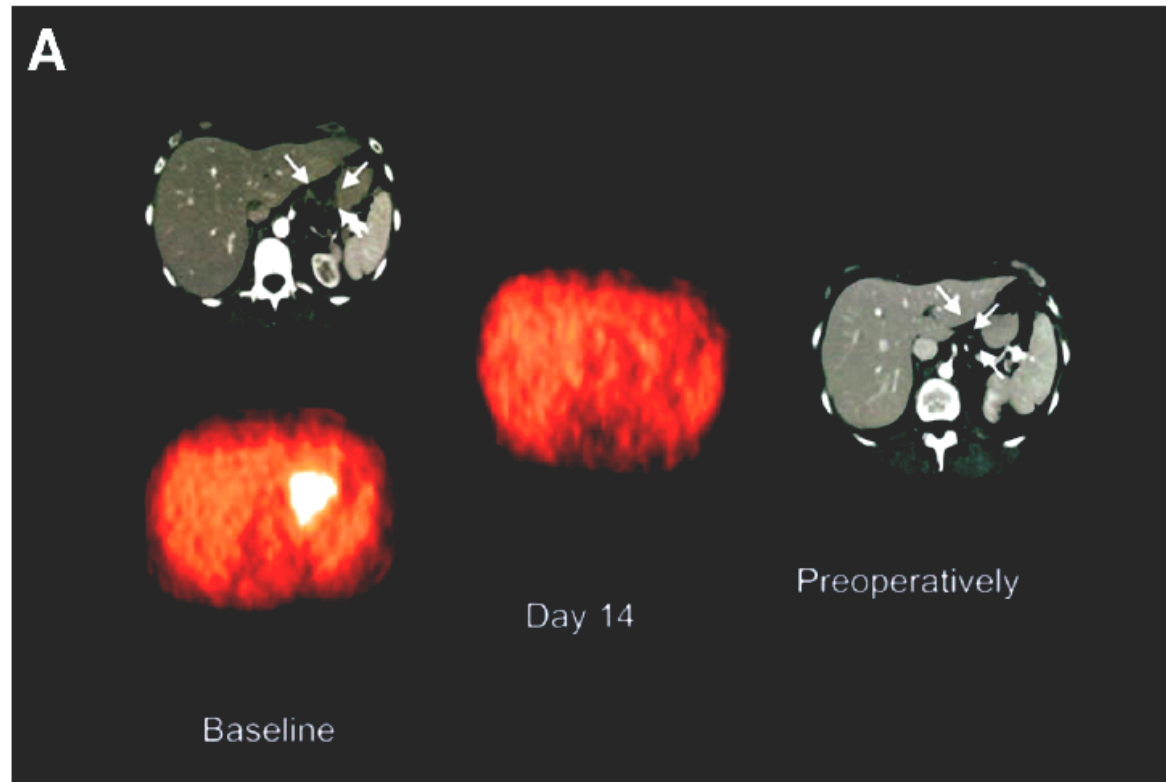
# GMP Production of FDG 2-[<sup>18</sup>F]Fluor-2-deoxy-D-Glucose, TU Munich



# Scheme of [ $^{18}\text{F}$ ]FDG Uptake

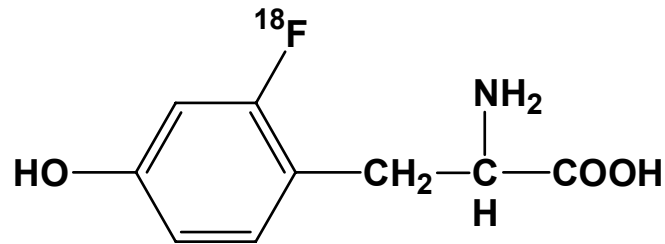


# [<sup>18</sup>F]FDG: Therapy control –gastric carcinoma-

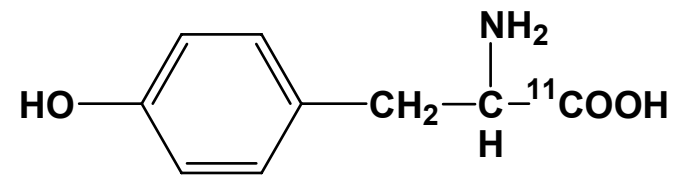


# Amino Acid Transport

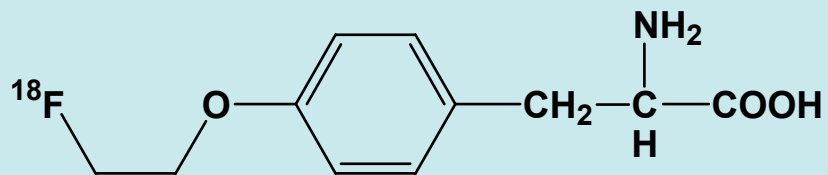
Primary target: Rate measurement of regional protein synthesis  
 But: During the short time period after injection the accumulation of tracer represent only the accumulation of amino acid by special transport systems



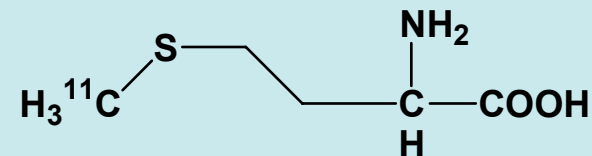
2-Fluoro-L-Tyrosin **2-[<sup>18</sup>F]Tyr**



L-Tyrosin **1-[<sup>11</sup>C]Tyr**



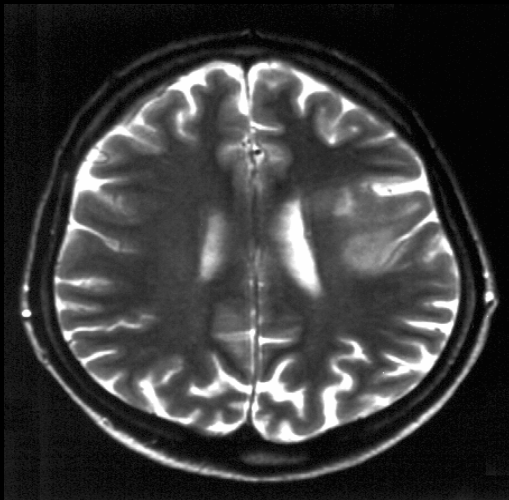
O-(2-Fluoroethyl)-L-Tyrosin **[<sup>18</sup>F]FET**



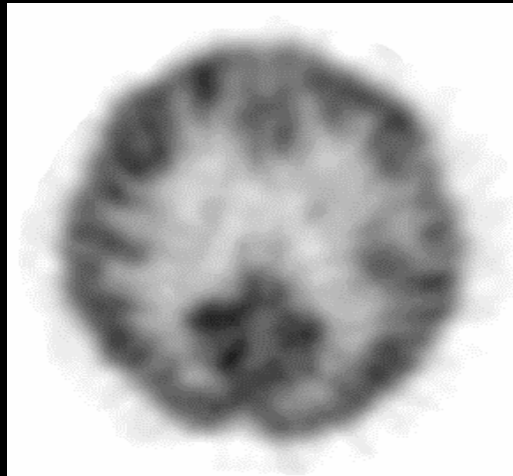
L-Methionine **[<sup>11</sup>C]MET**



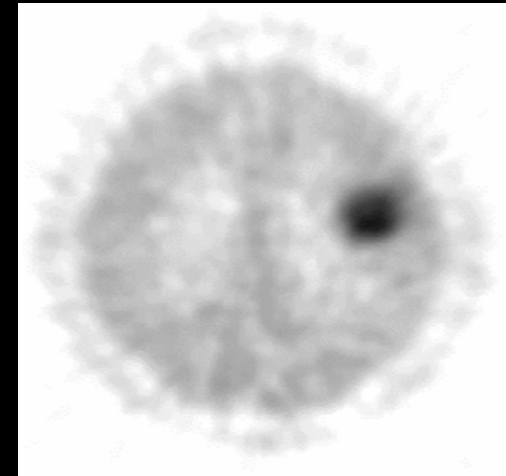
# $[^{18}\text{F}]$ FDG-PET versus $[^{11}\text{C}]$ MET-PET -Brain Tumor-



MRT (T2)



FDG-PET

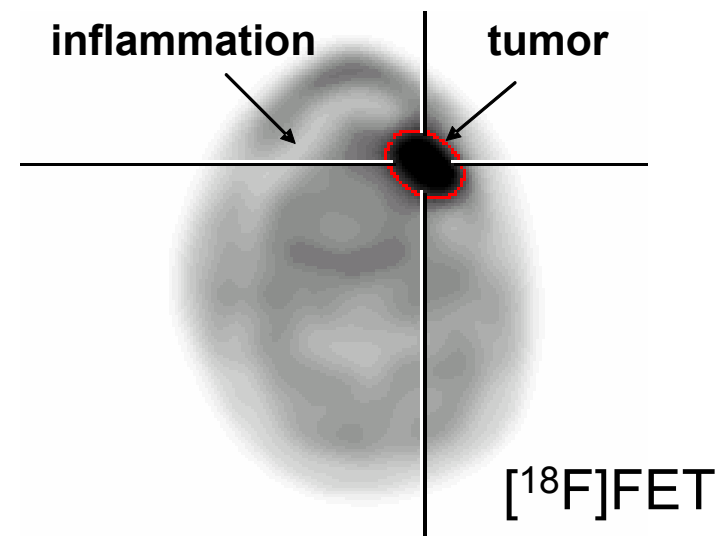
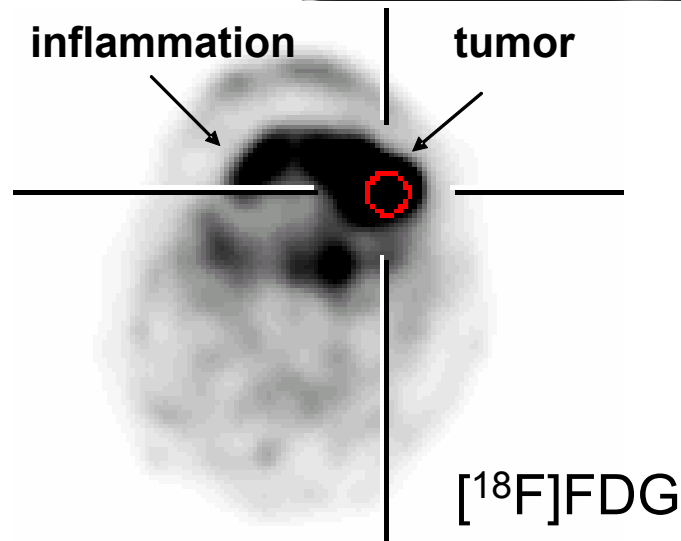


$[^{11}\text{C}]$ Methionine-PET

## O-(2-[ $^{18}\text{F}$ ]Fluoroethyl)-L-Tyrosin: [ $^{18}\text{F}$ ]FET (2)

FDG also accumulates in inflammation, amino acids and especially FET does not accumulate in inflammation.

Squamous cell carcinoma



# Imaging of Metastatic Prostate Cancer

**$^{11}\text{C}$ -Acetate:**

**Prostate cells undergo metabolic transformation from citrate producing normal cells to citrate oxidizing malignant cells (Costello LC et al. *Urology* 1997)**

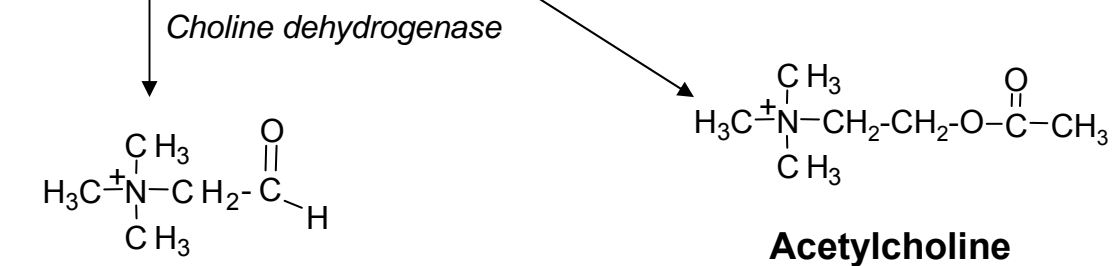
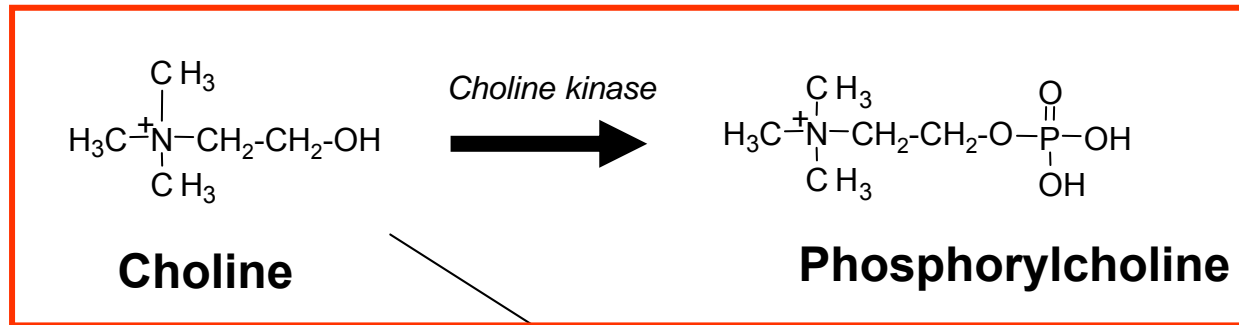
**$^{18}\text{F}/^{11}\text{C}$ -Cholines:**

**malignant transformation is associated with induction of choline kinase activity (e.g. Kotzerke et al. and refs herein; *J Nucl Med.* 2002)**

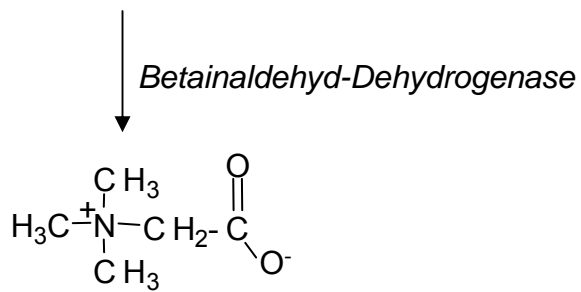
**( $^{18}\text{F}$ -Fluoride):**

**(for bone metastasis)**

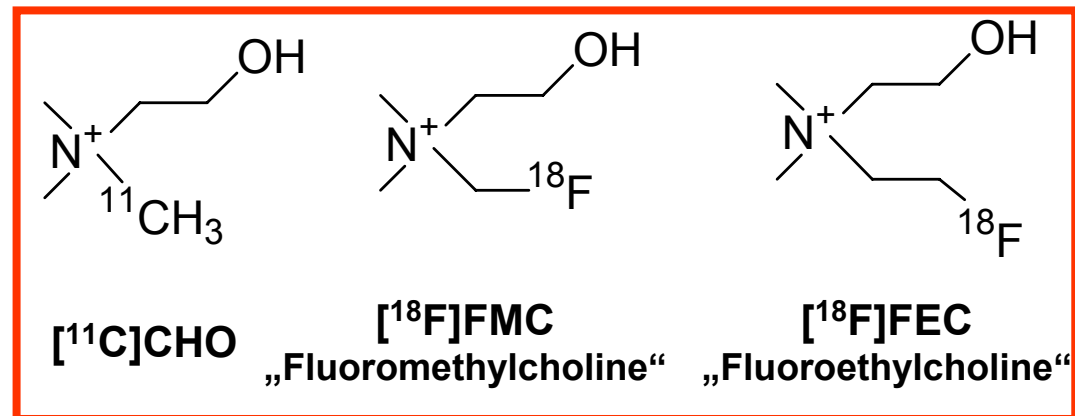
# Biochemical Model: Choline



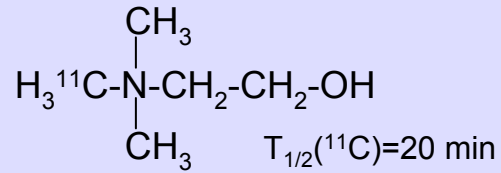
**Betain-aldehyde**



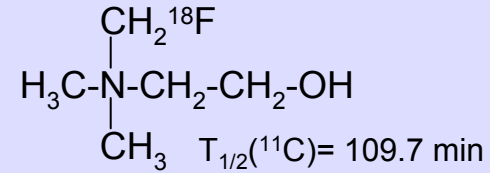
**Betain**



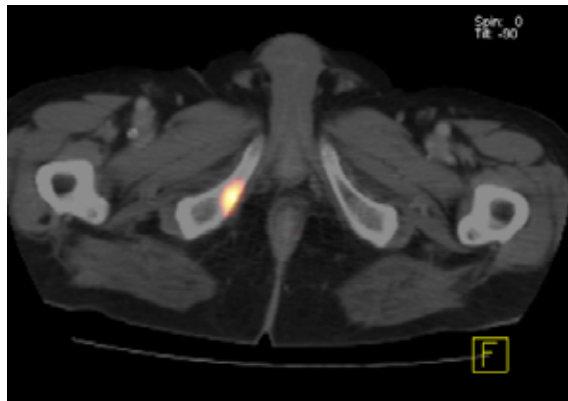
# <sup>11</sup>C-Choline-PET



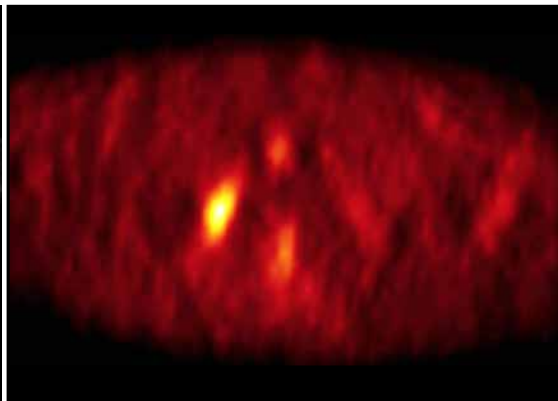
# <sup>18</sup>F-Choline-PET



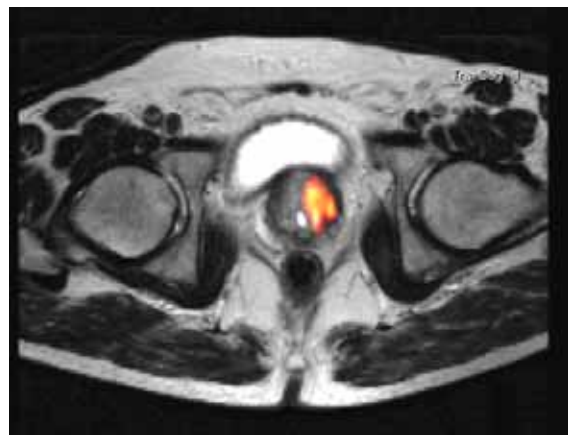
## Bladder cancer metastasis



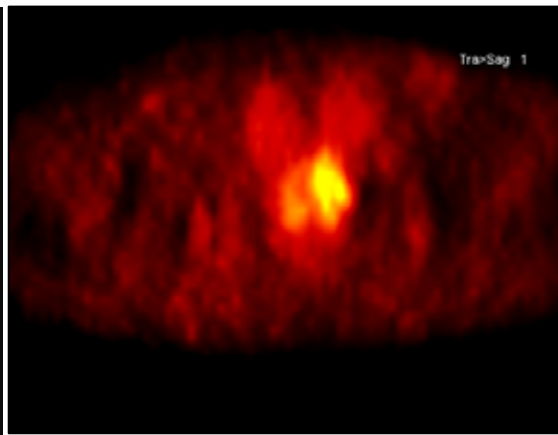
PET/CT



PET



Prostate carcinoma

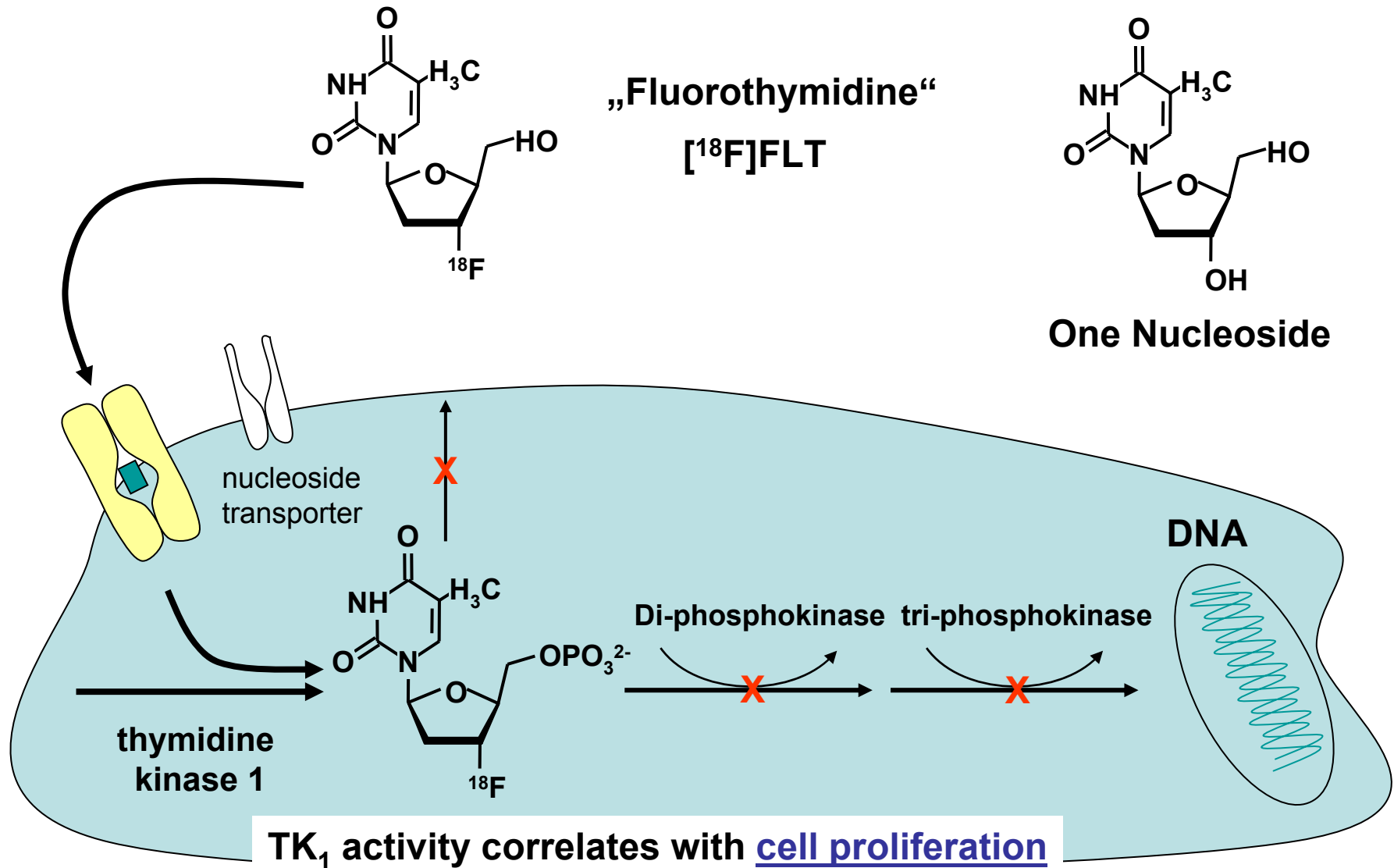


Tracer accumulation with:

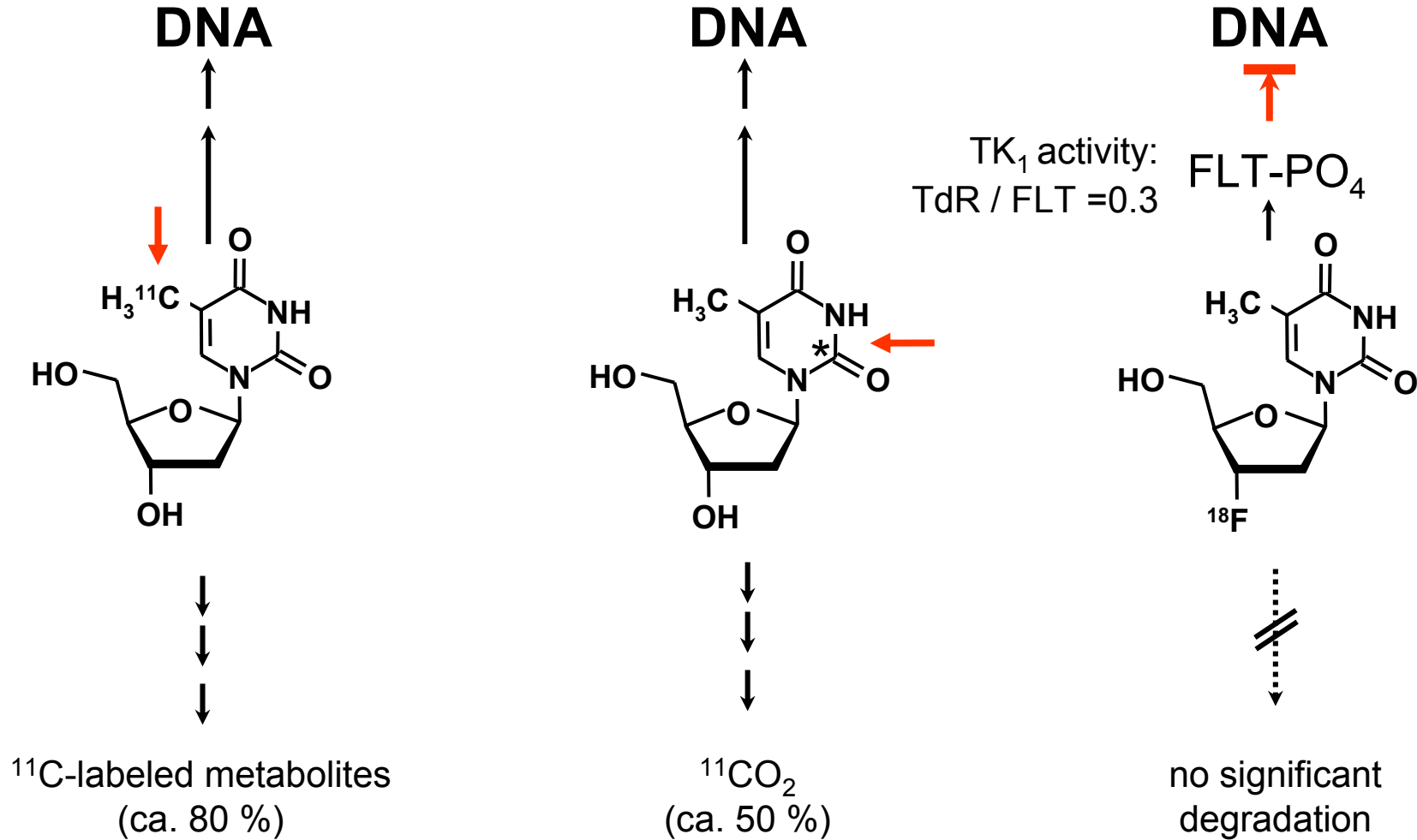
1. Cellular accumulation by choline transporter; (Signal in the first minutes after injection)

2. and followed by phosphorylation by choline kinase. (Signal by late imaging)

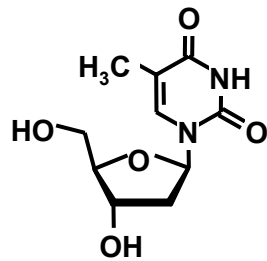
# 3'-[<sup>18</sup>F]Fluoro-3'-Deoxy-Thymidine: [<sup>18</sup>F]FLT



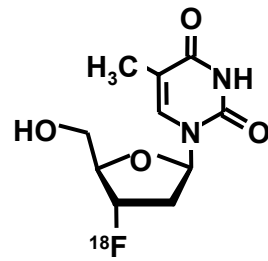
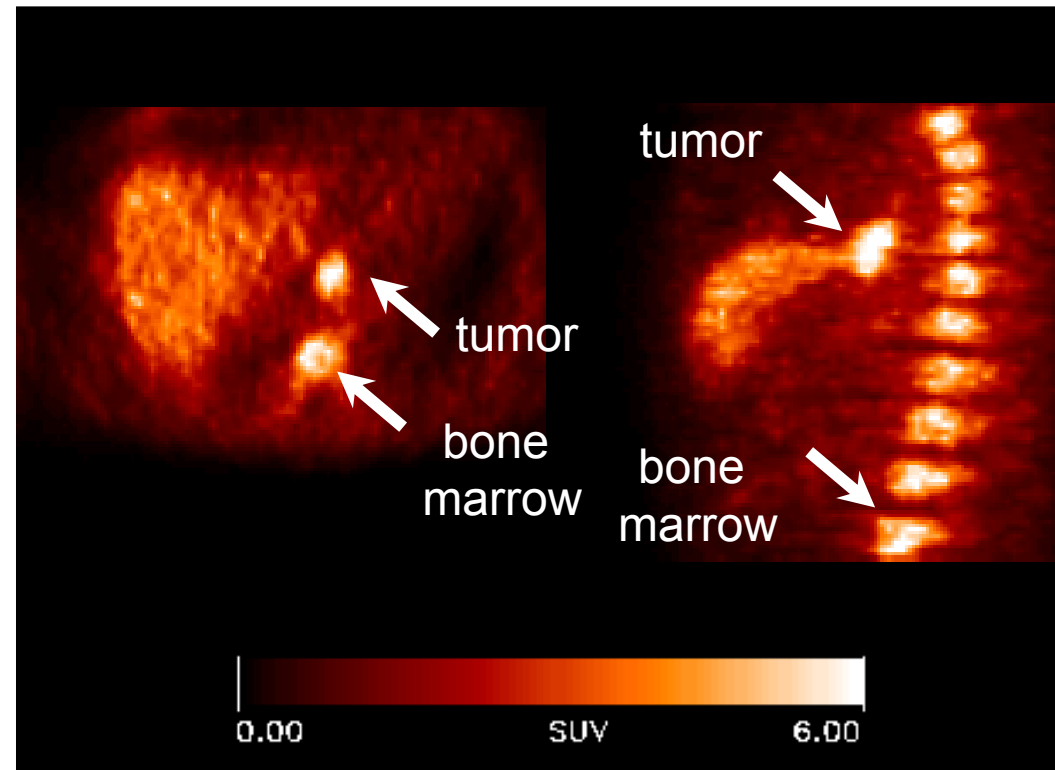
# Metabolic Scheme for [<sup>11</sup>C]Thymidine and FLT



# Visualization of Cell Proliferation with $^{18}\text{F}$ -thymidine (FLT) in Esophageal Cancer



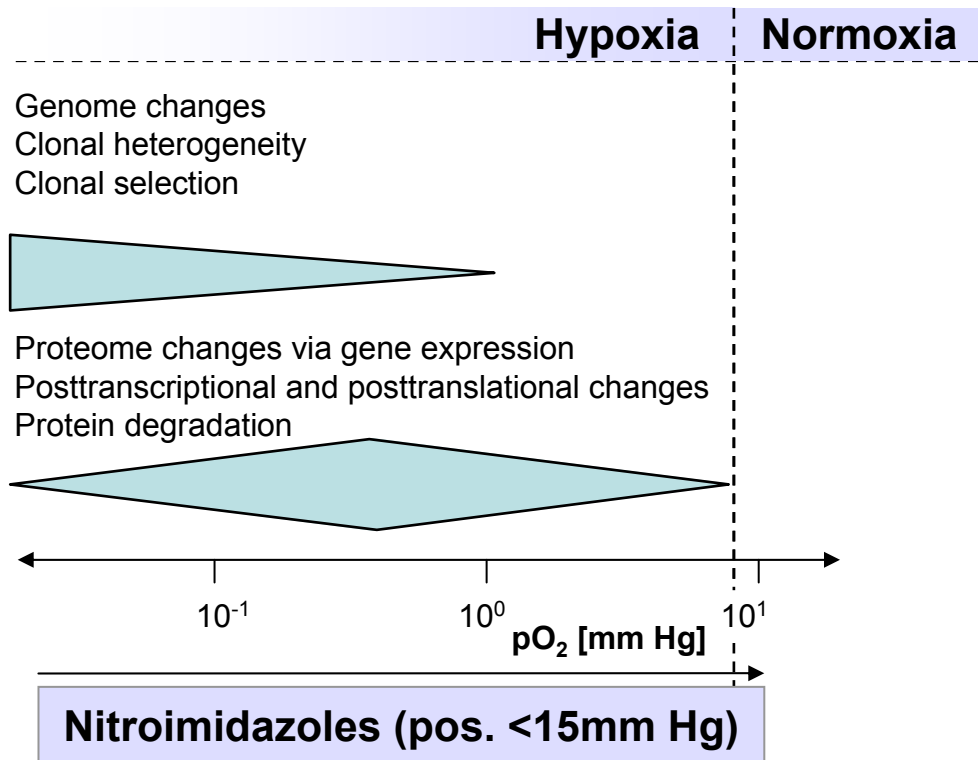
thymidine

 $[^{18}\text{F}]$ FLT

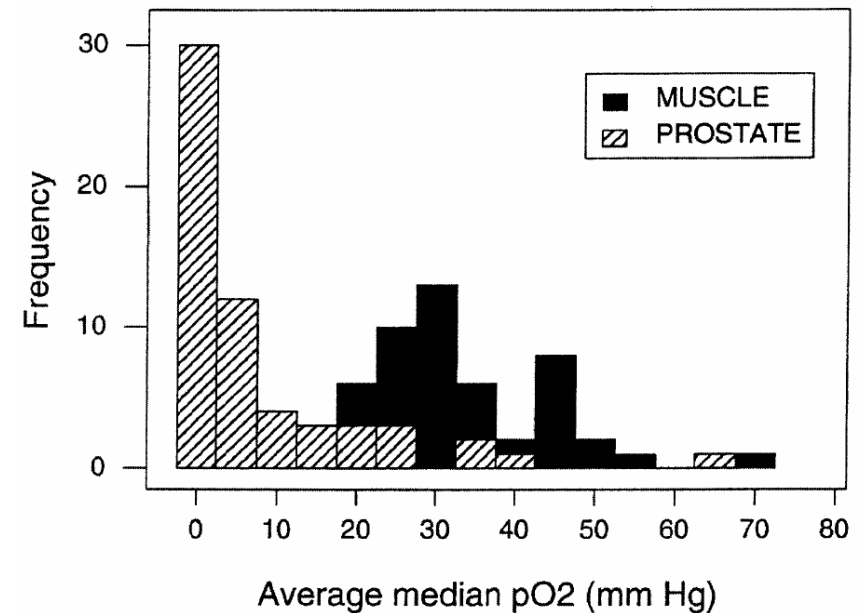


# Critical O<sub>2</sub> Levels

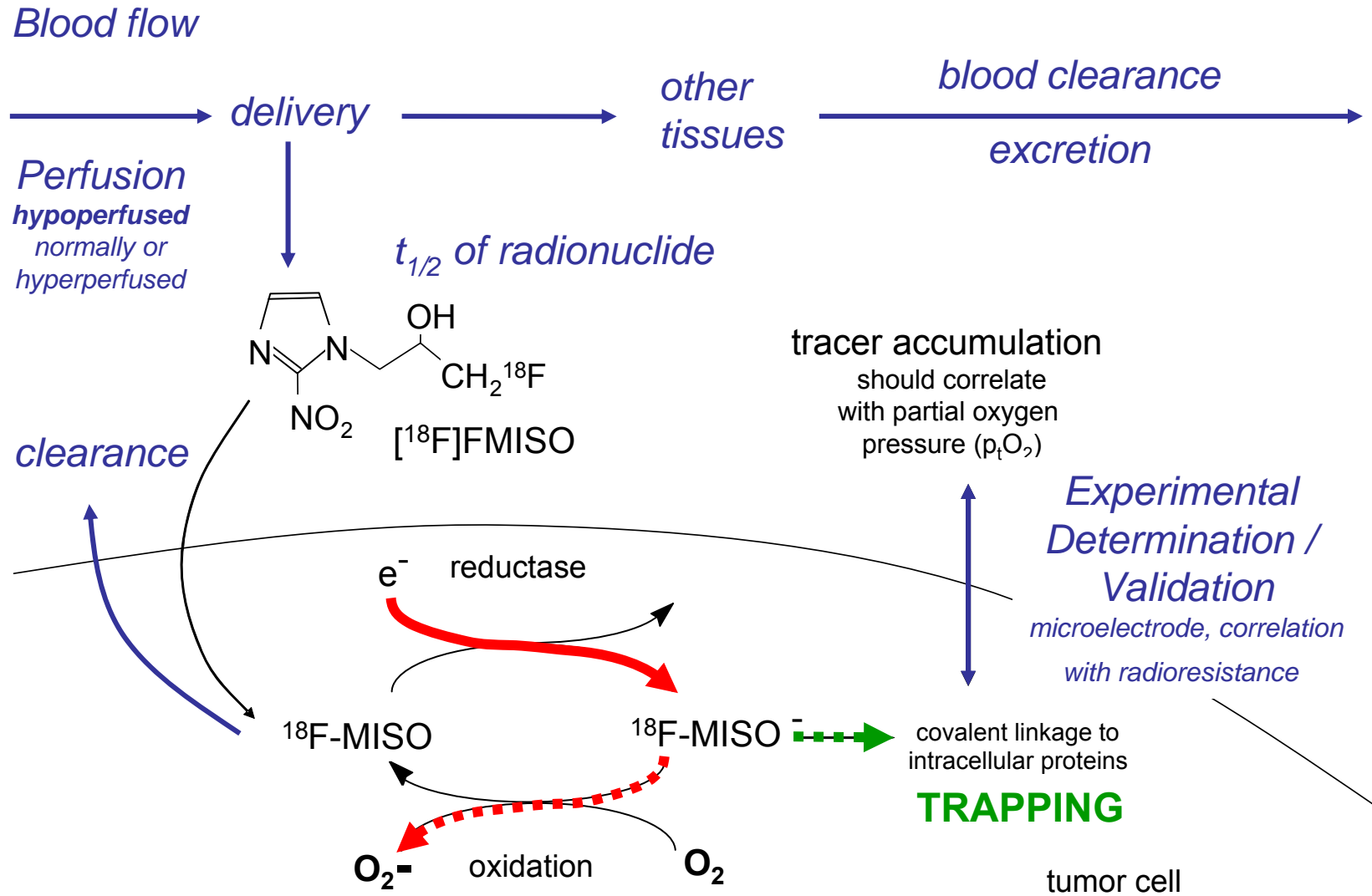
Aggressiveness ↑  
Tumor Progression



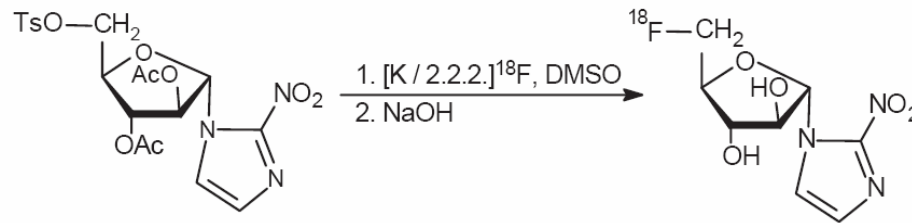
Distribution of medium pO<sub>2</sub> levels for prostatic tumor tissue versus muscle



# The Mechanism of Non-Invasive Detection of Tumor Hypoxia

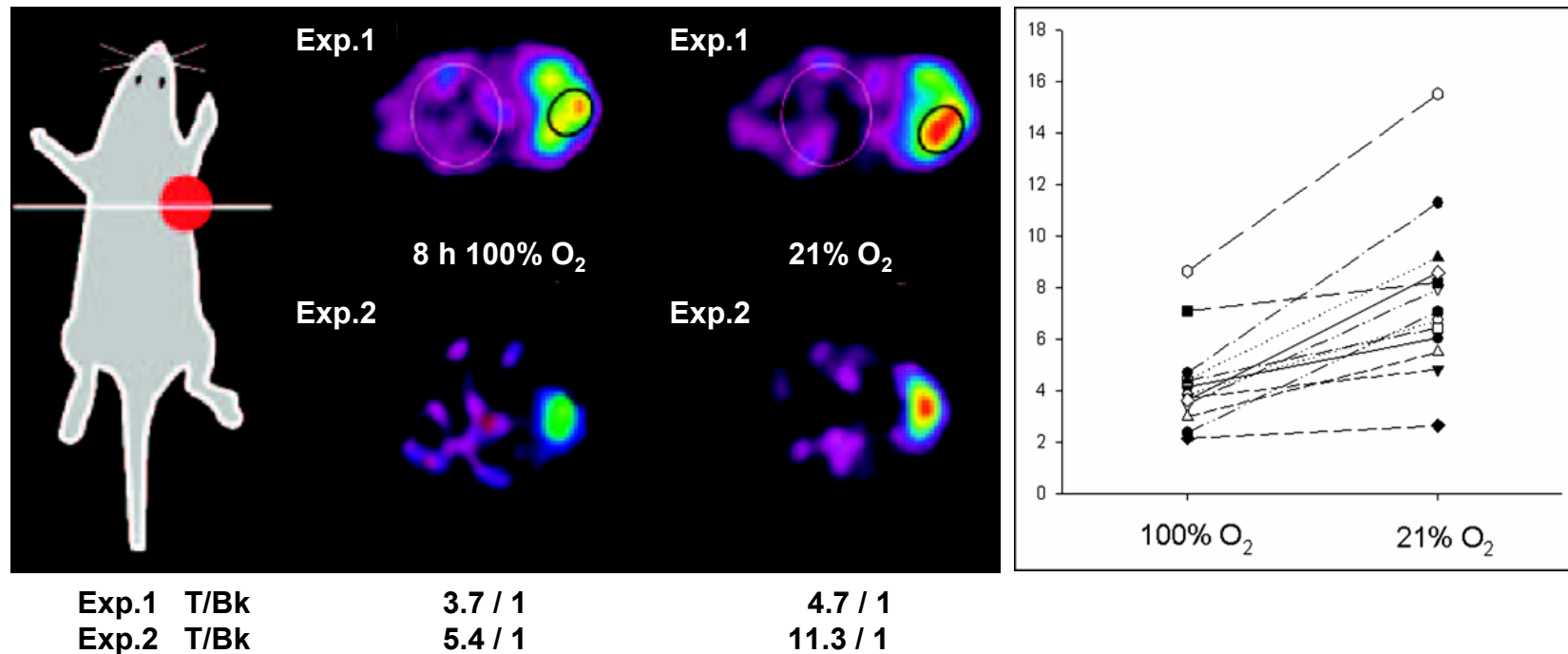


# Evaluation of [<sup>18</sup>F]FAZA

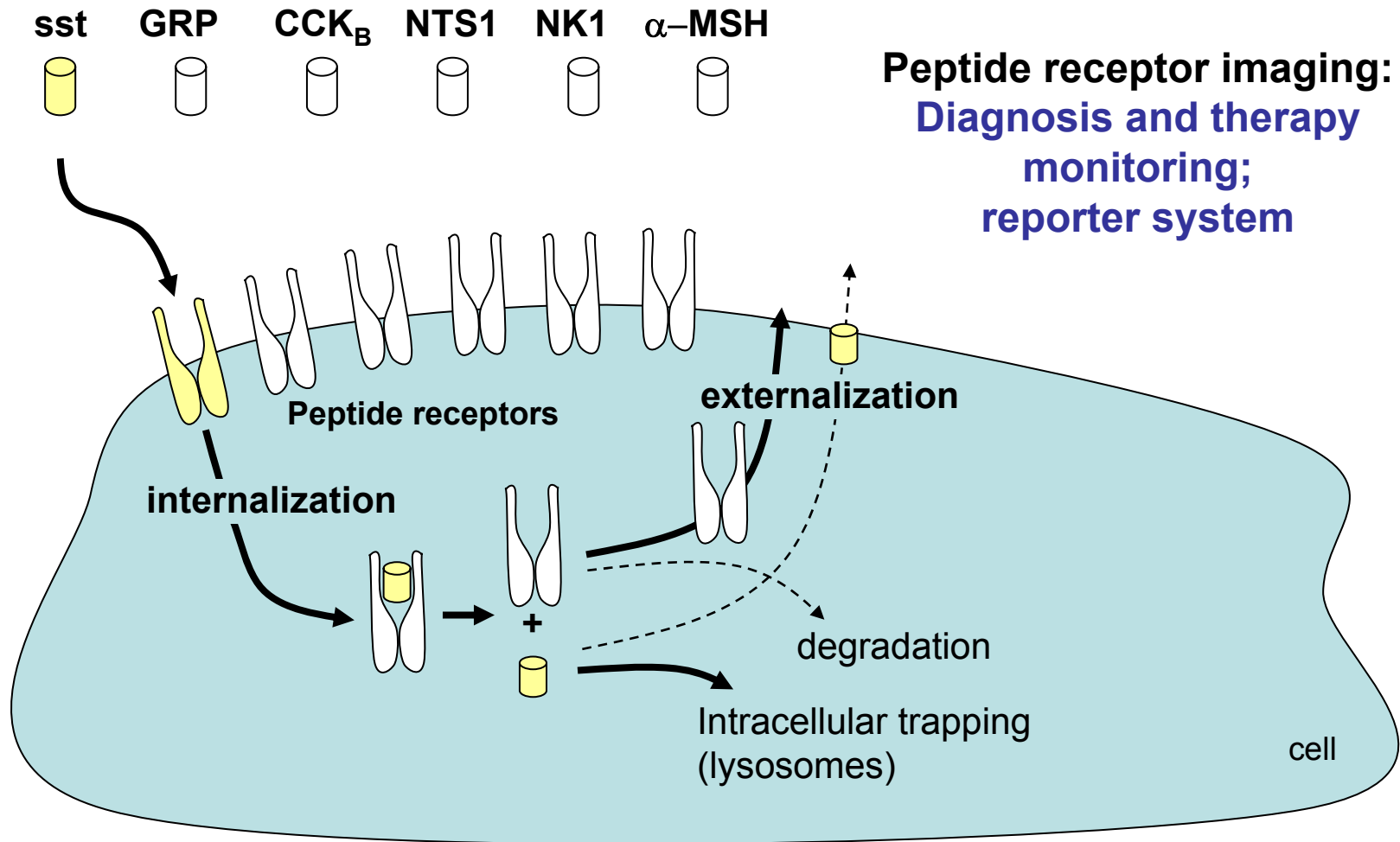


Synthesis of [<sup>18</sup>F]FAZA:  
 Radiochemical Yield: 20 ± 4%, 50 min  
 (Reischl et al., 2005)

Serial, transaxiale PET images -nude mice- with A431 tumors.



# Peptide Receptor Imaging: PRI



## Targets for Radiolabeled Peptides in Human Tumor Tissue

Somatostatin-R

neuroendocrine tumors, small cell lung cancer, medullary thyroid carcinoma, lymphoma (NHL)

Integrins

melanoma, breast tumor, osteosarcoma, glioblastoma

VIP-R

adenocarcinomas, small cell lung cancer, neuroendocrine tumors, lymphoma

CCK-B-R

medullary thyroid carcinoma, small cell lung cancer, stromal ovarian cancer, astrocytoma

Substance P-R

medullary thyroid cancer, small cell lung cancer, breast tumors

Bombesin/ GRP-R

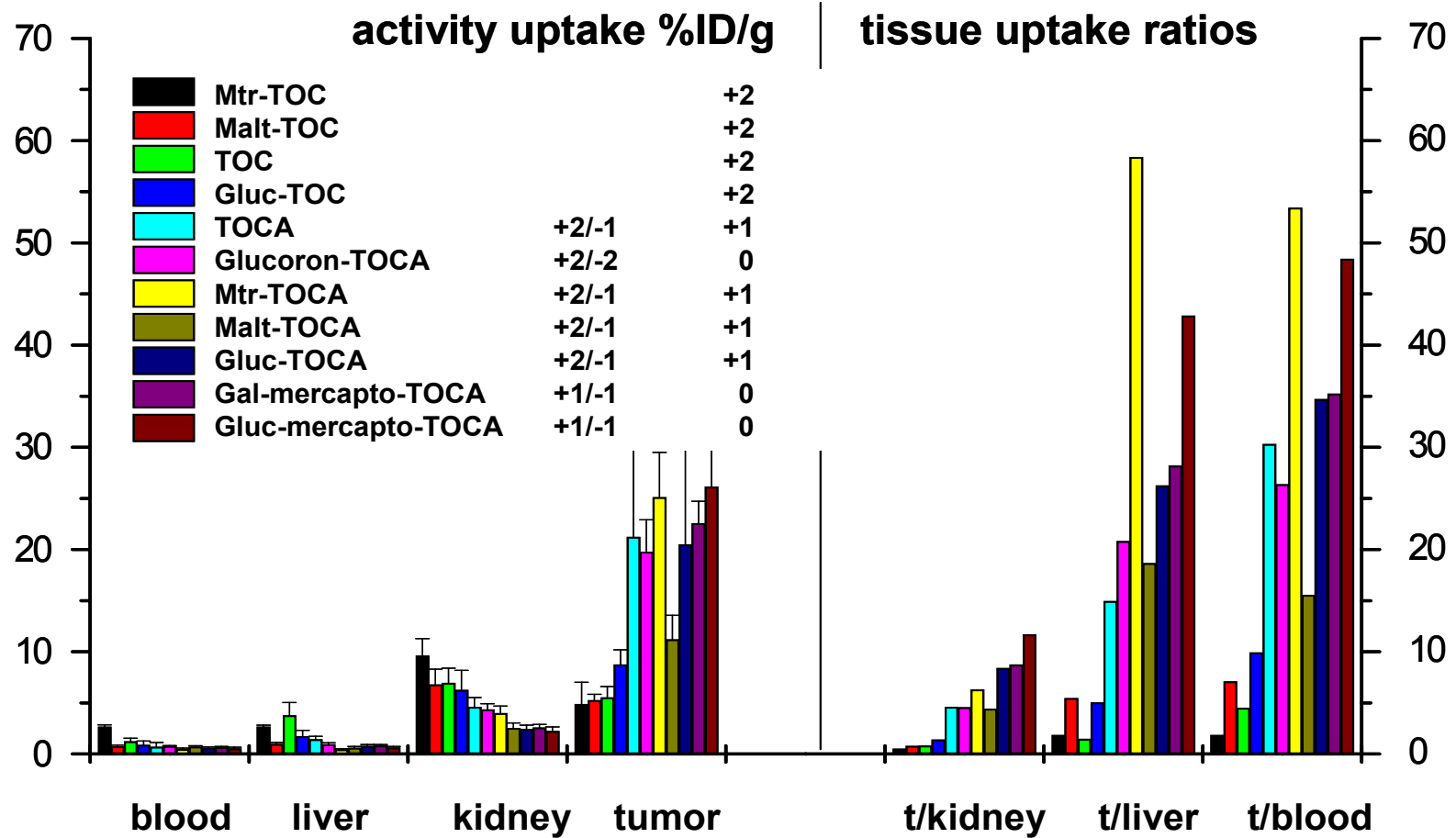
colon cancer, small cell lung cancer, glioblastoma

Neurotensin-R

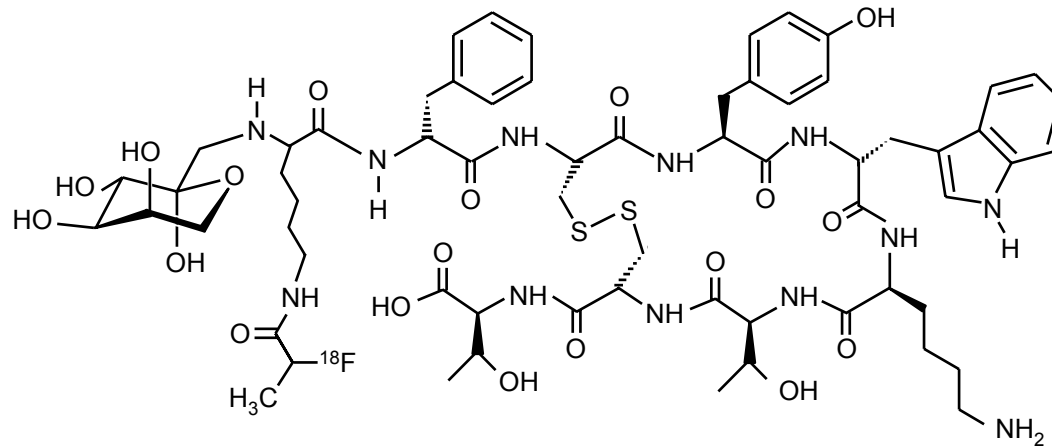
pancreatic cancer, prostate cancer, small cell lung cancer

# Influence of the Carbohydrate on the Biodistribution of Octreotides/-tates

(Mice, AR42J, n=3-5, 60 min p.i.)



# Chemical Structure of Gluc-FP<sup>[18F]</sup>-TOCA

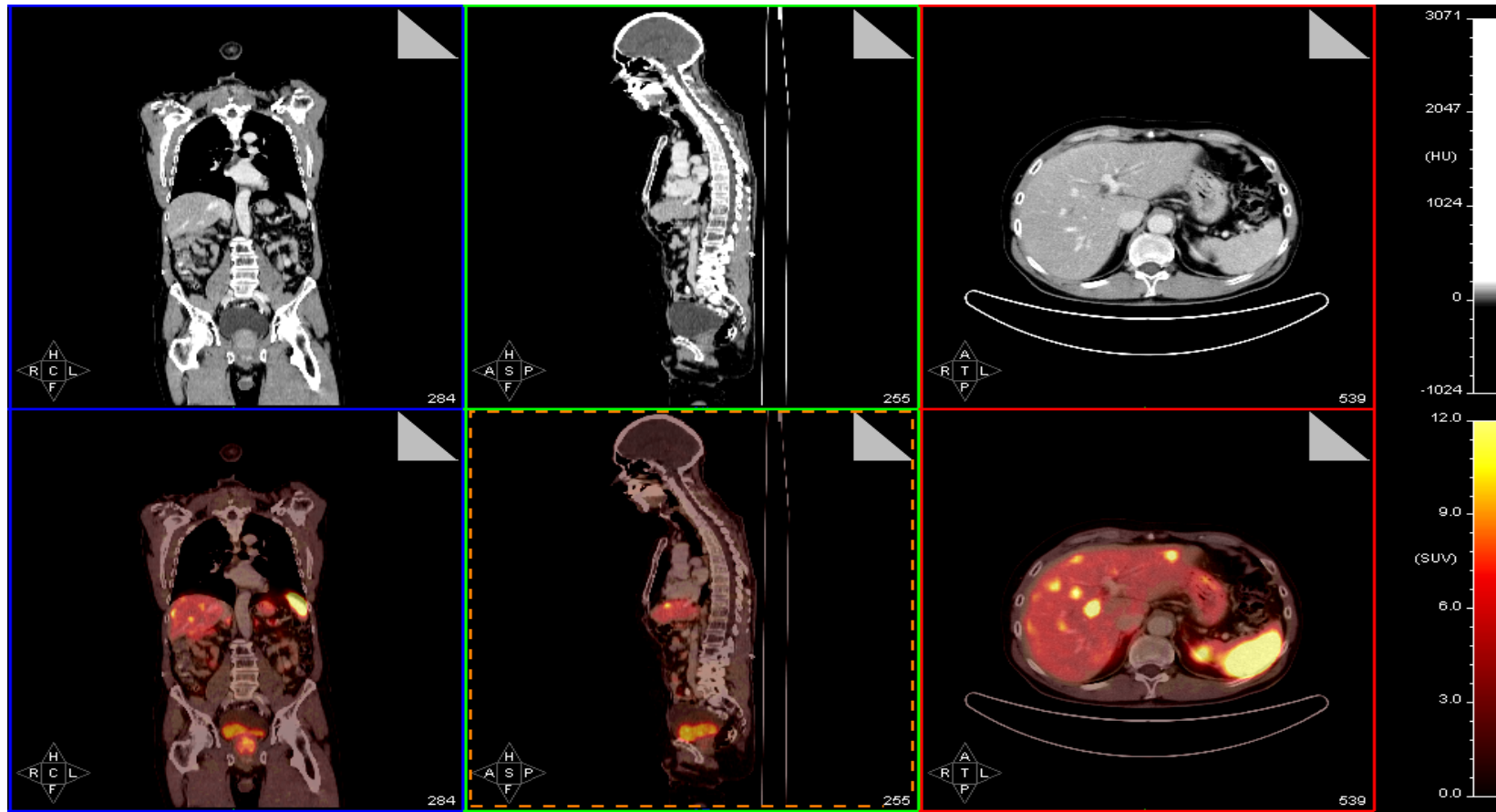


**Gluc-Lys([<sup>18</sup>F]FP)-TOCA**

[<sup>18</sup>F]FP = 2-[<sup>18</sup>F]Fluoropropionic acid

TOCA = Tyr<sub>3</sub>-octreotate, -DPhe-Cys-Tyr-DTrp-Lys-Thr-Cys-Thr-OH

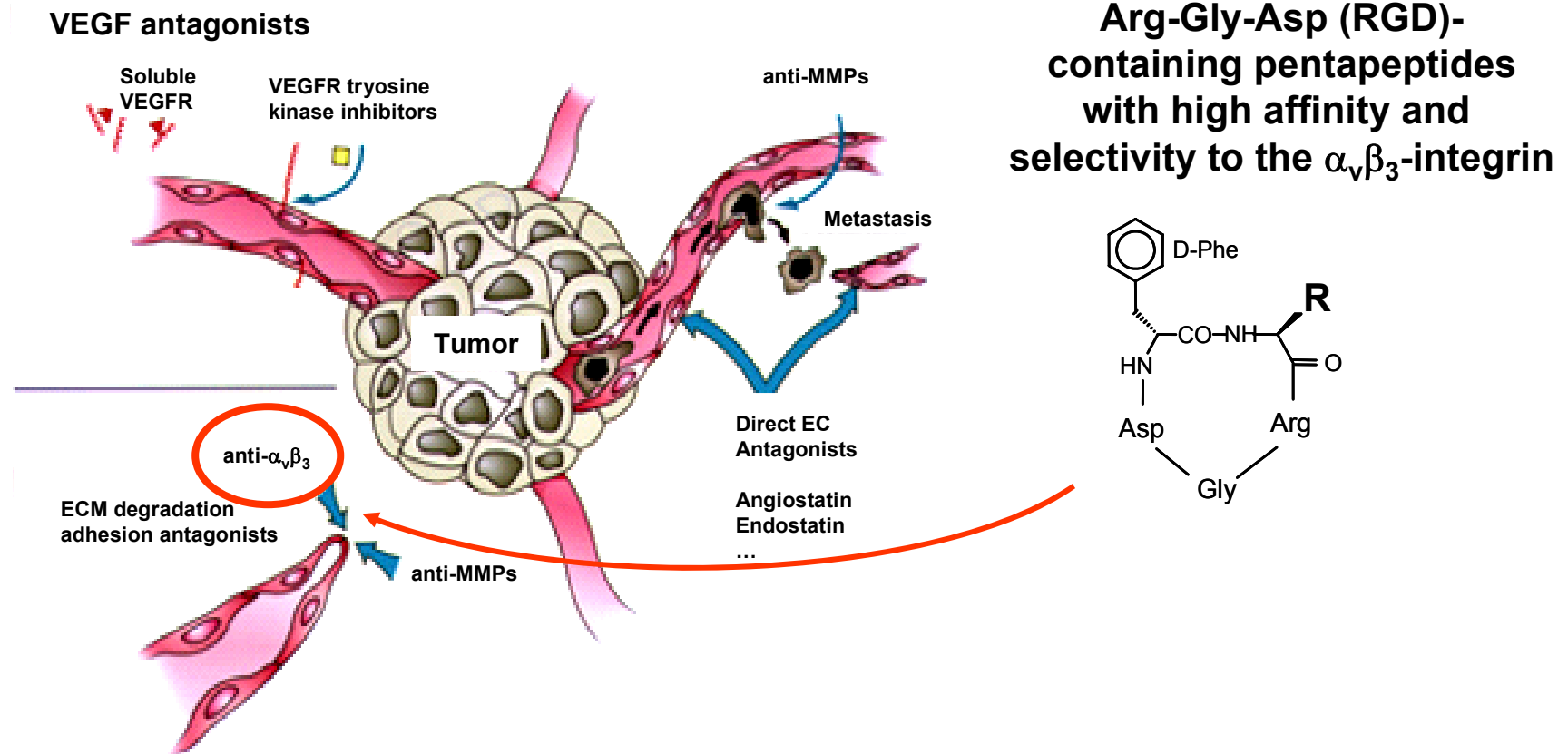
# Gluc-FP[<sup>18</sup>F]-TOCA



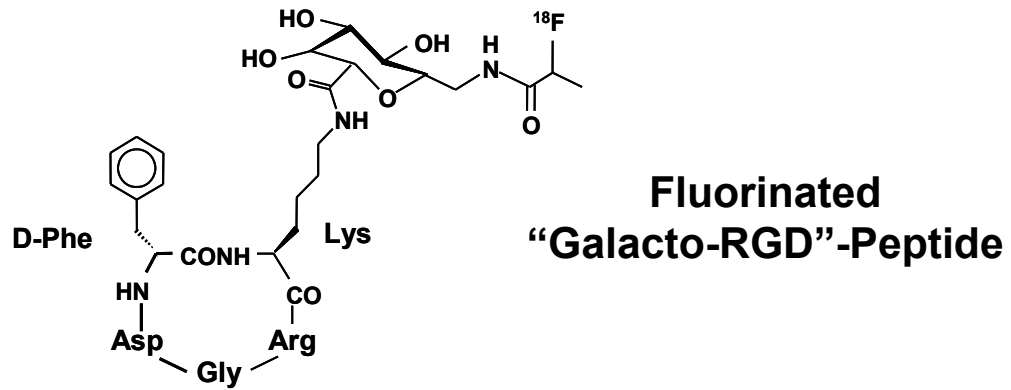
Male patient, 50 yrs, carcinoid with multiple metastases



# Imaging of Neoangiogenesis



# Carbohydrated RGD-Peptide : [<sup>18</sup>F]Galacto-RGD



Inhibition of  
Metastasis

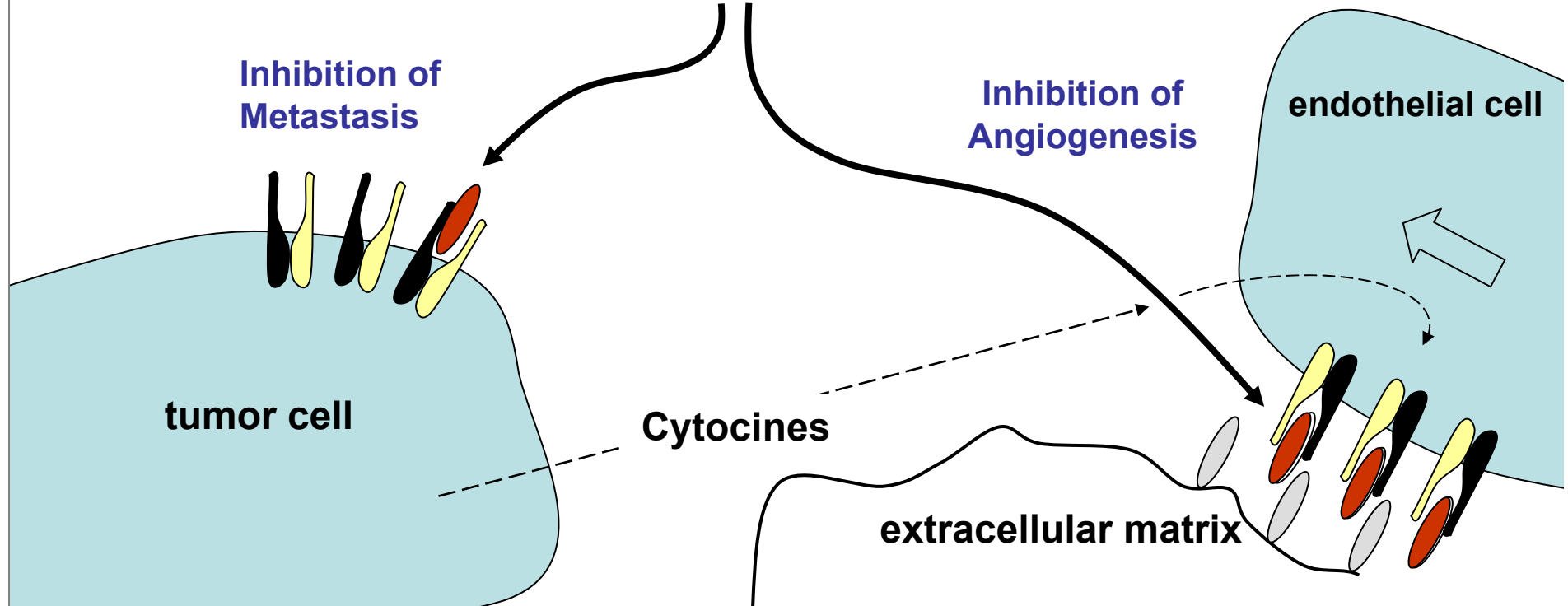
Inhibition of  
Angiogenesis

endothelial cell

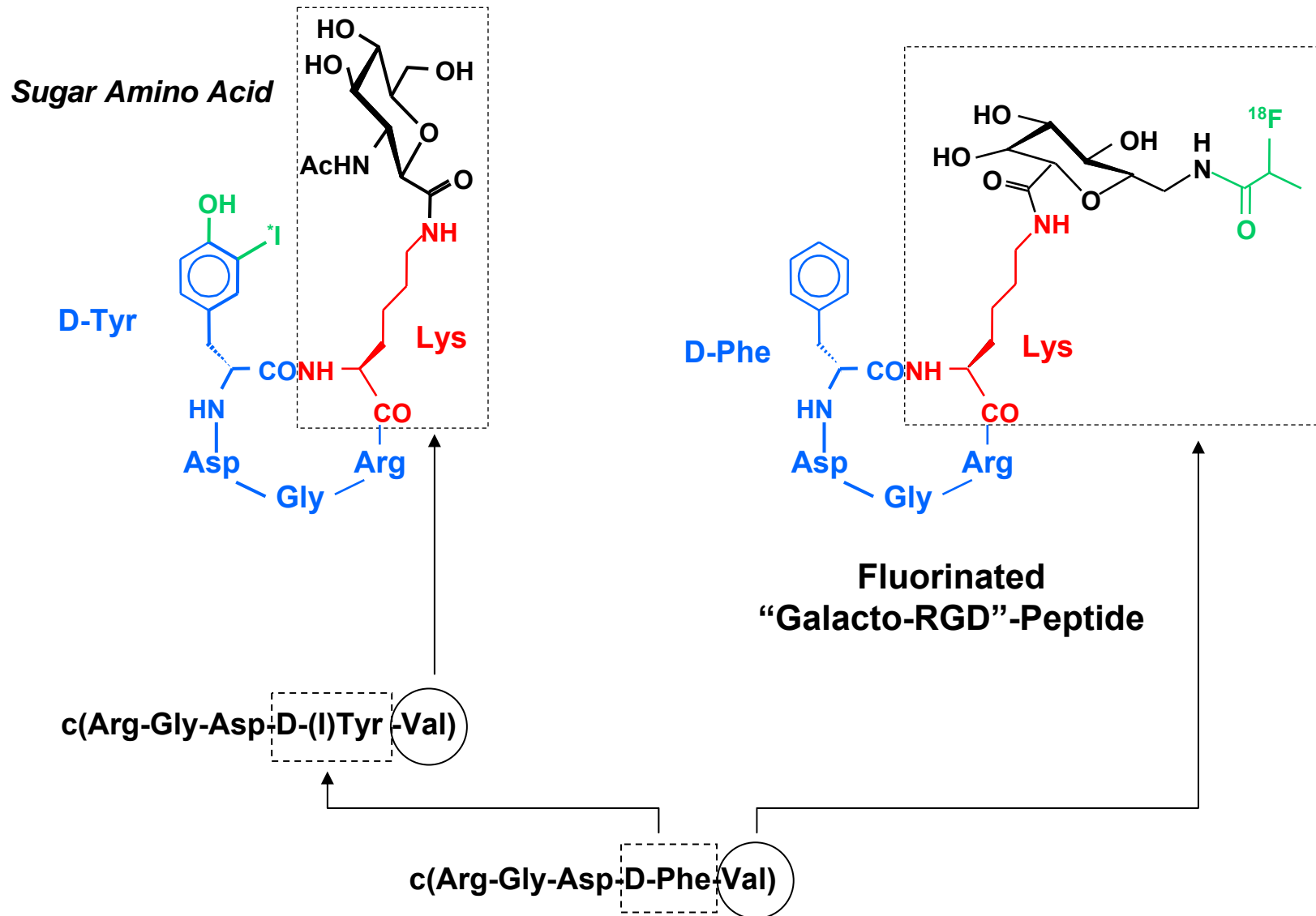
tumor cell

Cytokines

extracellular matrix

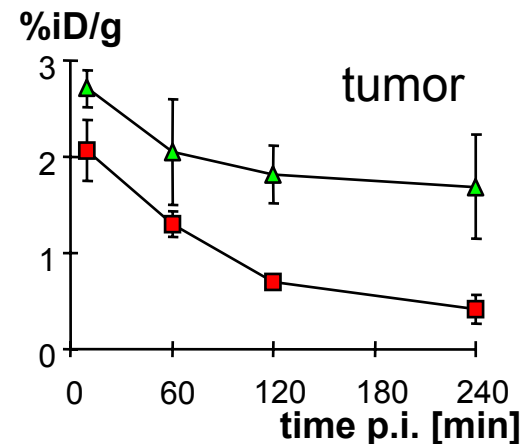
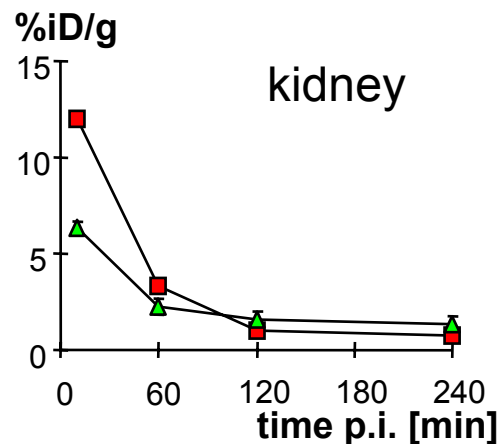
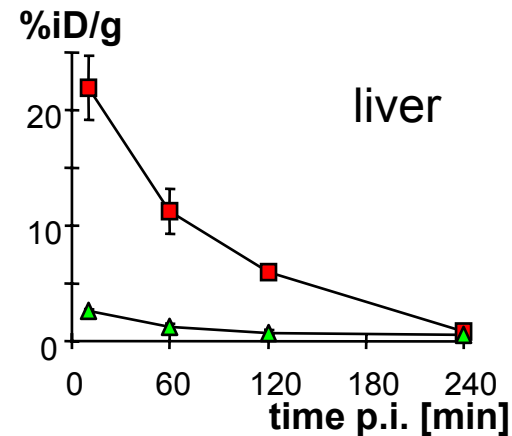
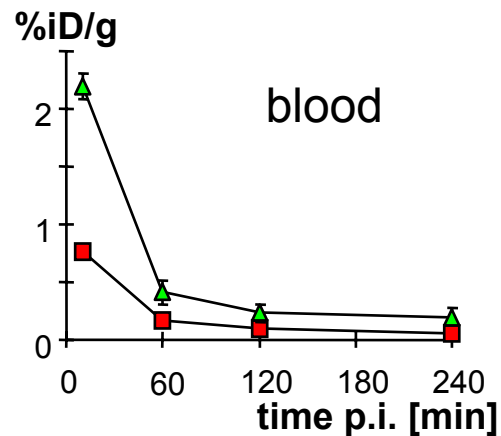


# Carbohydrated RGD-Peptides with Improved Pharmacokinetics



# Comparison of the Pharmacokinetics in Selected Tissues

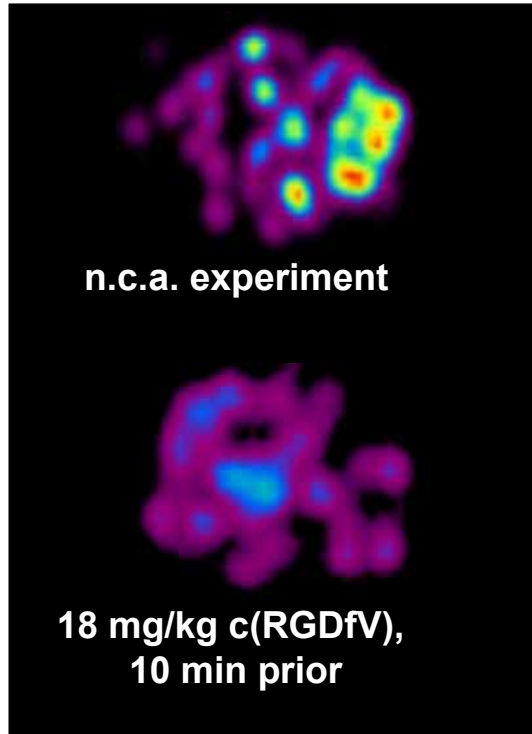
- *c(Arg-Gly-Asp-D-(l)Tyr -Val)*: **Log P = -1.89**
- ▲ I-Gluco-RGD: **Log P = -2.45**



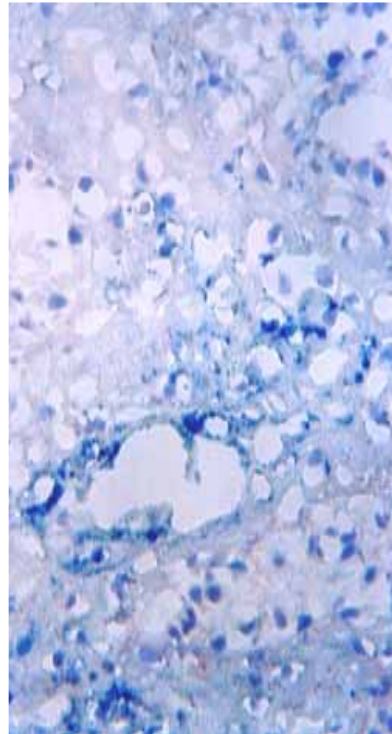
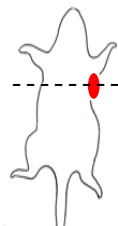
BALB/c mice,  
osteosarcoma model;  
comparable data obtained  
with M21melanoma bearing  
mice

# Non-invasive Monitoring of $\alpha_v\beta_3$ Expression on the Tumor Vasculature

nude mouse bearing a human squamous cell carcinoma at the right shoulder

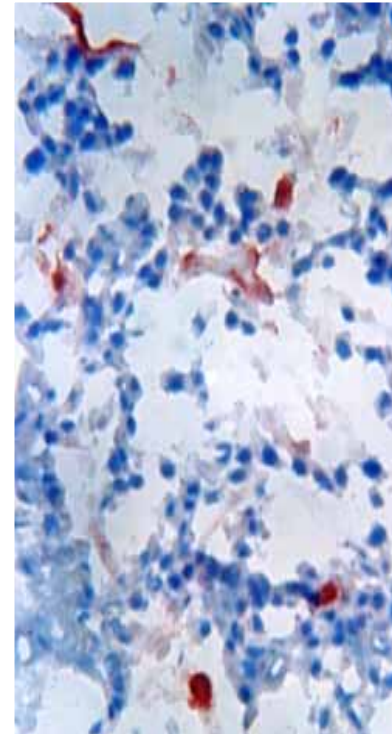


1.5h p.i



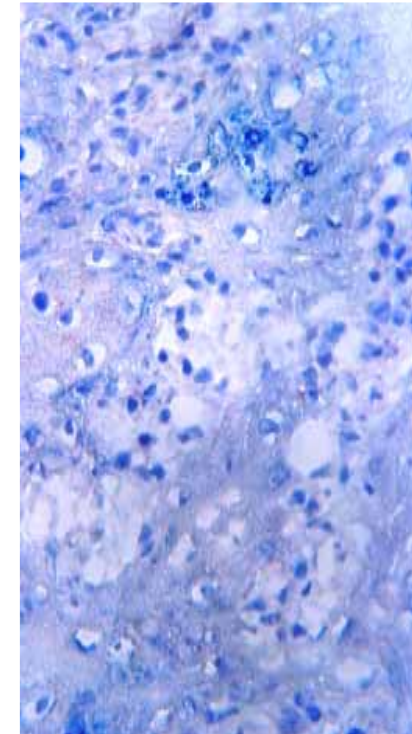
anti human  $\alpha_v\beta_3$   
MAb LM609

no expression  
of  $\alpha_v\beta_3$  on cells



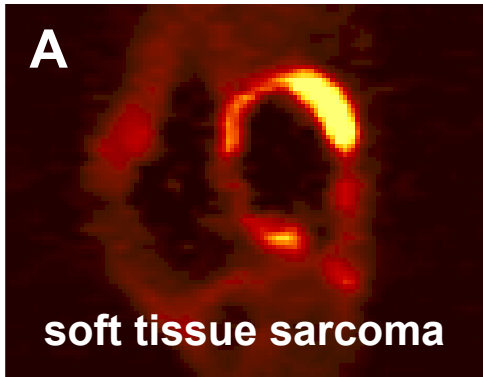
anti murine  $\beta_3$   
MAb 2C9.G2

expression of murine  
 $\beta_3$  on vasculature

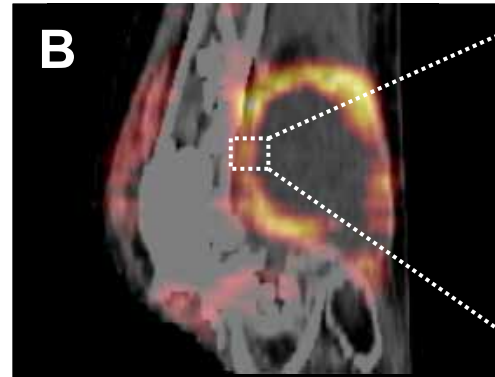


control  
(unspecific MAb)

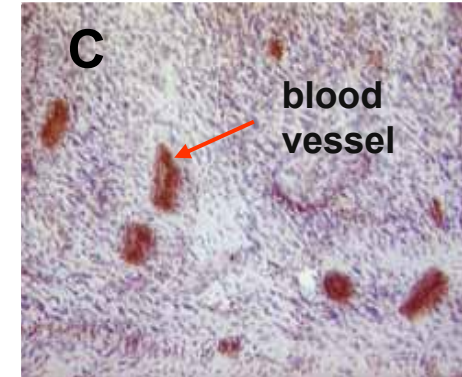
# Determination of $\alpha_v\beta_3$ -Expression in vivo



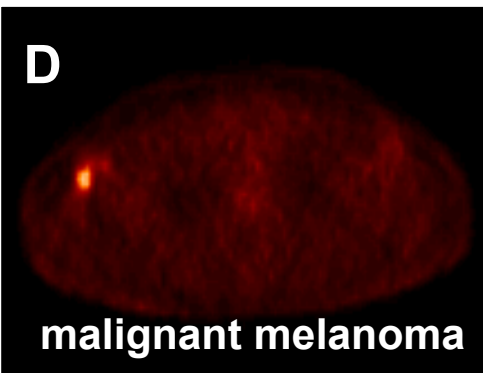
sagittal section, 170 min p.i. ,  
circular tracer uptake,  
max. SUV=10



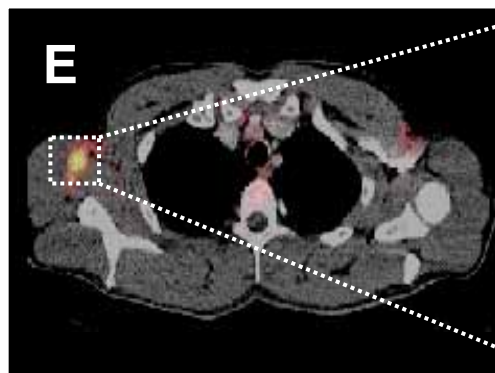
PET/CT image fusion;  
uptake corresponds with  
the tumor-wall



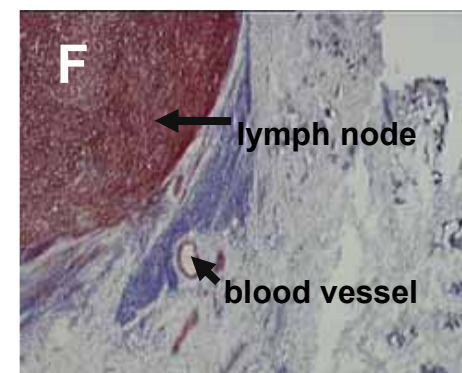
Immunohistochemistry,  
MAb LM609, staining of  
blood vessels



axial section, 140 min p,i,  
uptake in the lymph node

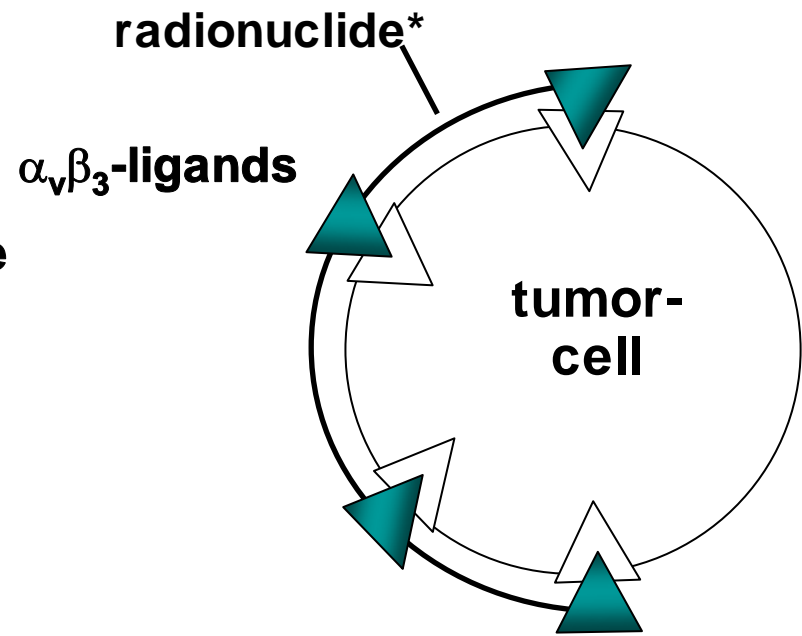
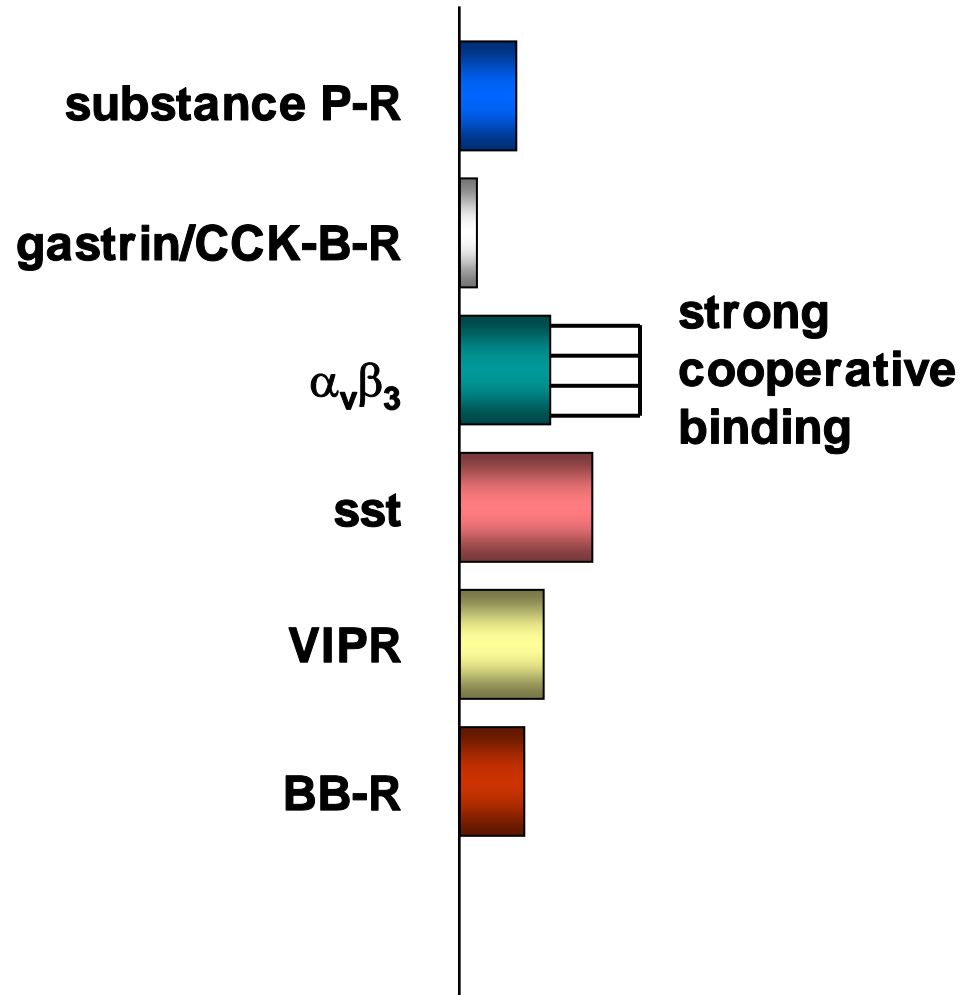


PET/CT image fusion

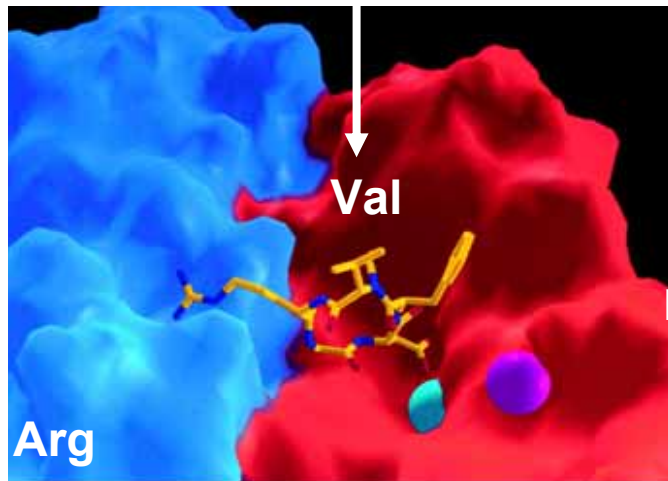


Immunohistochemistry, focal  
MAB LM609, staining of  
tumor cells and blood vessels

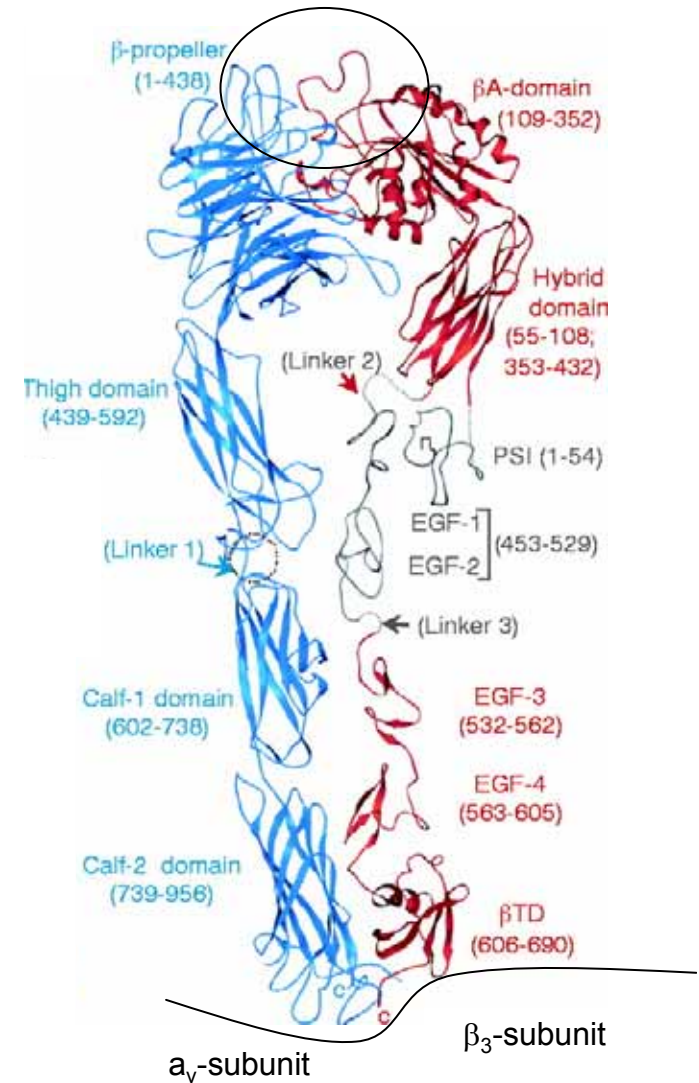
# Multiple-Ligand-Tumortargeting (MLT)



# Structure of the Extracellular Domain of $\alpha_v\beta_3$

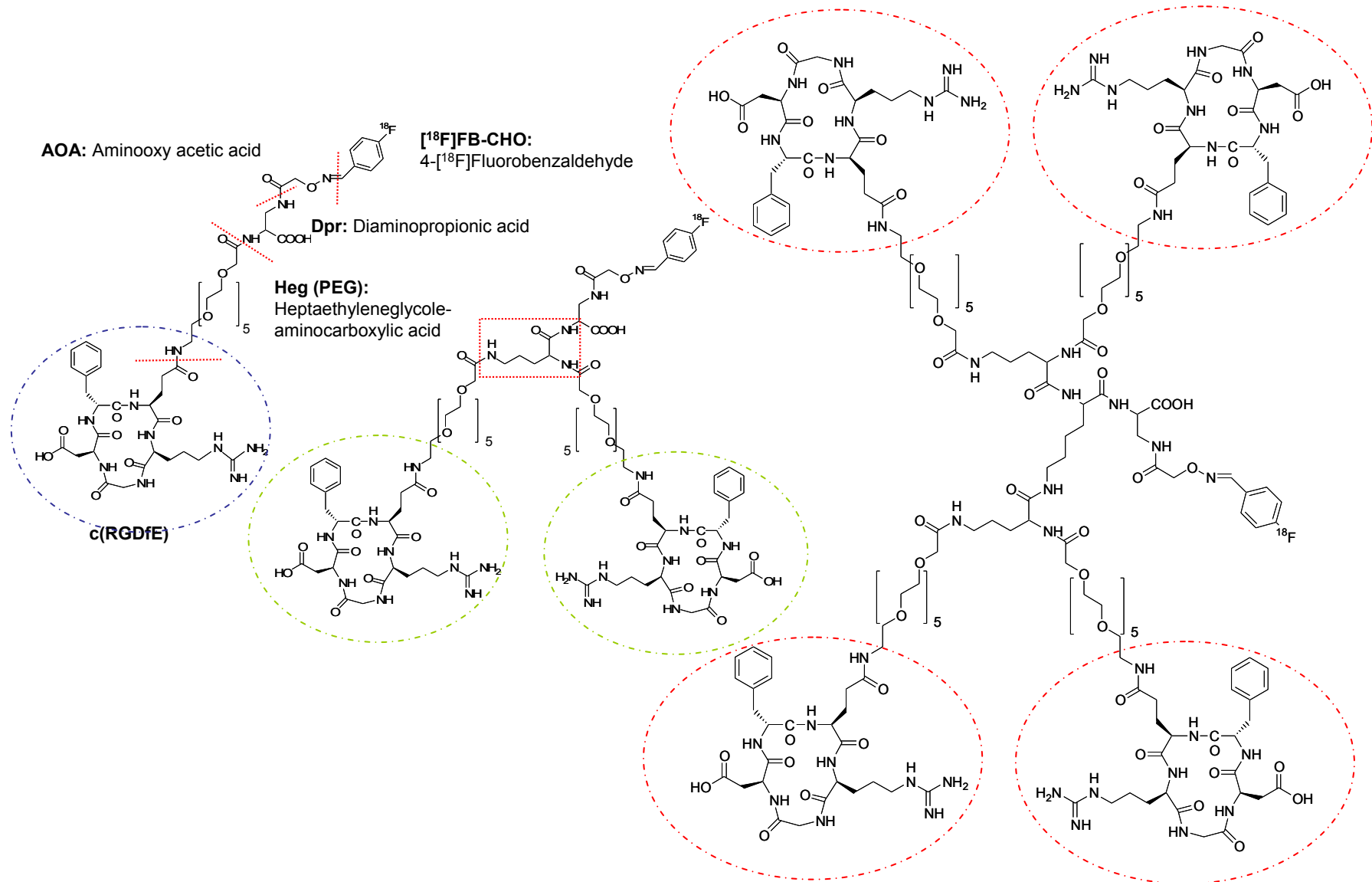


J.-P. Xiong, et. al, Science 2001.

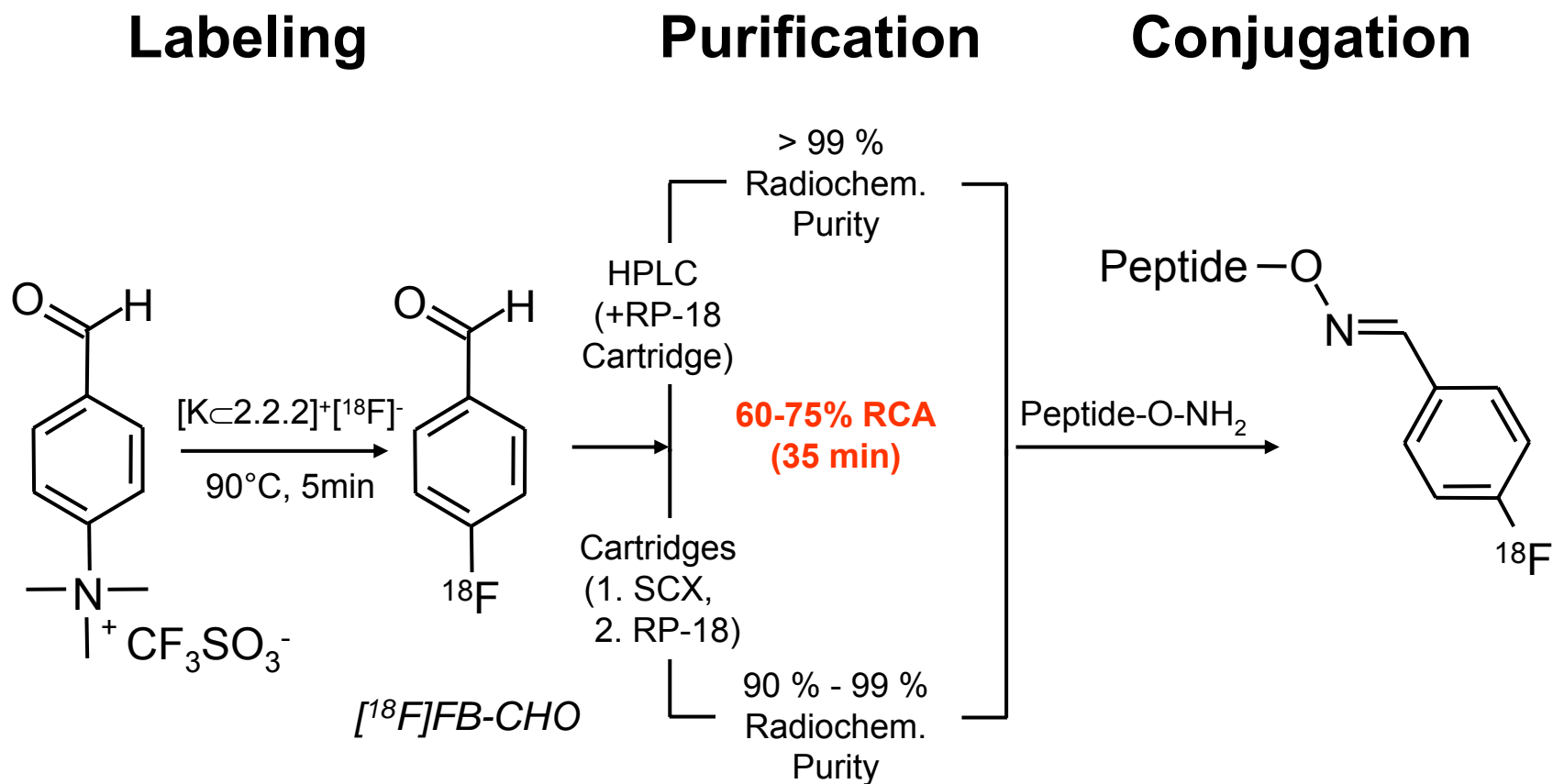




# Multimeric [<sup>18</sup>F]c(RGDfE)-Peptides

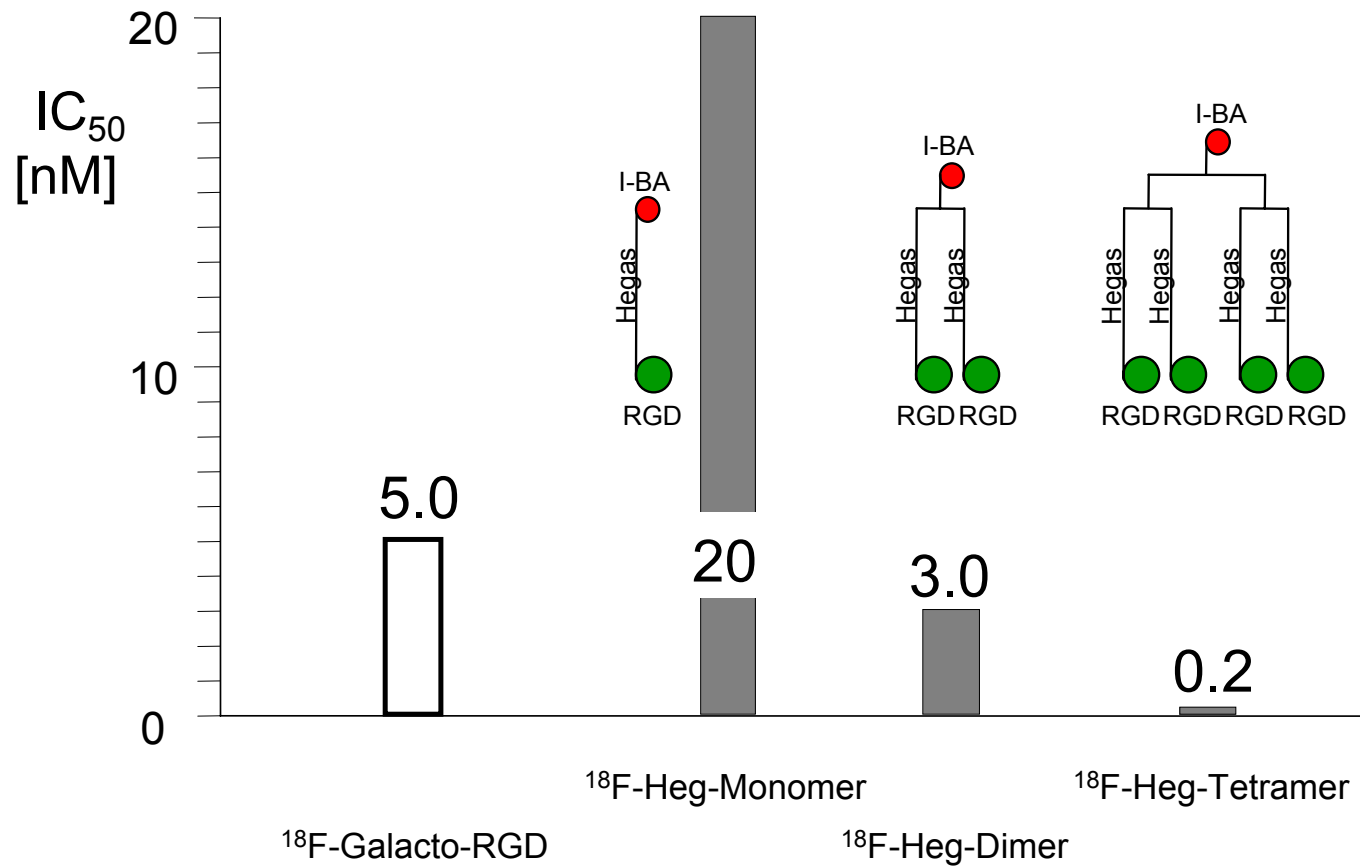


# $^{18}\text{F}$ -Labeling via Oxime Formation



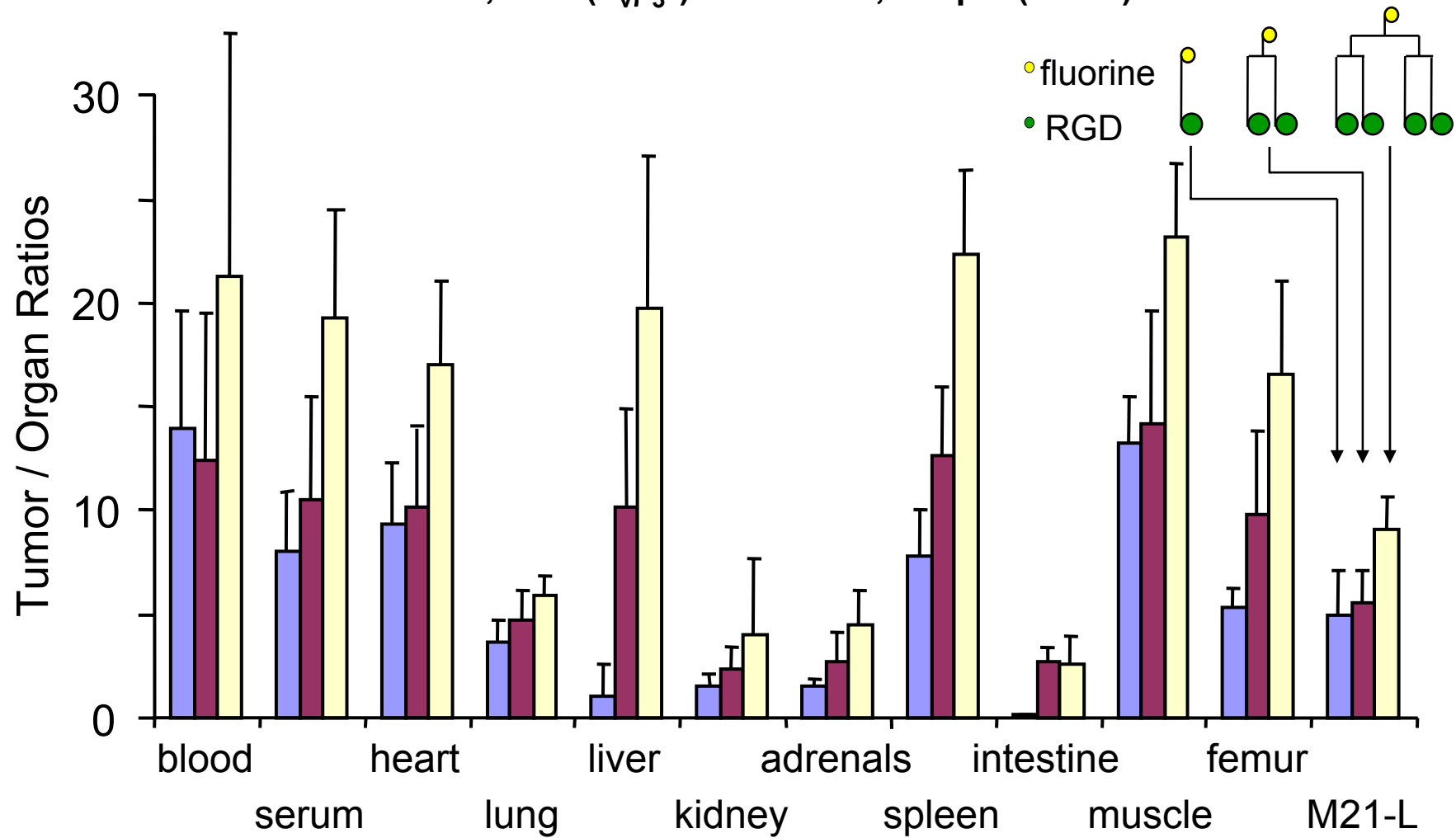
Route suitable for a variety of radiolabeled aldehydes and ketones

# Binding Affinities of Multimeric RGD-Peptide Constructs

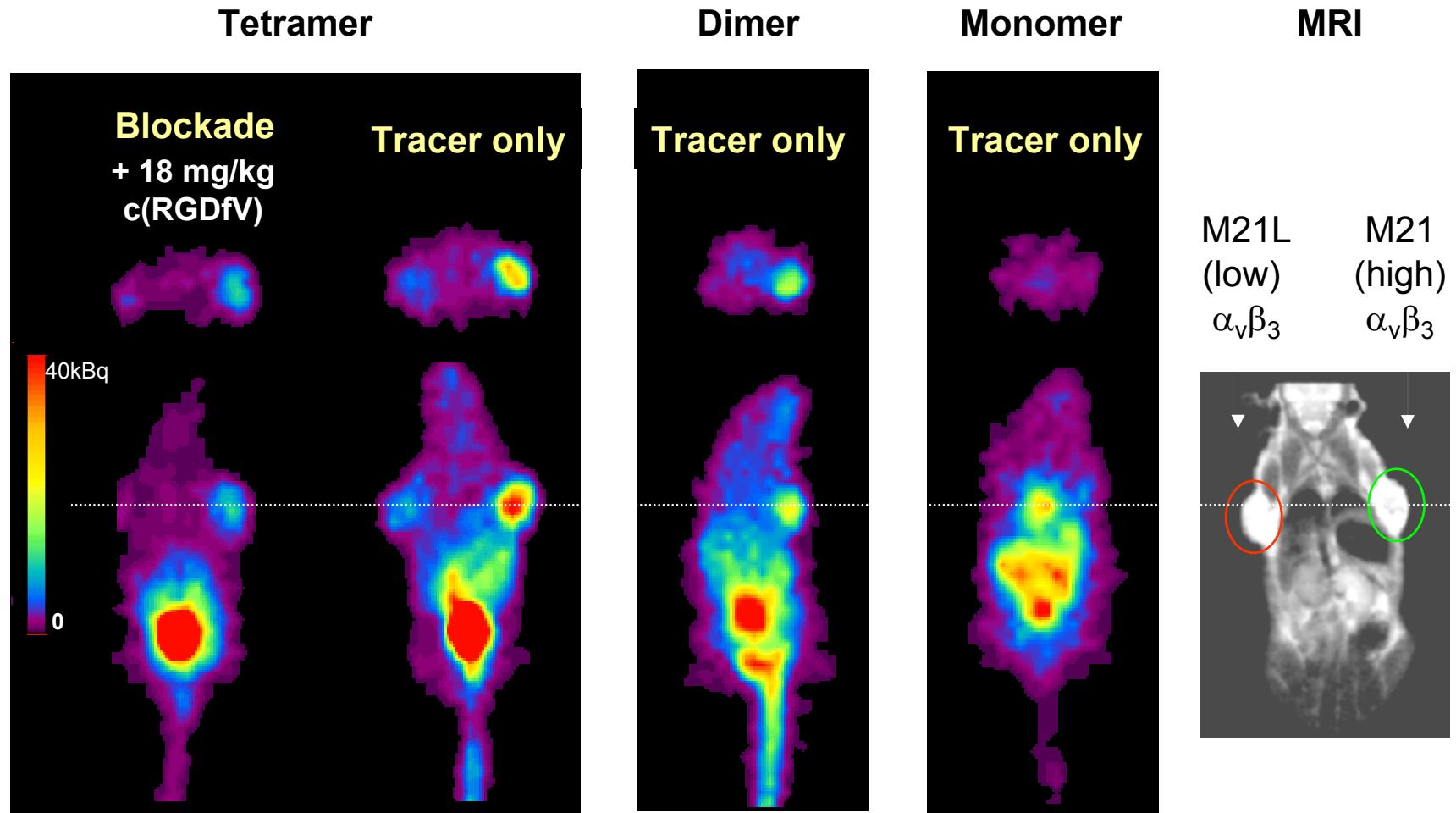


# Tumor to Organ Ratios

Nude Mice, M21-( $\alpha_v\beta_3^+$ )-Melanoma, 2 h p.i. (n=3-5)

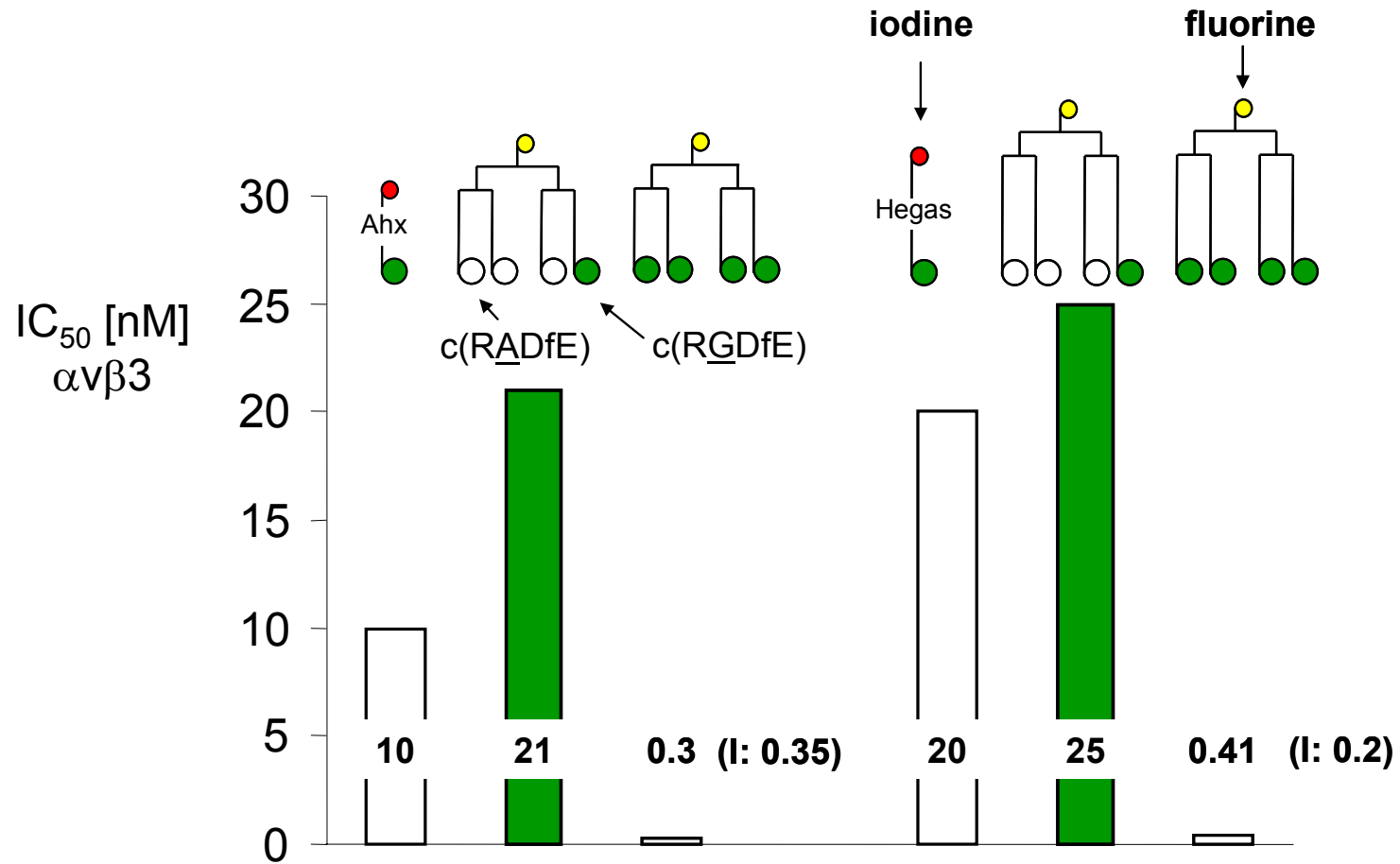


# PET Imaging of [<sup>18</sup>F]RGD-Mono-, Di- and Tetramers

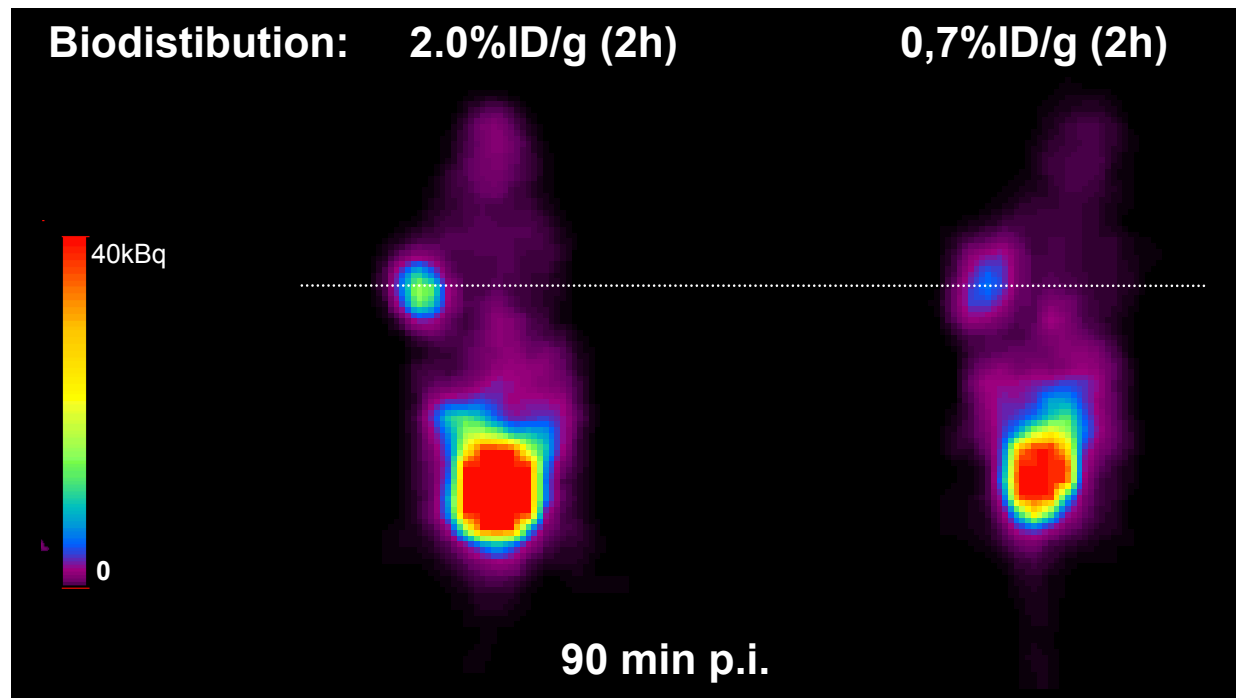
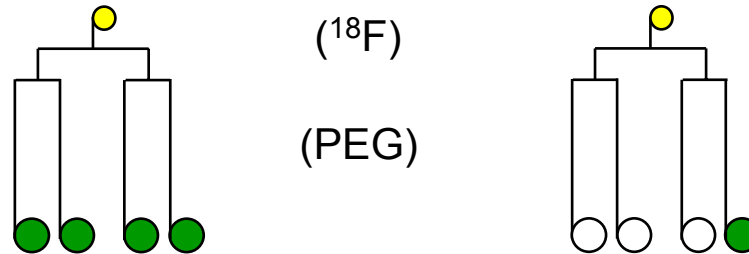


ECAT Exact HR<sup>+</sup>, 90 min p.i.

# Affinities of Multimeric RGD-Peptides with/without RAD-Sequences



# PET Imaging of Tetrameric [<sup>18</sup>F]RGD with and without „Knockout“ Sequences



# Radiopharmaceutical Chemistry and Development of Radiopharmaceuticals

***Triple T***

**Target**

**+ Tracer**

**+ Technology**

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**= Suitable Radiopharmaceutical  
and Contrast Agent**